

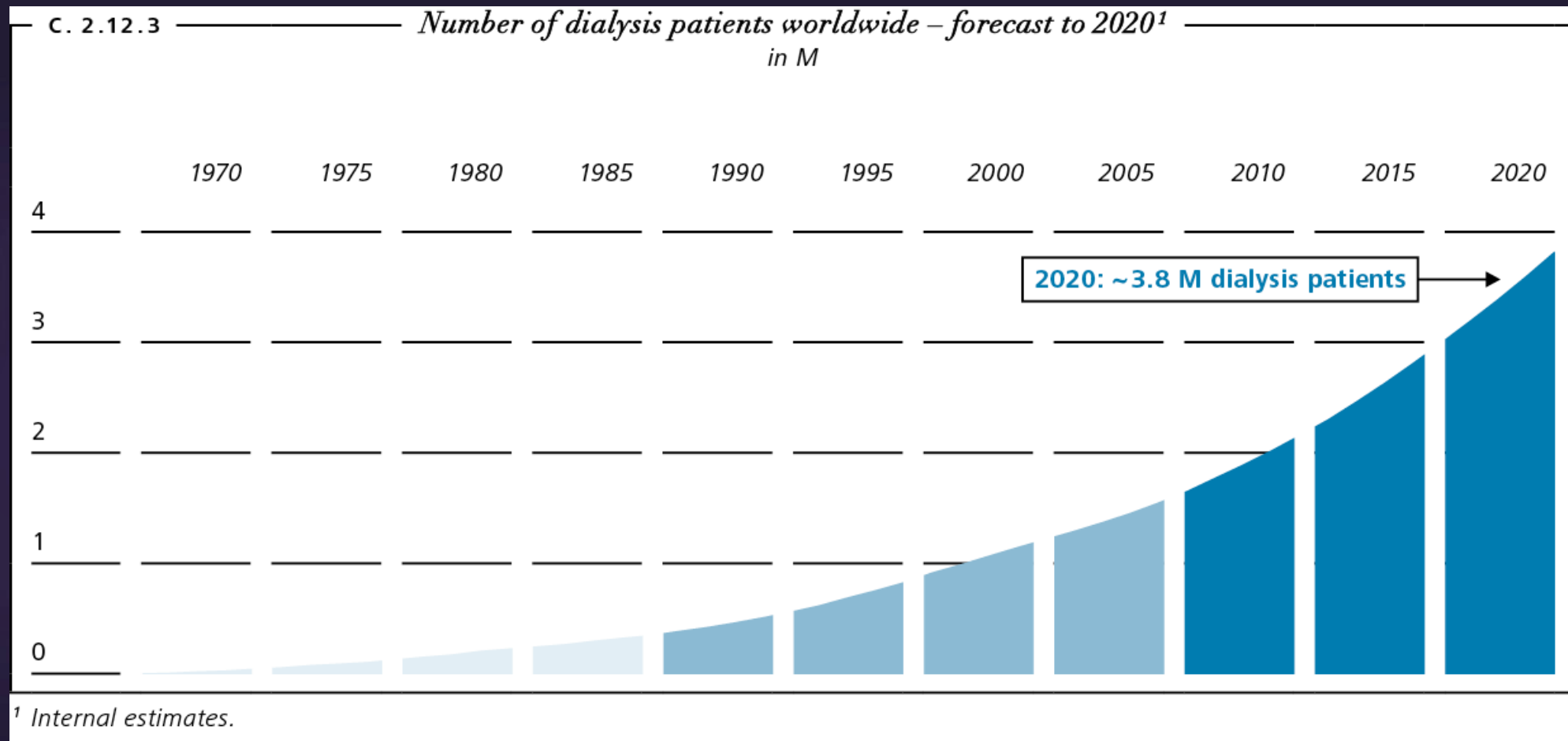
# Advances in HD Bio-Artificial Kidney (BAK)

**HESHAM ELSAYED**  
**PROFESSOR OF NEPHROLOGY**  
**AIN SHAMS UNIVERSITY**



# Do we Need Innovations in HD ?

- ▶ 2.5 millions on HD
- ▶ 350 million HD sessions / year





Questions to be Addressed

**Do we Need Innovations in HD Therapy ?**

**Are patients satisfied by HD ?**

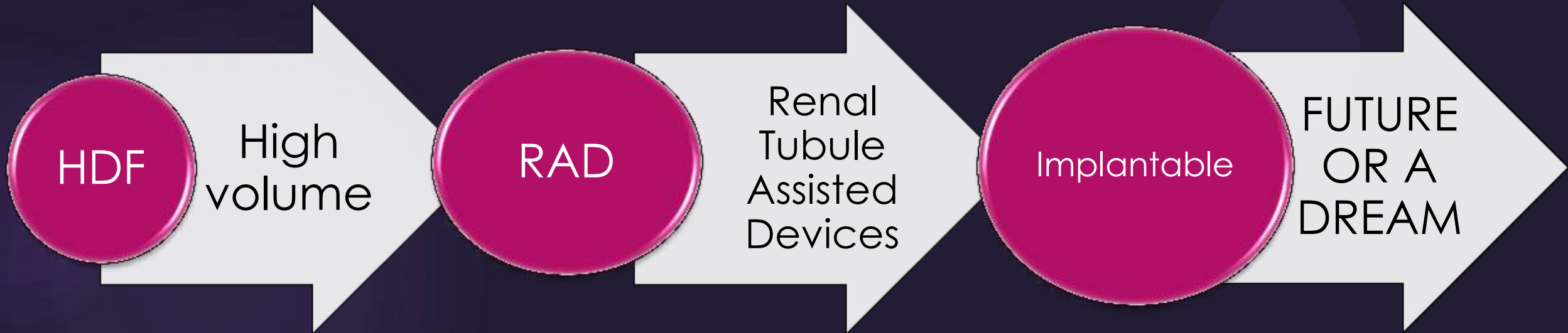
**What is the Best marker of HD adequacy  
for the Nephrologist ?**

# Current HD Therapy limitations

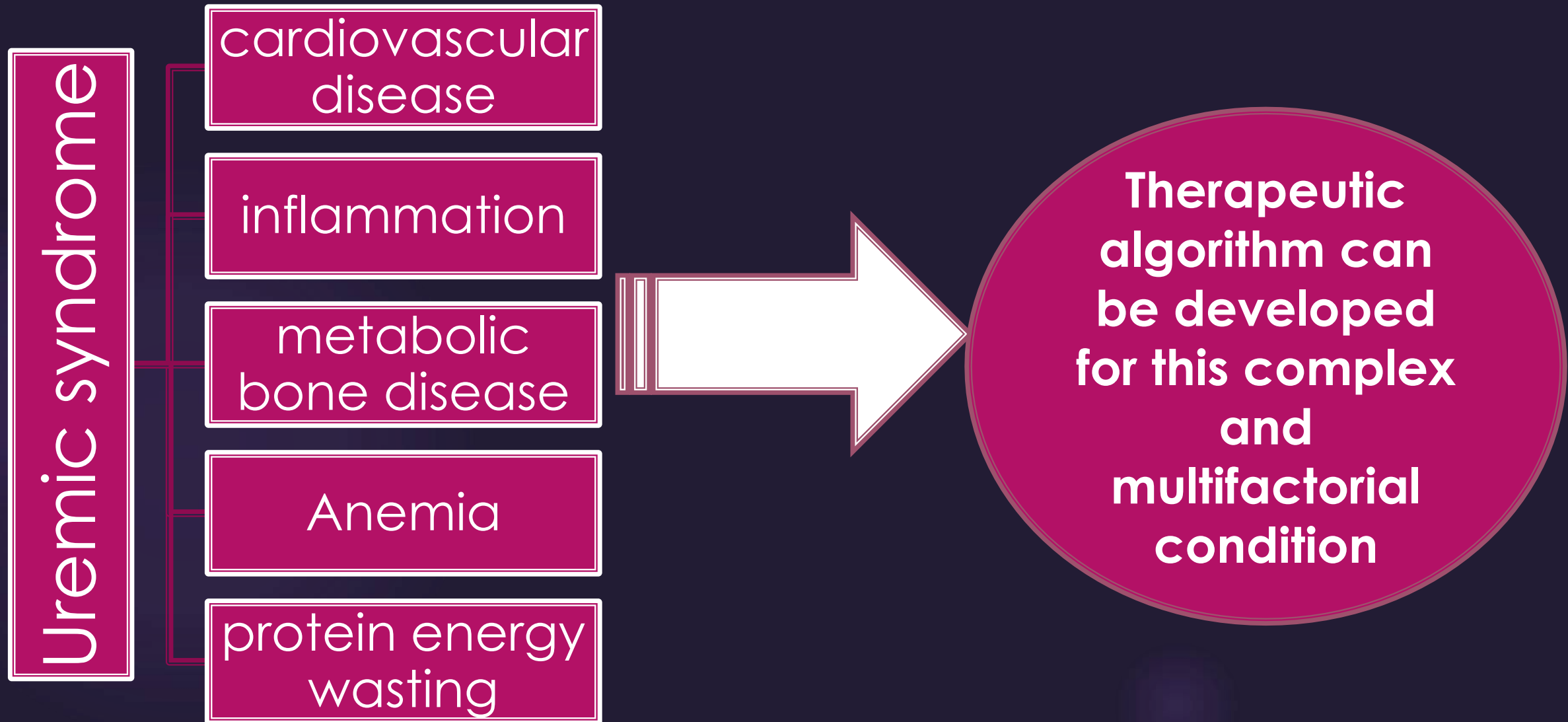
- ▶ Therapy only depends on Filtration
- ▶ Completely retention of PB uremic toxins
- ▶ No single or multiple Biomarkers are sufficient .
- ▶ Problems in Inflammation and Malnutrition.
- ▶ Non Physiological HD frequency and duration.



# Advances in HD therapy



# The uremic syndrome (the lancet Mar 2, 2016)

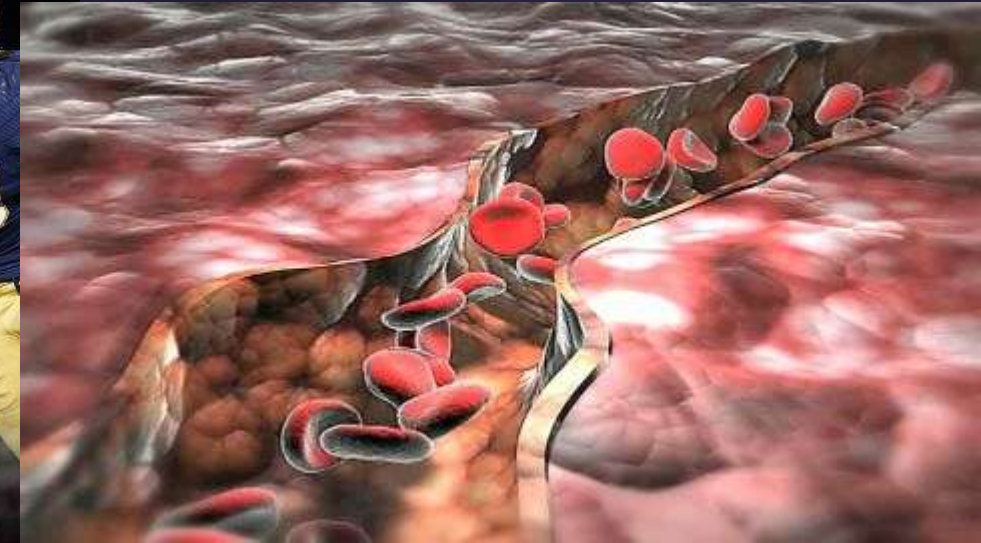
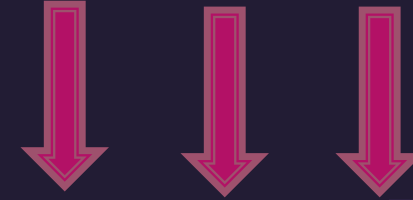




# CKD MANY PLAYERS WITH THE SAME TARGET



Targeting

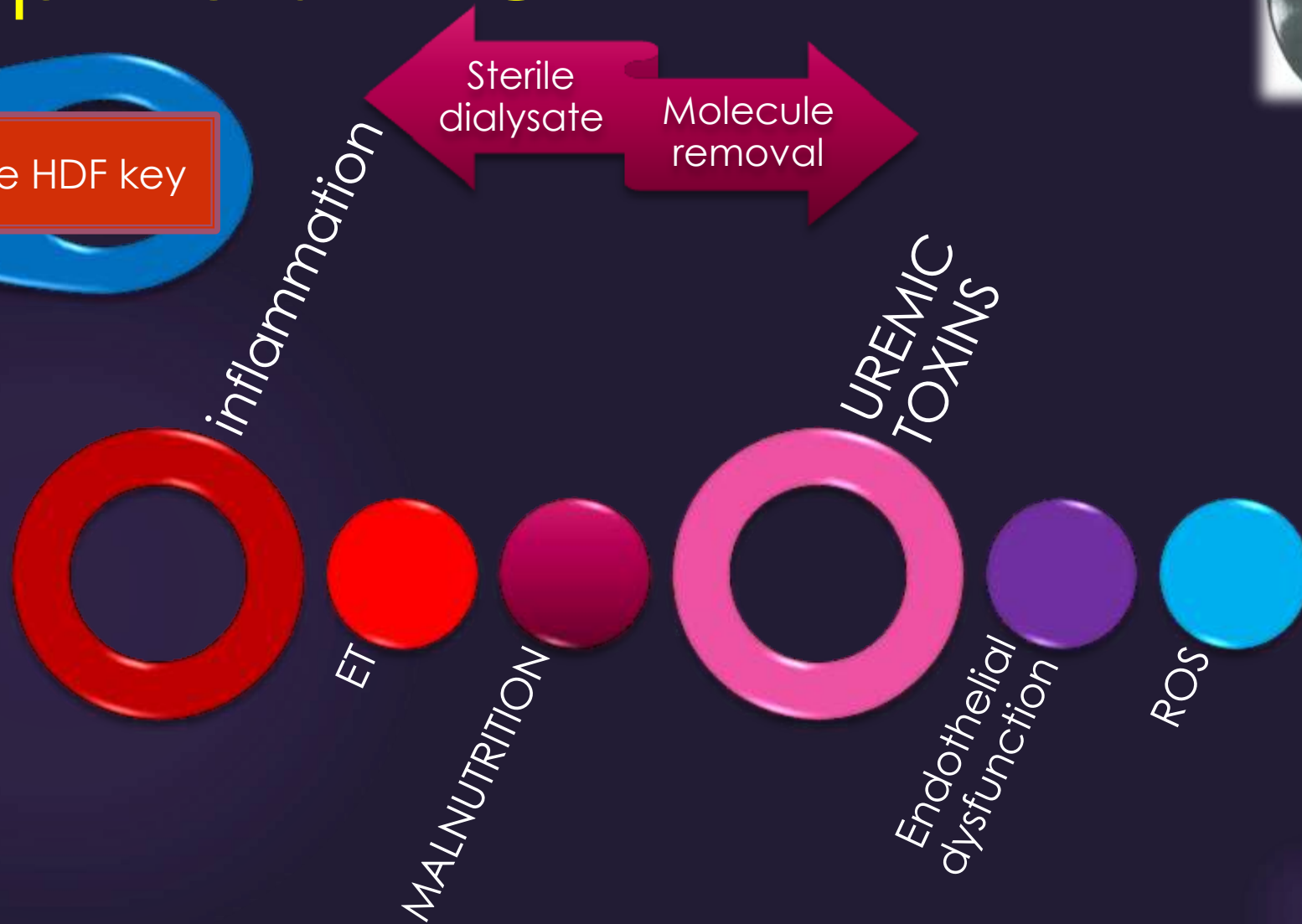


Inflamed ET

# Amplifiers in CKD

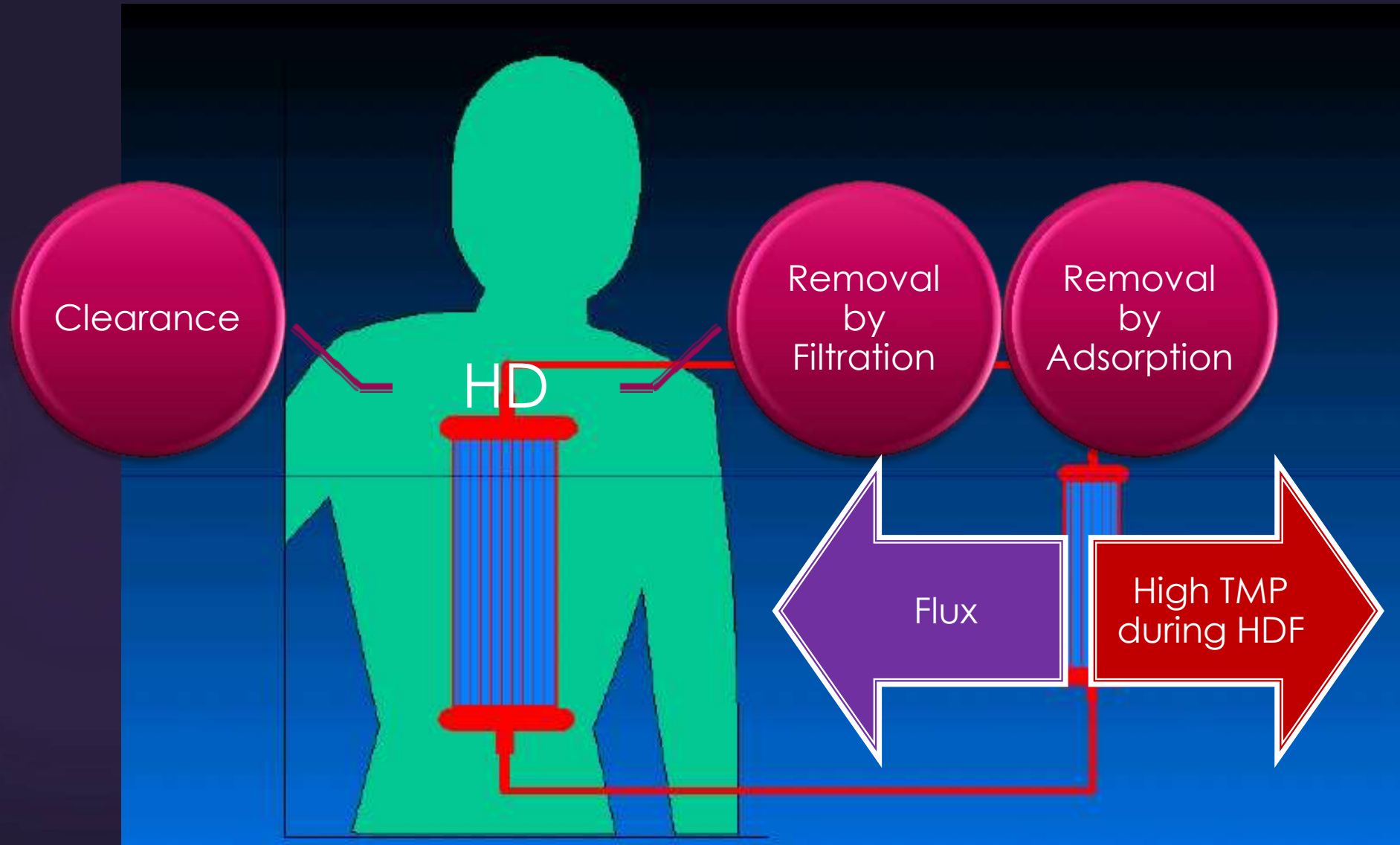


Possible HDF key

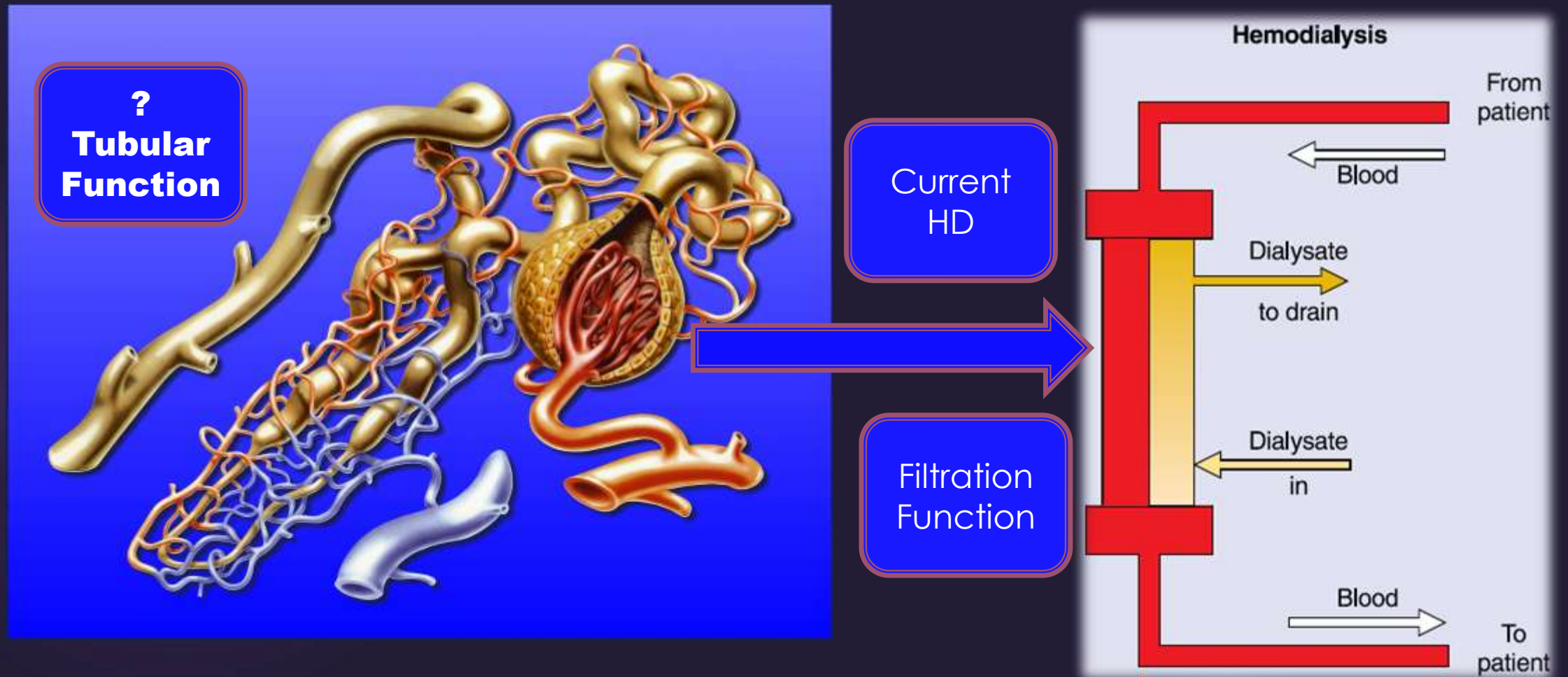




# HD : a Filtration Therapy



# Filtration Versus Metabolism



# Researches in HD membranes Towards better sieving



SC

Antifouling

Larger  
Pores

Accepting  
3 gm  
Albumin  
loss /  
session



# Uremic toxins and Pore diameter Is Not a Simple Button and a Hole



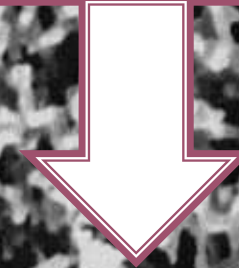
size

Dragging force  
= convect **HDF**

shape

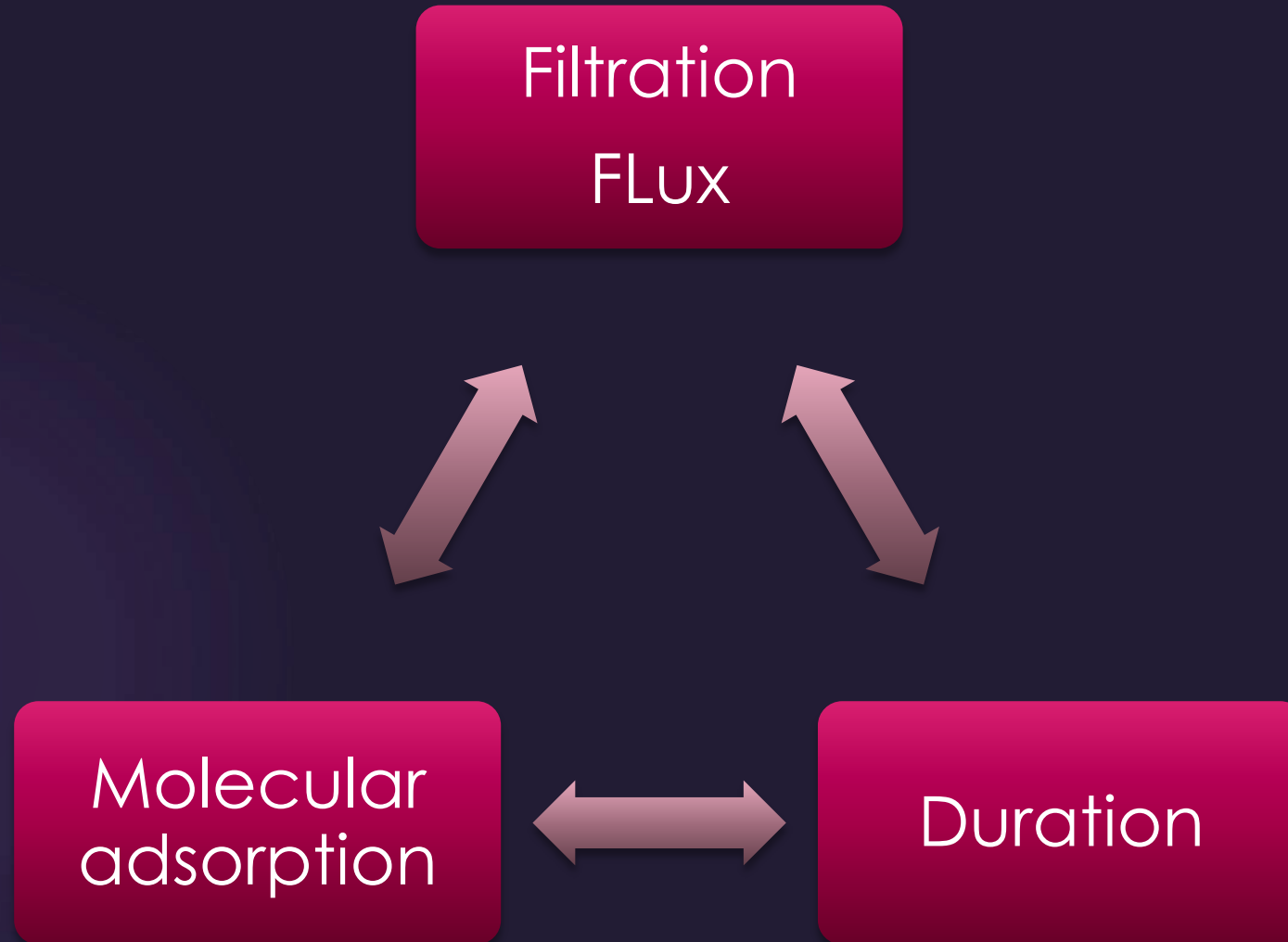
Electric  
charge

Flux Alone will Not improve  
the overall outcome  
LF – HF – HCO



**Membrane coating** for  
1-Adsorption.  
2- RAD.

# Removal By filtration



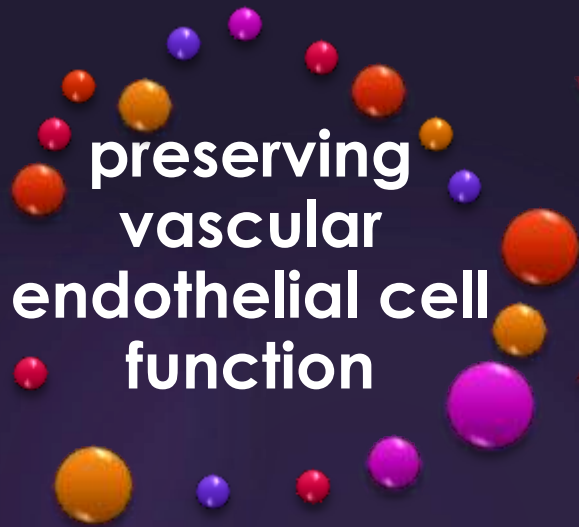
# Therapeutic challenges in Reversing the Attack of the Endothelial cells





# HDF Japanese Perspective Blood Purif

2015;40



Nephrol Dial  
Transplant 2014; 29:

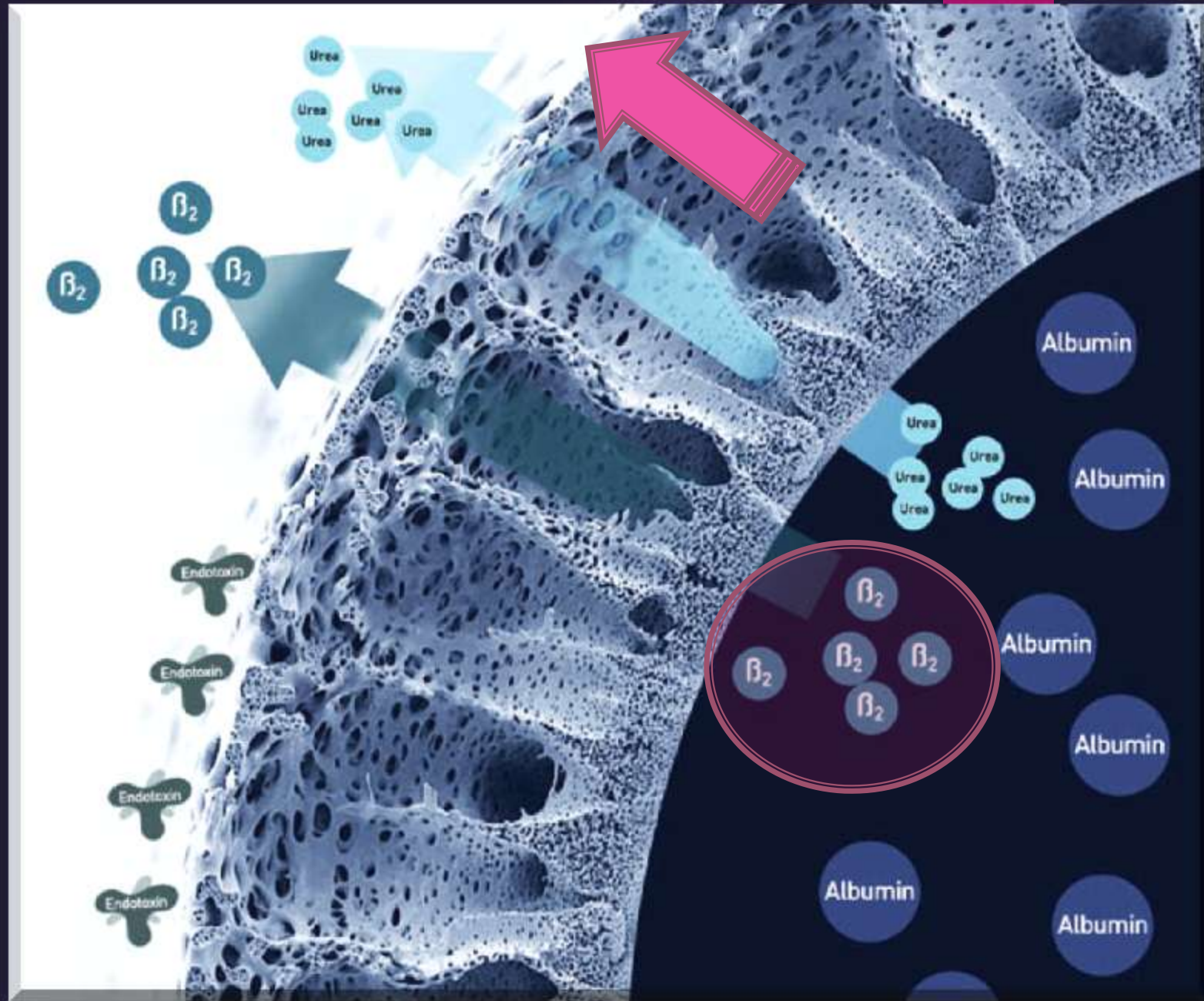


**reduction in  
fibroblast  
growthfactor-23**



**improvement of  
the nutritional  
status by reducing  
inflammatory  
stress**

HD and HDF is  
considered to be  
Glomerular  
Replacement  
therapy GRR  
Focusing in Middle  
Molecules

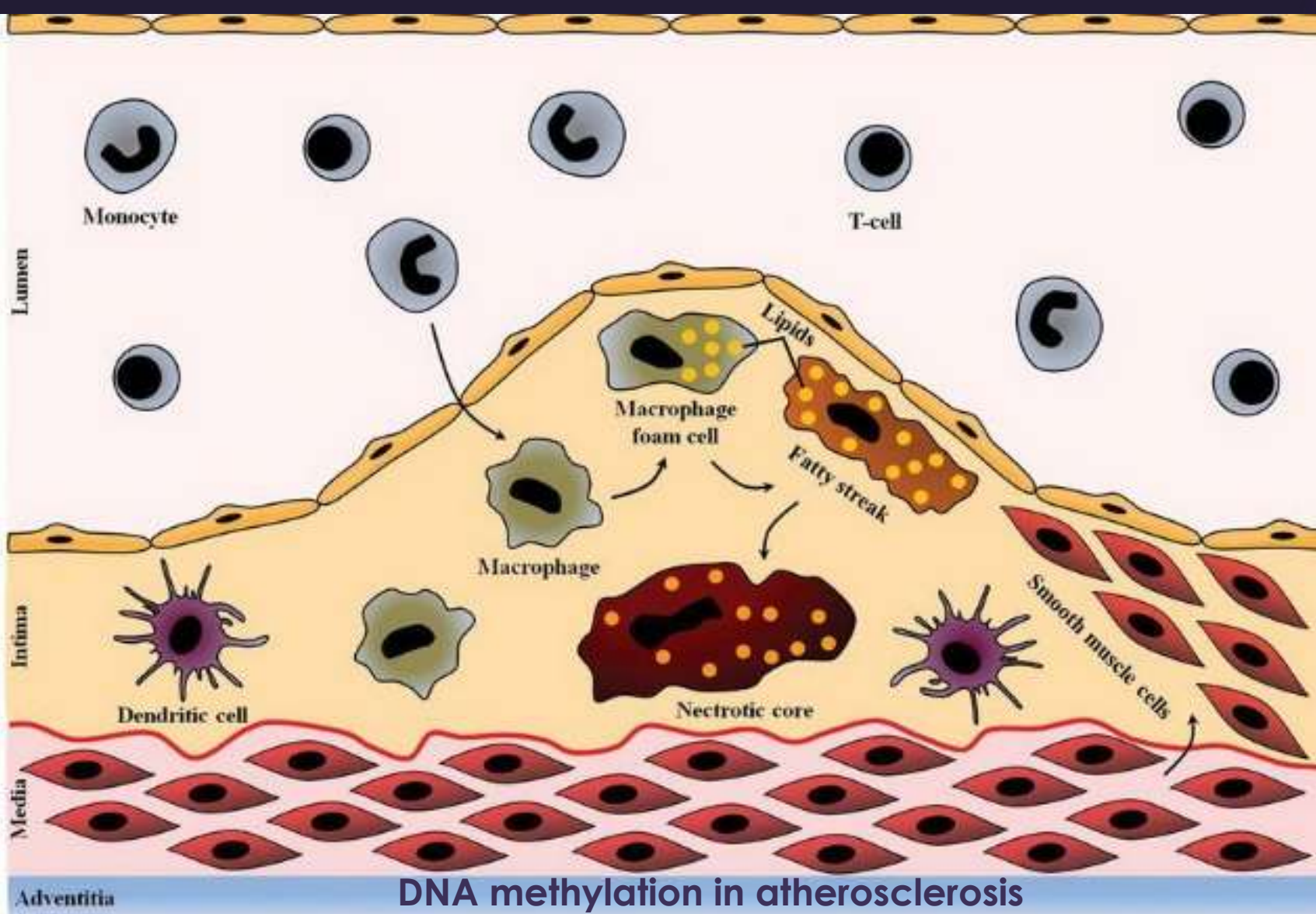


# HDF and Endothelia Functions versus HF dialysis



- OLHDF improved endothelial dysfunction
- decrease in the number of endothelial microparticles (EMP)
- increase in the percentage of endothelial progenitor cells (EPC)





monocytes differentiate into macrophages

gene-specific DNA methylation suggests alterations and advanced atherosclerotic lesions

**toxic uraemic milieu may exert a crucial impact on epigenetic gene regulation and CKD-associated accelerated arteriosclerosis**

Adam M. Zawada et al. Nephrol. Dial. Transplant. 2013

# WHICH MEMBRANE FOR HDF

Wider inner diameter  $\geq$   
**200  $\mu\text{m}$**



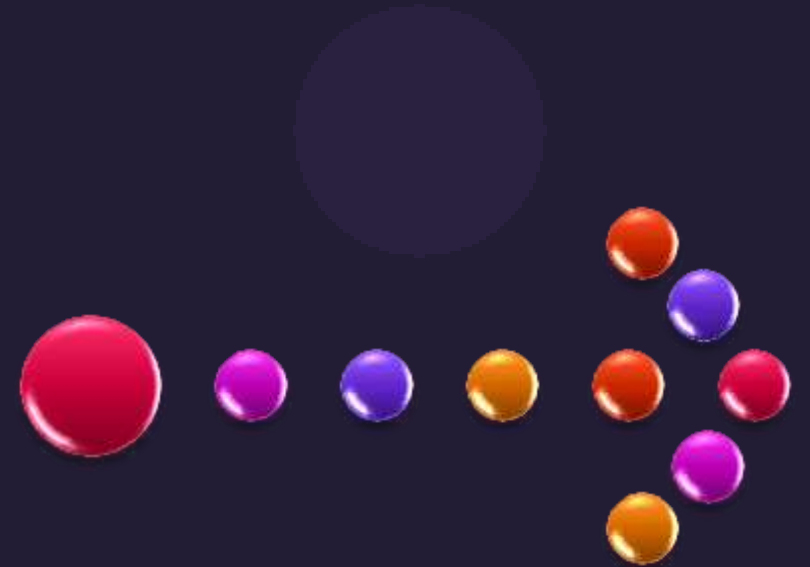
Higher UF  $\geq 50$



Higher Blood Flow  $\geq 400$   
ml/min

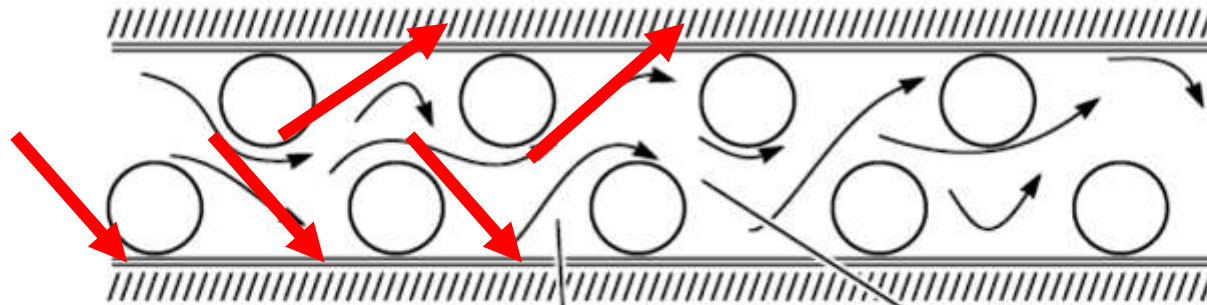


Substitution  
volume  
25 litre  
SC of B2m  
 $\geq 0.8$

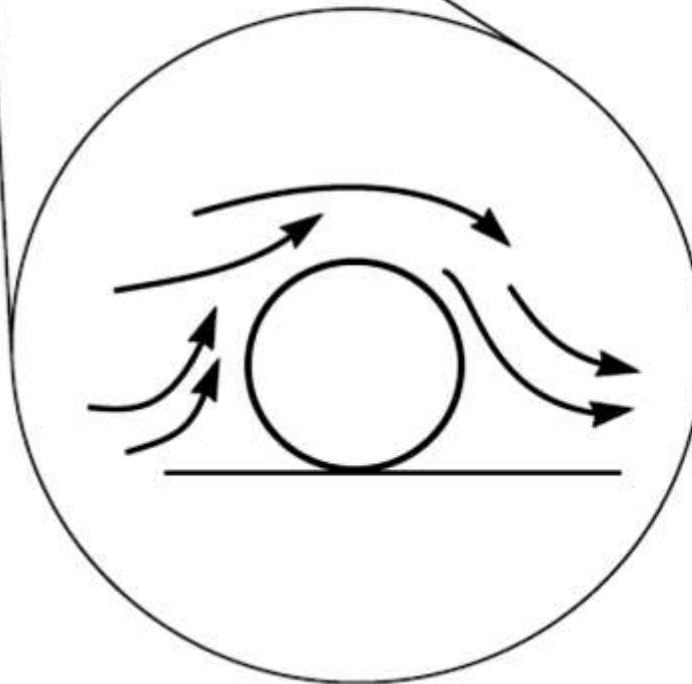


Inner diameter Fiber  $\leq 200 \mu\text{m}$

Contrib Nephrol. 2011;173



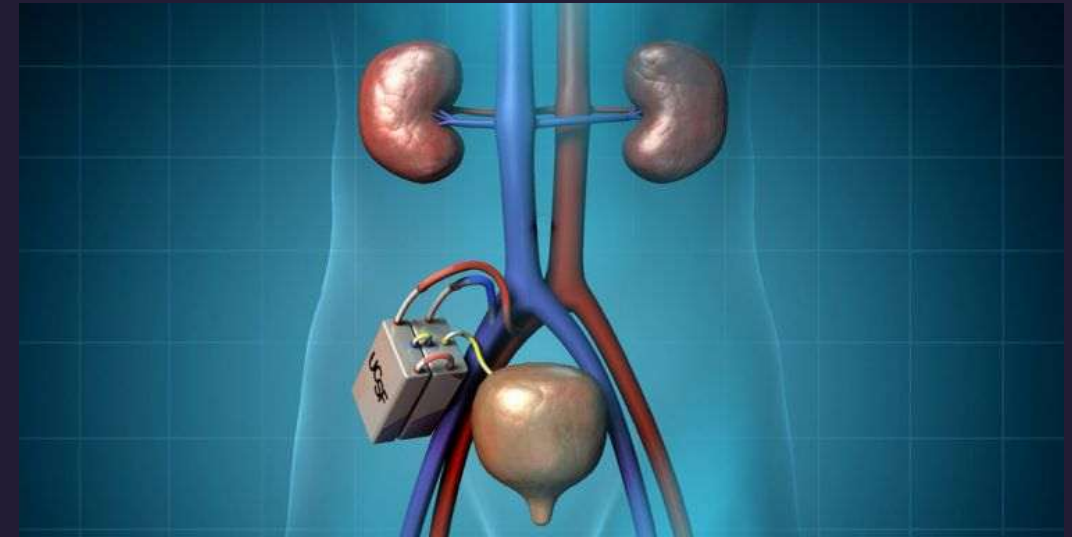
(IFEHD) using these dialyzers, therefore, has the advantage of increasing solute removal efficiency by enhancing convective transport and the simultaneous disadvantage of decreasing solute removal efficiency **by causing membrane fouling**



**TURBULENT  
FLOW  
HIGH SHEAR  
STRESS  
INCREASE  
FOULING INSIDE  
THE FIBER  
LUMEN**



# If we believe in History : we should Realize The Future !

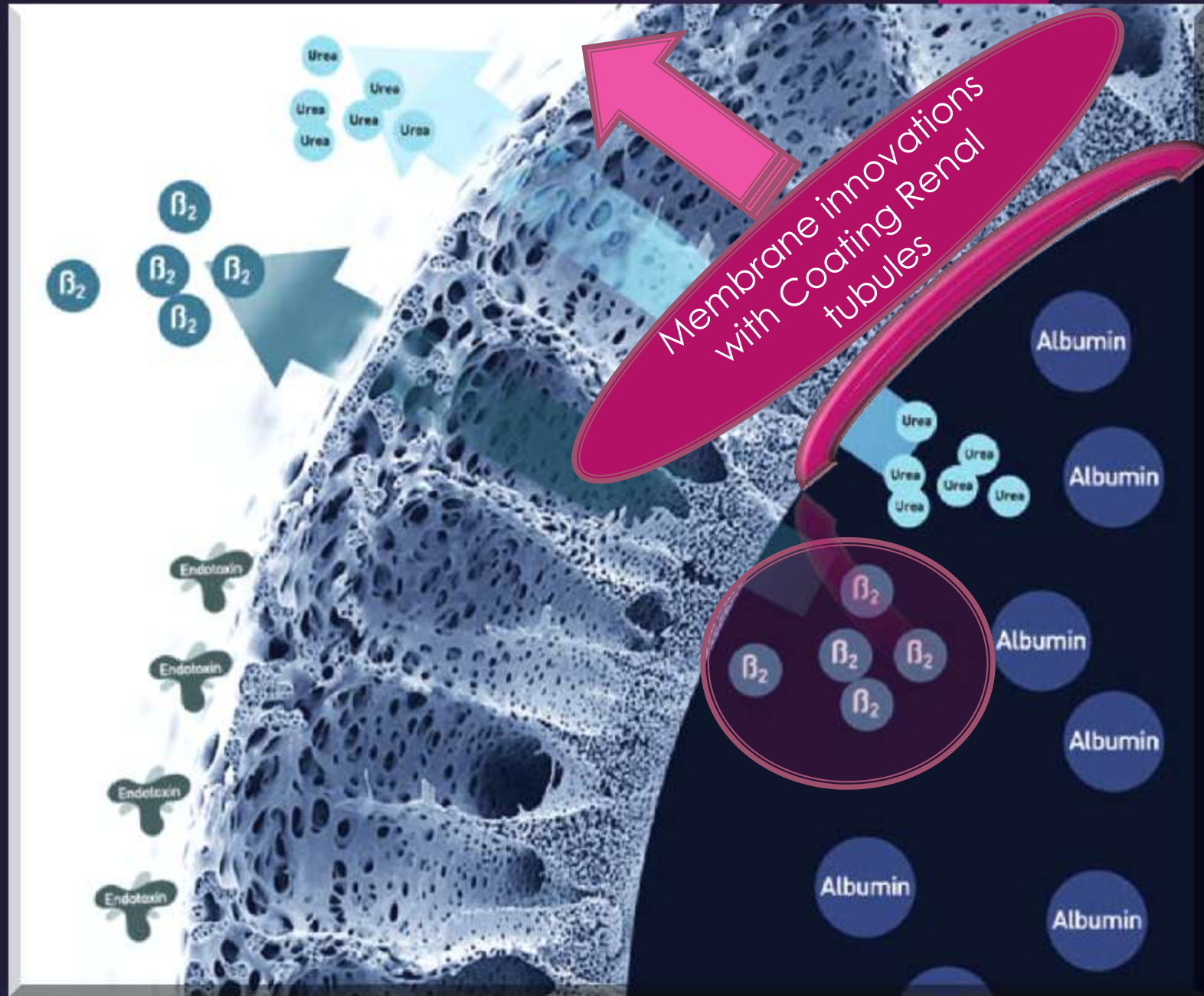


**BioArtificial Kidney  
Implantable IBAK**

# Renal Tubule Assisted Devices

The Philosophy Deserve to innovate  
Why we are in need of RAD ?

HD is considered  
to be Glomerular  
Replacement  
therapy GRR  
Focusing in  
Middle  
Molecules



# ► What Beyond Filtration is Missing in HD

Fountain of Youth

Regeneration  
capacity to stress

Senescent  
cells

Frail

Healthy  
Peoples

Above  
70 y

FRAIL

Loss of cellular  
survival ,  
Regeneration  
and function

Genetic and  
Epigentic  
changes

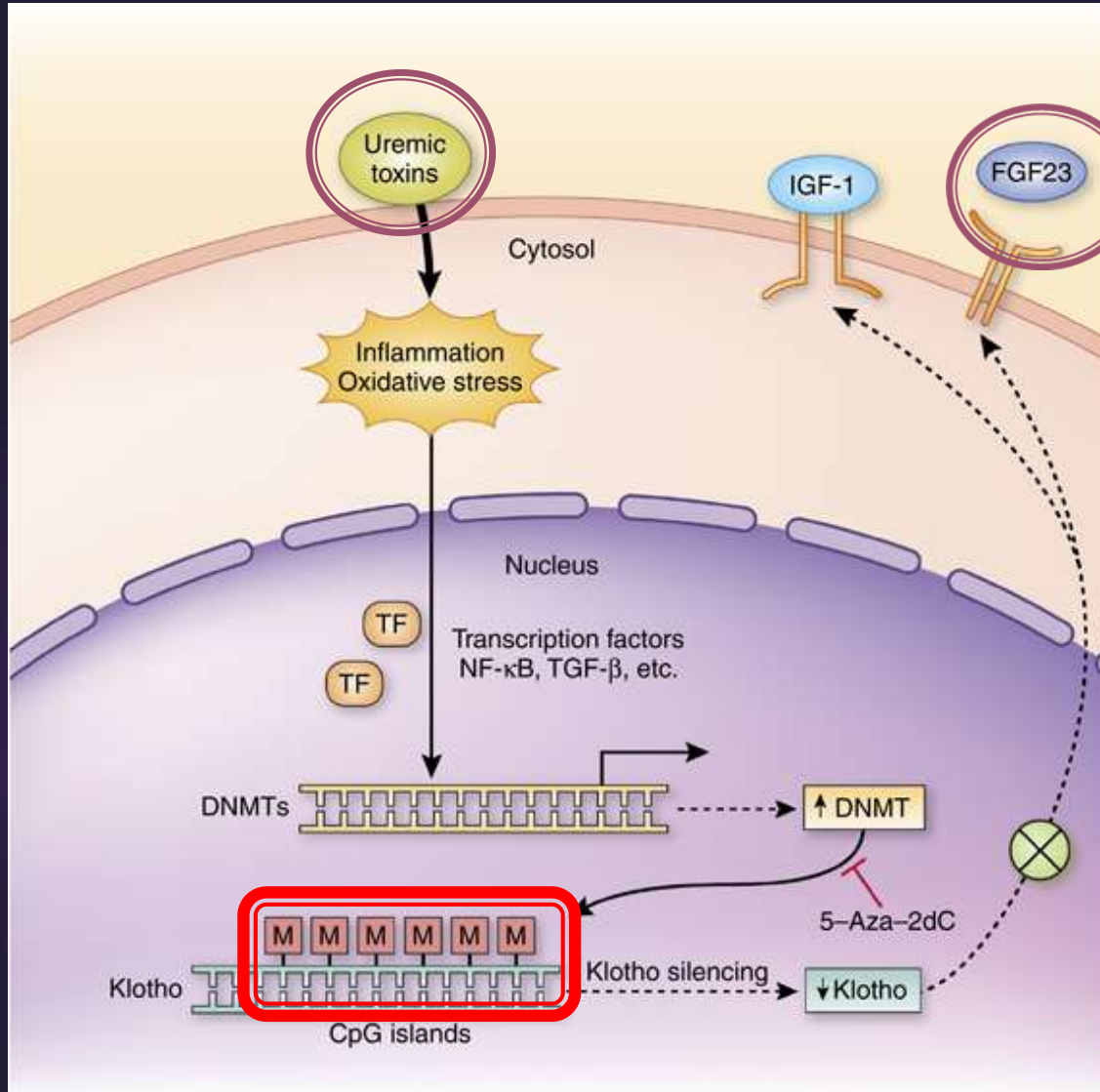
Accumulation of  
Metabolites

Below  
40 y  
On HD



## ROLE OF UREMIC TOXINS : Effect on KLOTHO Gene

JASN December 4, 2014



coreceptor

Uremic Toxins

Hypermethylated  
status of *KLOTHO*

induce DNA  
methyltransferase  
(DNMT) protein  
expression,

Nephrol Dial Transplant (2013) 28: 48–54

doi: 10.1093/ndt/gfs451

Advance Access publication 8 November 2012

## **Out of control: accelerated aging in uremia**

Jeroen P. Kooman<sup>1</sup>, Natascha J.H. Broers<sup>1</sup>, Len Usvyat<sup>2</sup>, Stephan Thijssen<sup>2</sup>, Frank M. van der Sande<sup>1</sup>, Tom Cornelis<sup>1</sup>, Nathan W. Levin<sup>2</sup>, Karel M.L. Leunissen<sup>1</sup> and Peter Kotanko<sup>2</sup>

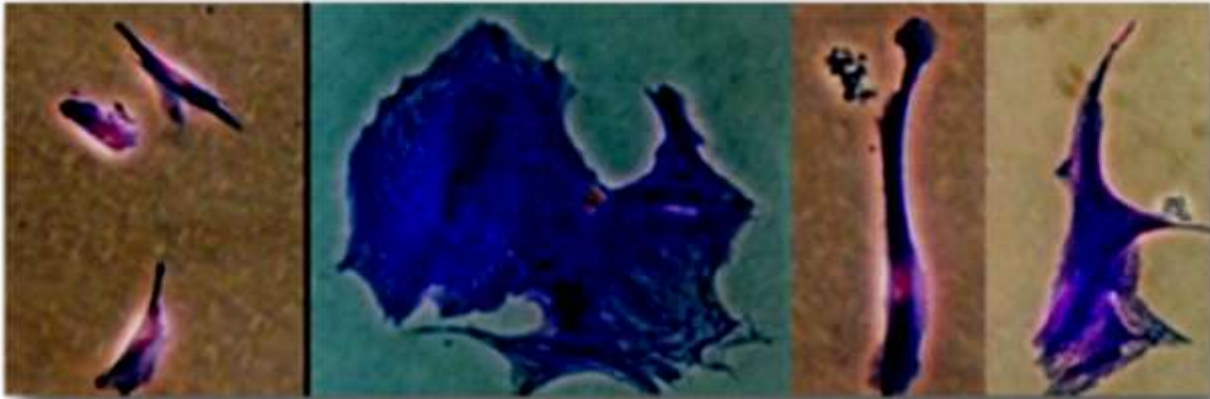
<sup>1</sup>Department of Internal Medicine, Division of Nephrology, University Hospital Maastricht, Maastricht, the Netherlands and <sup>2</sup>Renal Research Institute, New York, USA

reduced physical capacity and the loss of muscle mass are associated with a high prevalence of frailty. Phenotypically, frailty is a clinical syndrome characterized by multiple pathologies, such as weight loss, fatigue, weakness, low activity, slow motor performance and balance and gait abnormalities

**44% of dialysis patients below 40 years of age were classified as frail**



# Advanced CKD characterized by many features of Aging:



Senescent cells change their morphological characteristics and these changes are accompanied by alterations in nuclear structure, gene expression, protein processing and metabolism.



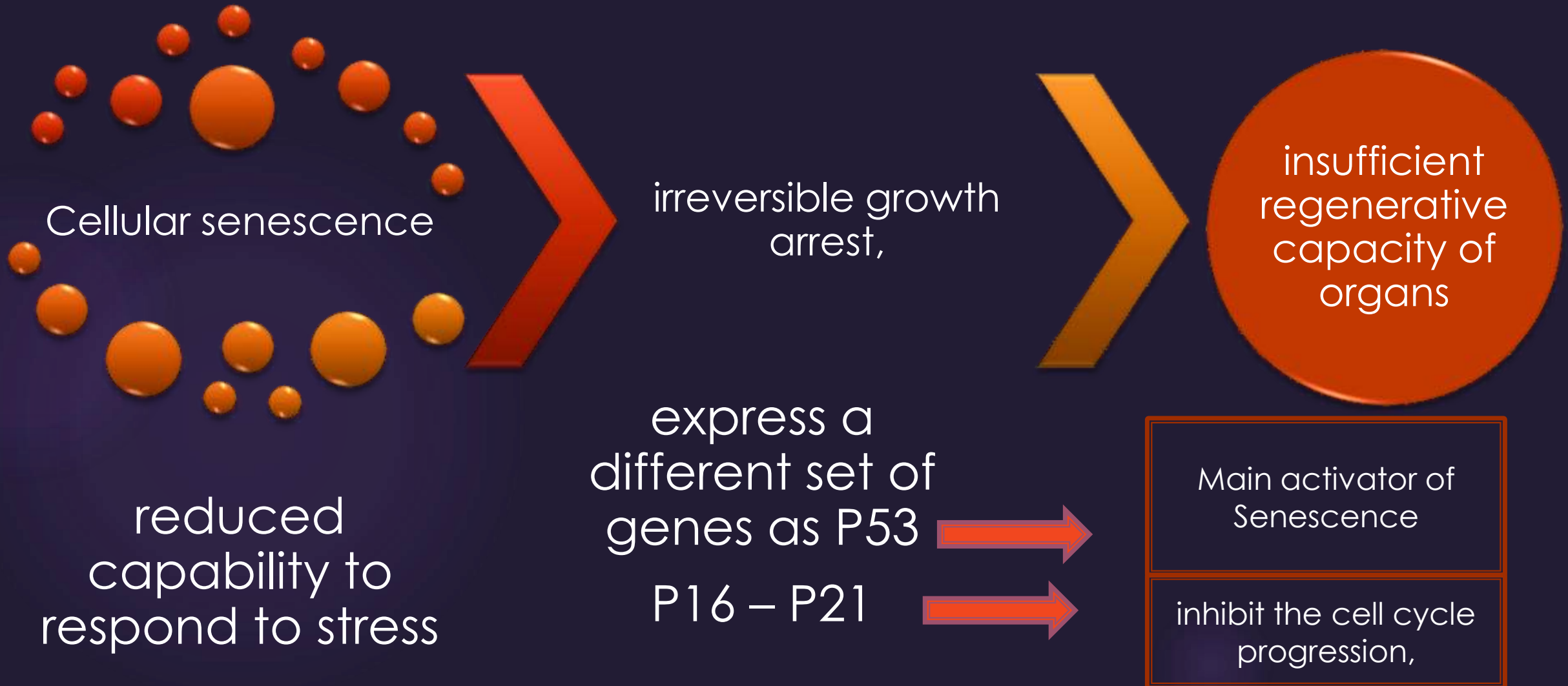
Senescent cells



Stem cells : Senescent

# Cellular senescence is a state of permanent and irreversible cell cycle arrest

American Journal of Phys 15 July 2012





## **Indoxyl Sulfate Induces Endothelial Cell Senescence by Increasing Reactive Oxygen Species Production** *January 2012 Volume 22, Issue 1*

## **Protein-Bound Uremic Toxins: New Culprits of Cardiovascular Events in Chronic Kidney Disease Patients**

***toxins***

*Toxins* **2014**, 6, 665-678

### **Cardiorenal Syndrome**

#### **The Emerging Role of Protein-Bound Uremic Toxins**

*Circulation Research*

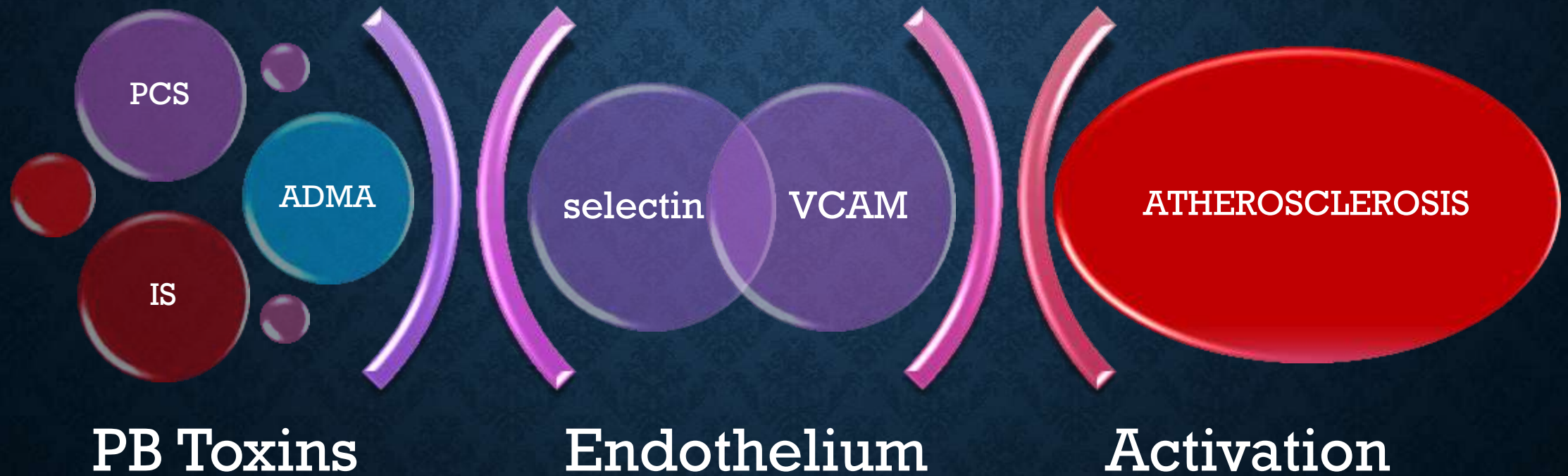
November 9, 2012





# Protein-Bound Uremic Toxins Stimulate Crosstalk between Leukocytes and Vessel Wall

JASN December 2013



# Evidences in Uremia to promote Aging

Human umbilical vein endothelial cells (HUVEC)  
incubated with uremic serum **Experimental Gerontology August 2014**



Uremic serum  
increased ROS

Uremic serum  
increased NF-  
κB

uremic serum  
induce  
apoptosis  
In Aging Cells

oxidative  
stress damage  
senescent  
cells

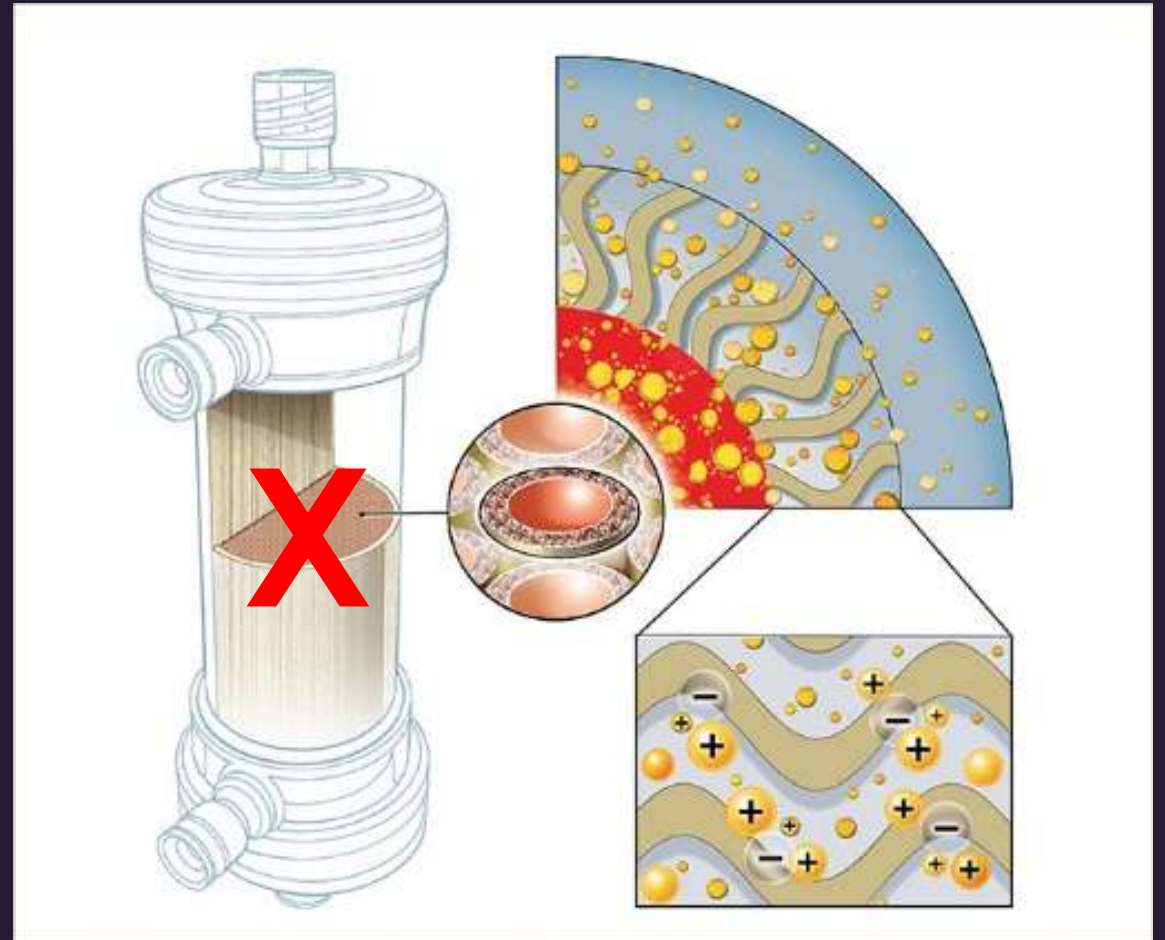


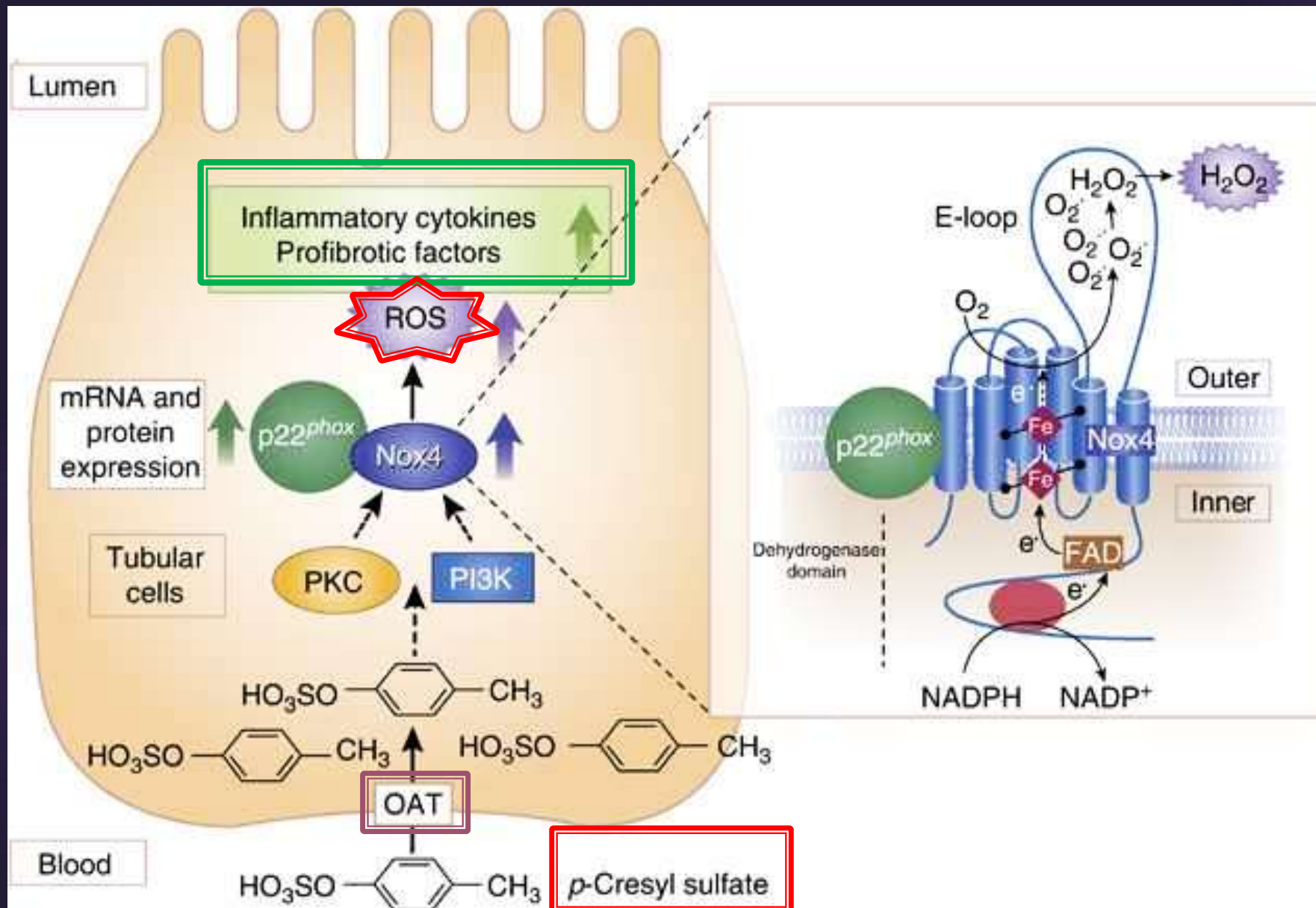
PB Uremic Toxins

Gut feeling and Retention in uremics  
the marker of inadequate HD therapy



The Protein  
Bound Uremic  
Toxins  
Removed By  
Tubules not By  
filtration !



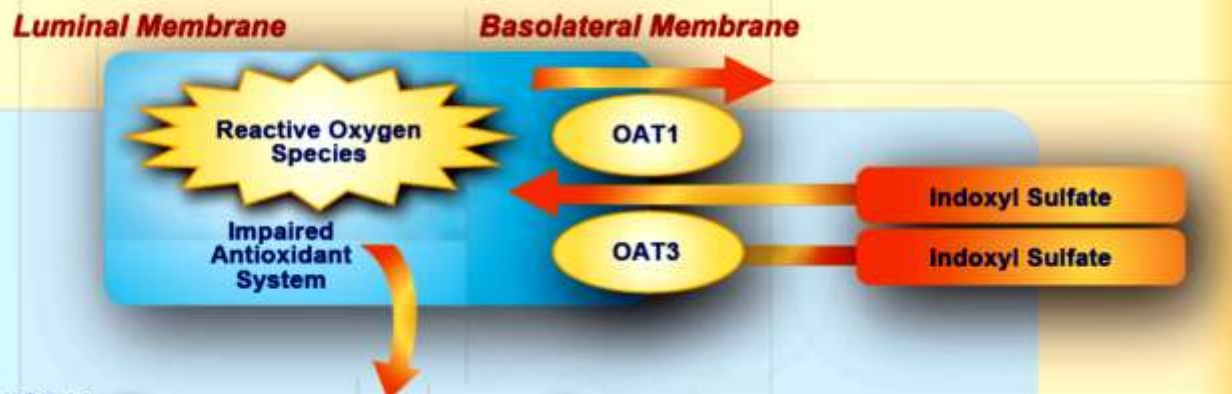
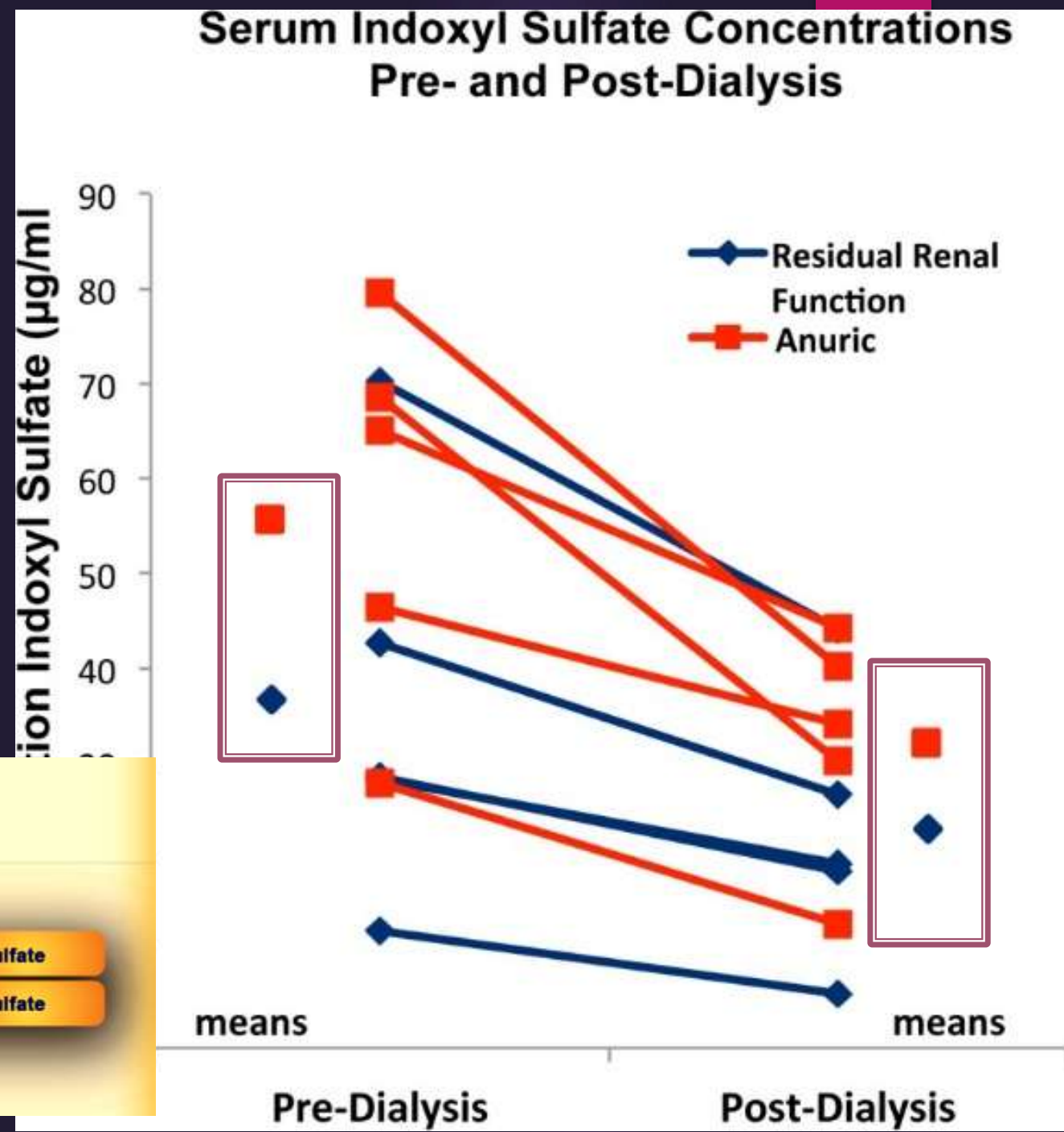


PB Toxins  
 ↑ ROS  
 Through  
 NOX4 of  
 NADPH  
 oxidase

# Indoxyl Sulfate

IS level is better in patients with  
Residual Renal Functions  
( Tubular Organic Anion Transporter )  
OATs

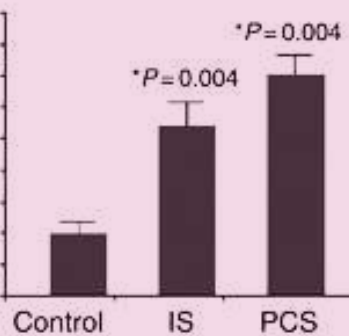
PLoS One v.10(3); 2015





**a**

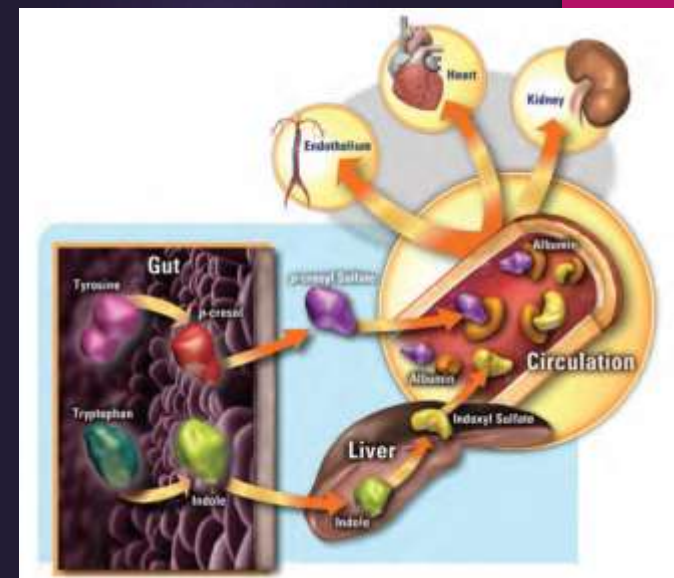
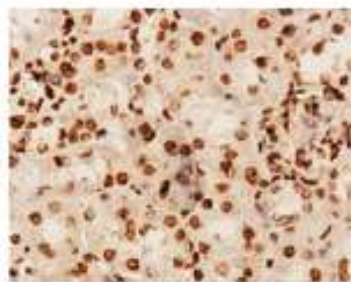
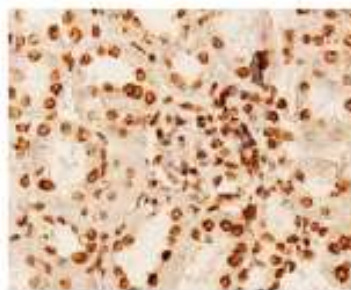
Relative DNMT 1/actin  
ratio



Control

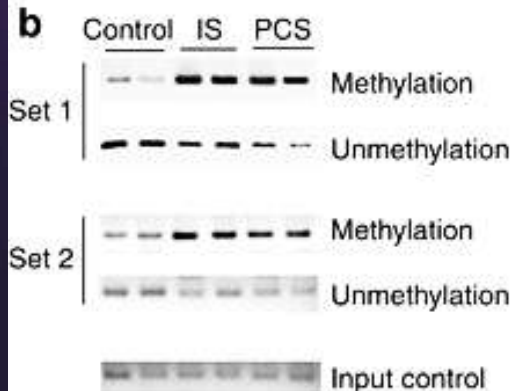
IS

PCS

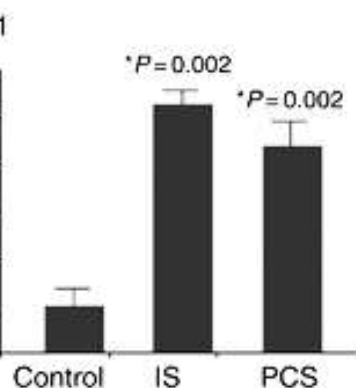


Indoxyl sulfate (IS)- and p-cresyl sulfate (PCS)-injected mice had increased DNA methyltransferase 1 (DNMT 1) expression and DNA hypermethylation of the Klotho gene

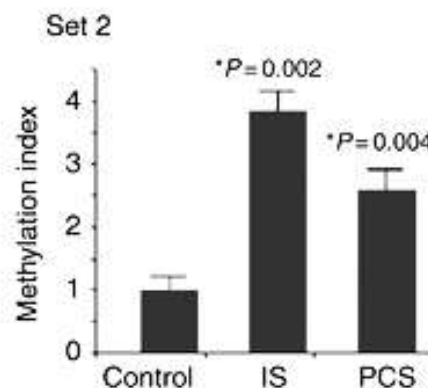
Kidney International (2012) 81, 640–650

**b**

Set 1  
Methylation index



Set 2  
Methylation index

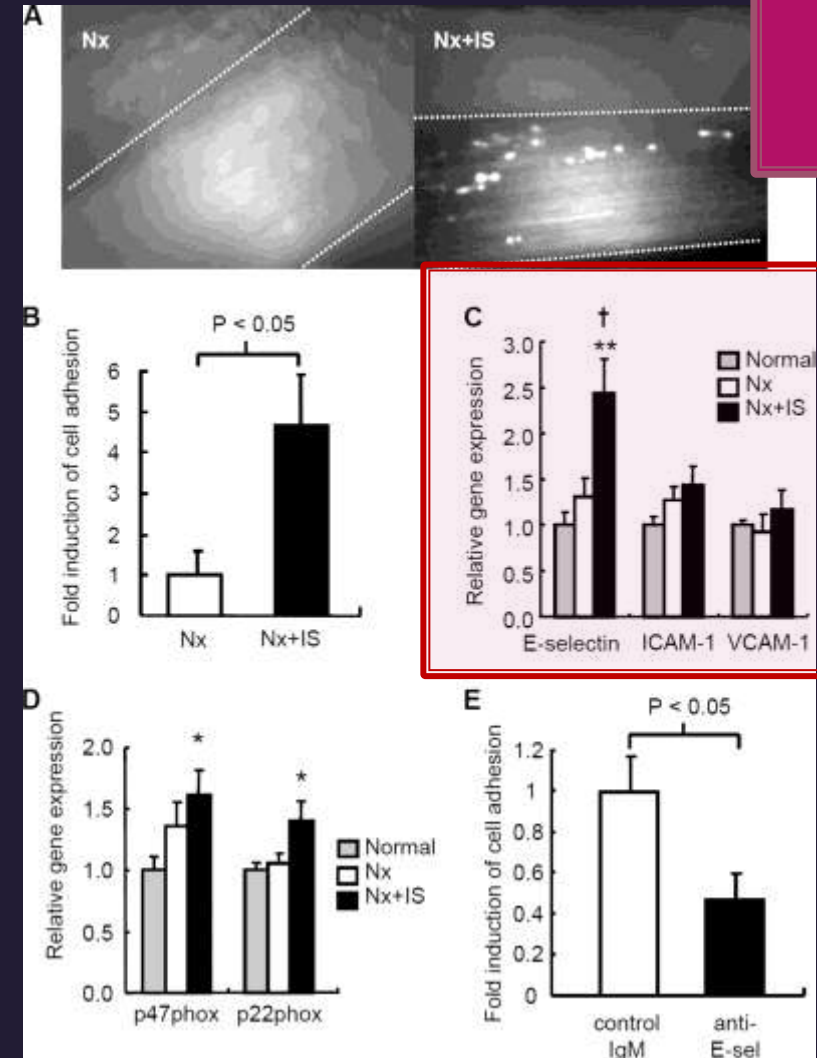
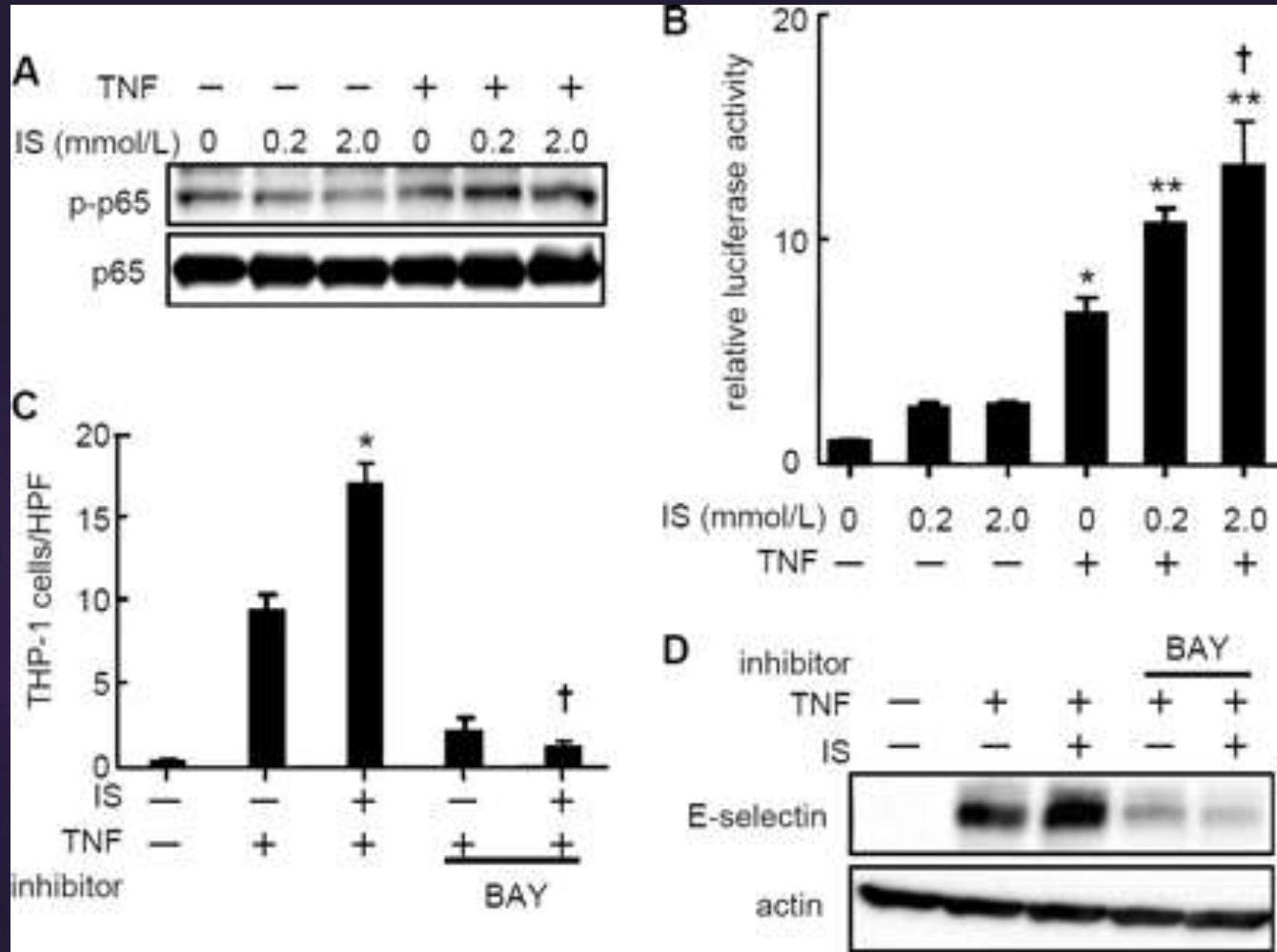




# Indoxyl Sulfate Induces Leukocyte-Endothelial Interactions through Up-regulation of E-selectin , ICAM , VCAM and TNF $\alpha$

Journal of Biological Chemistry ,Dec 2010

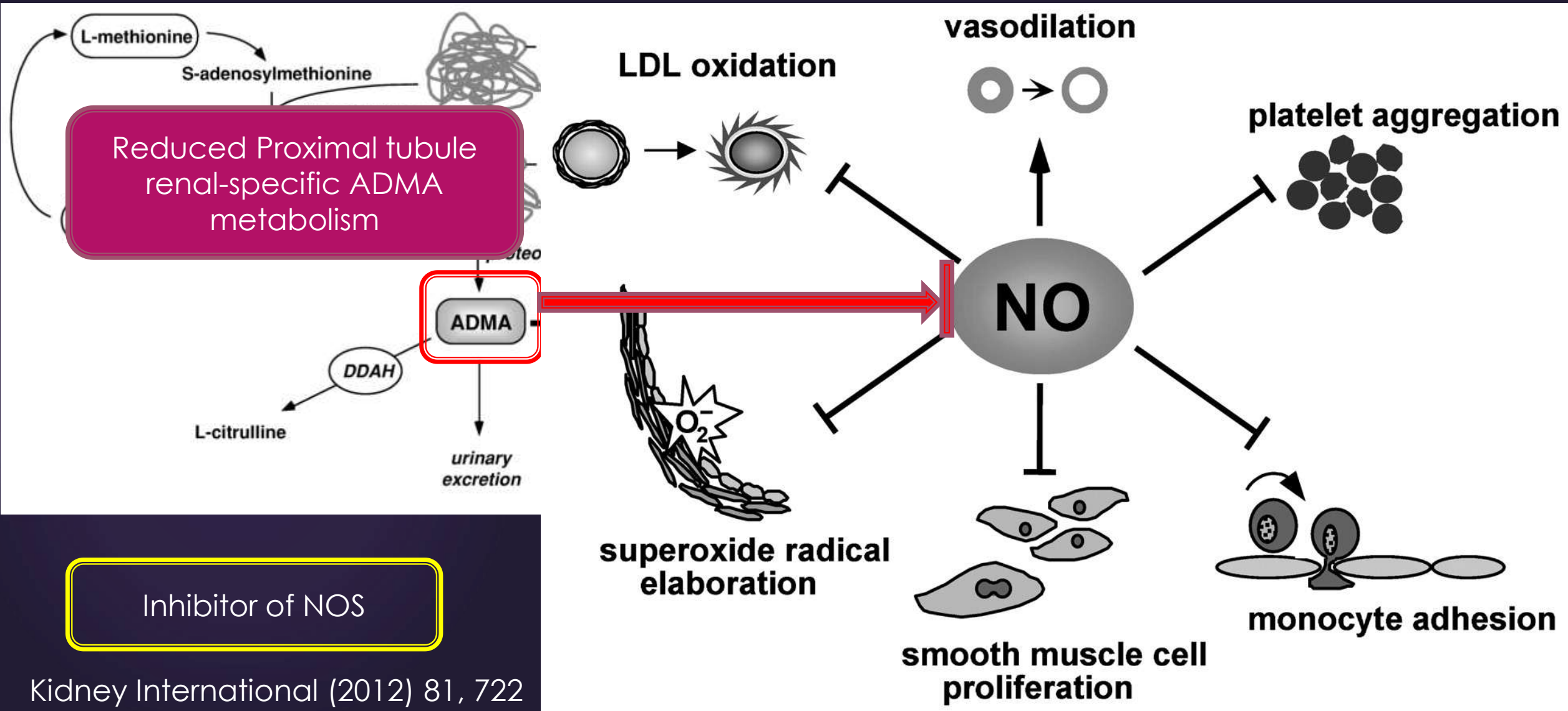
Nx: only water  
Nx IS : IS



Effects of indoxyl sulfate on the TNF- $\alpha$ -induced NF- $\kappa$ B pathway

# ADMA : PB Toxins Retention

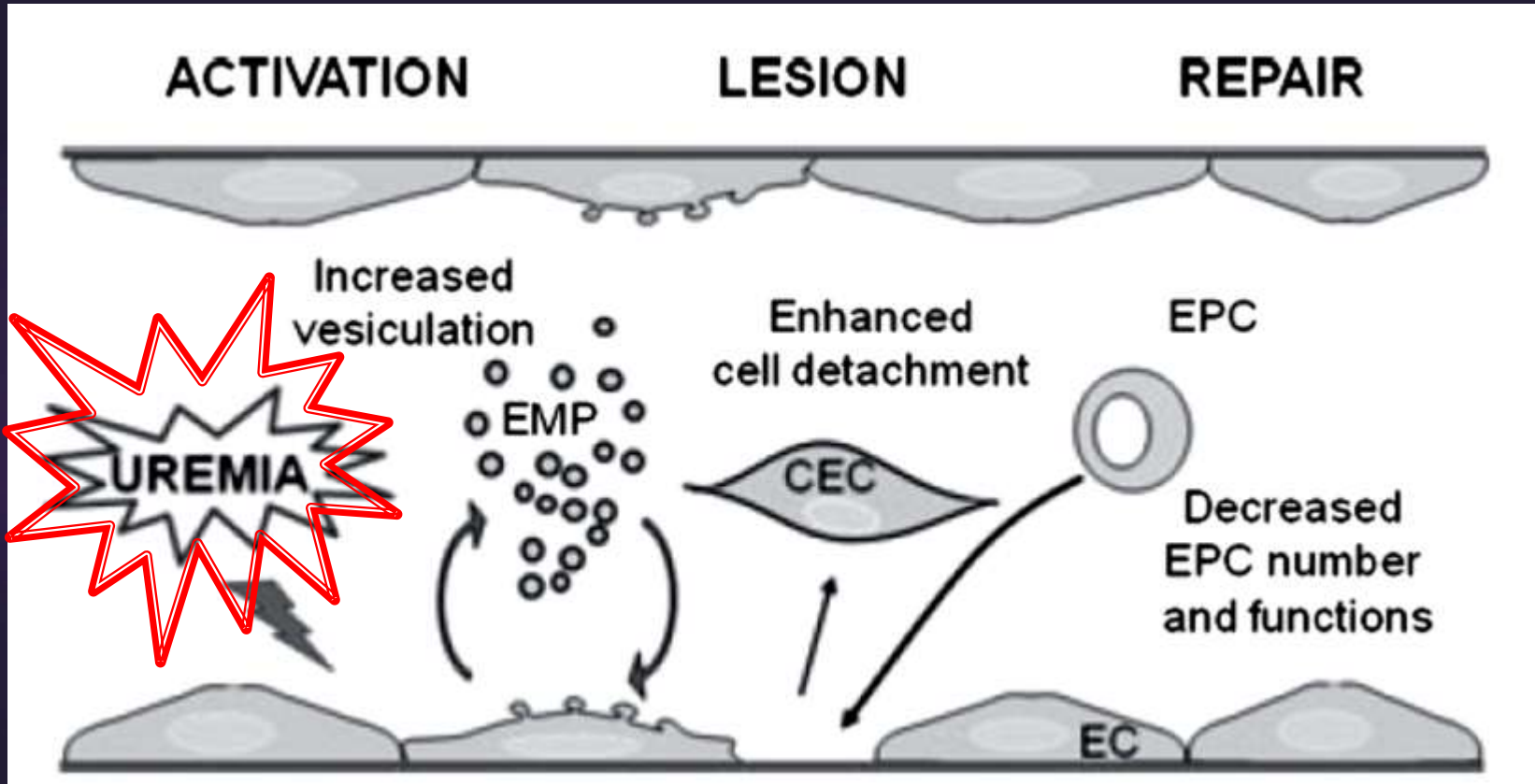
J Am Soc Nephrol. 2015 Apr



# Circulating Endothelial Cells (CES)

BioMed Research International Volume 2014

► CEC counts are increased in diseases associated with a high degree of endothelial cell activation and/or injury



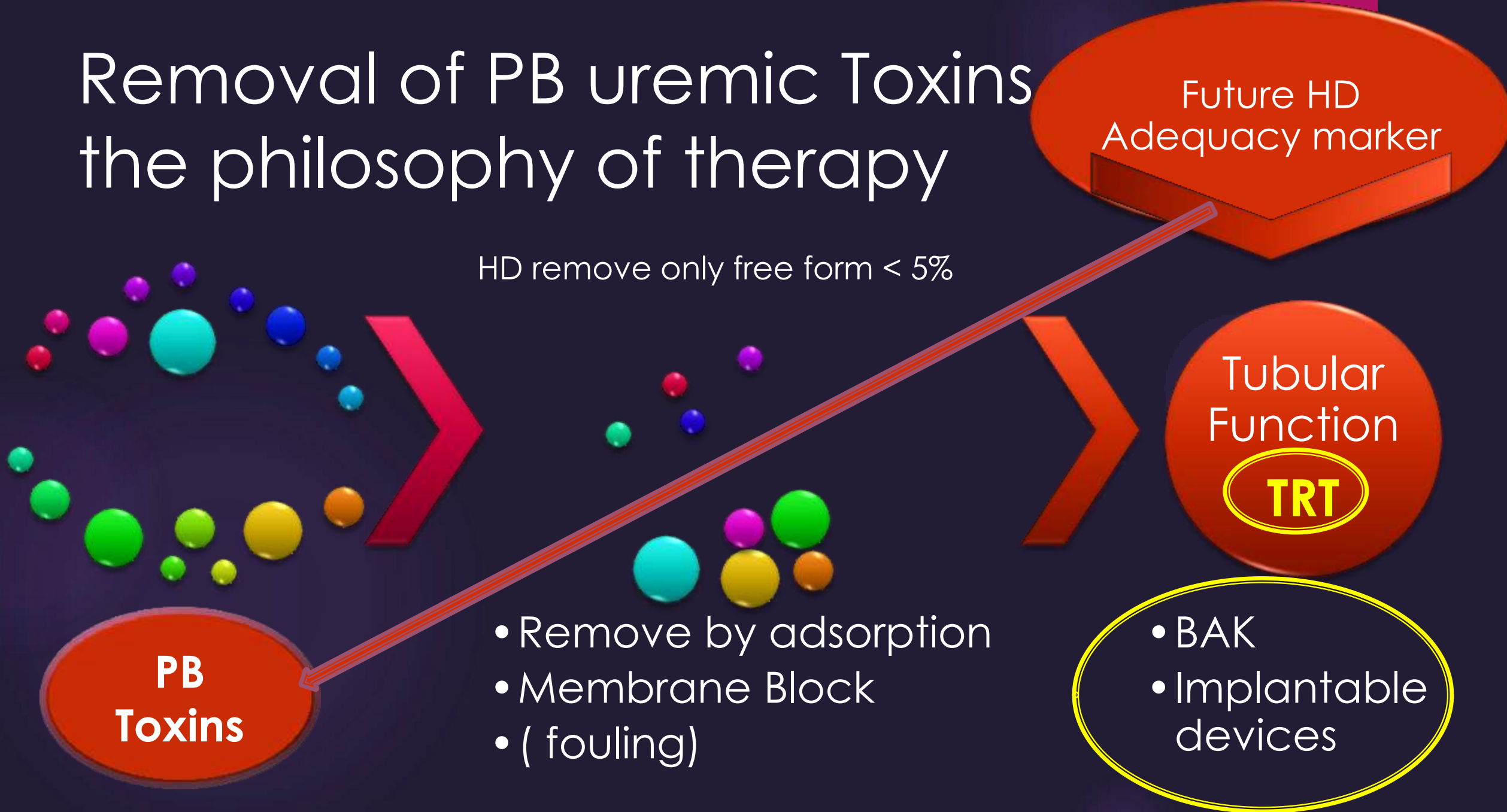
(1) Uremia induces the release of endothelial microparticles (EMP)

(2) increase in circulating endothelial cells (CEC)

(3) uremia impairs the survival of endothelial progenitor cells (EPC)

combination of different surface antigens such as CD146, CD45, and CD31 to detect the endothelial cells

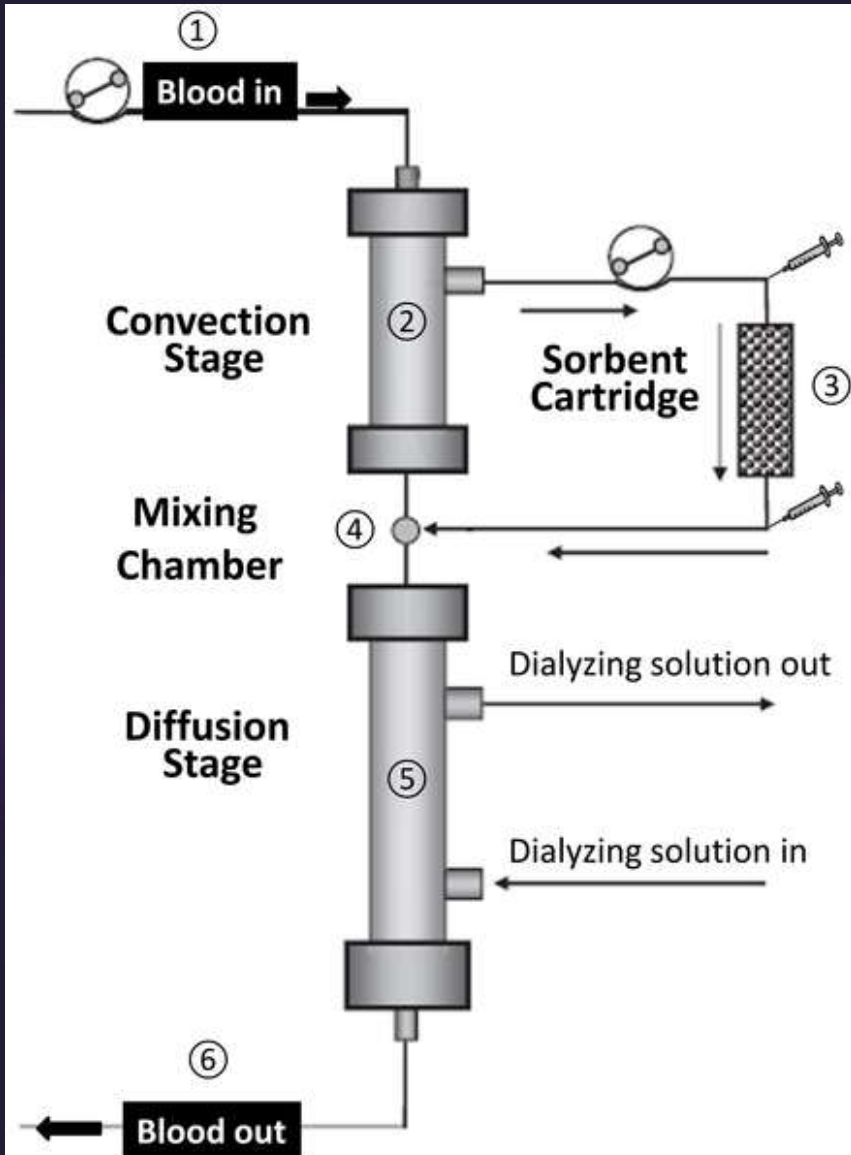
# Removal of PB uremic Toxins the philosophy of therapy





# Towards Adsorption Techniques

plosone.org April 2014 | Volume 9



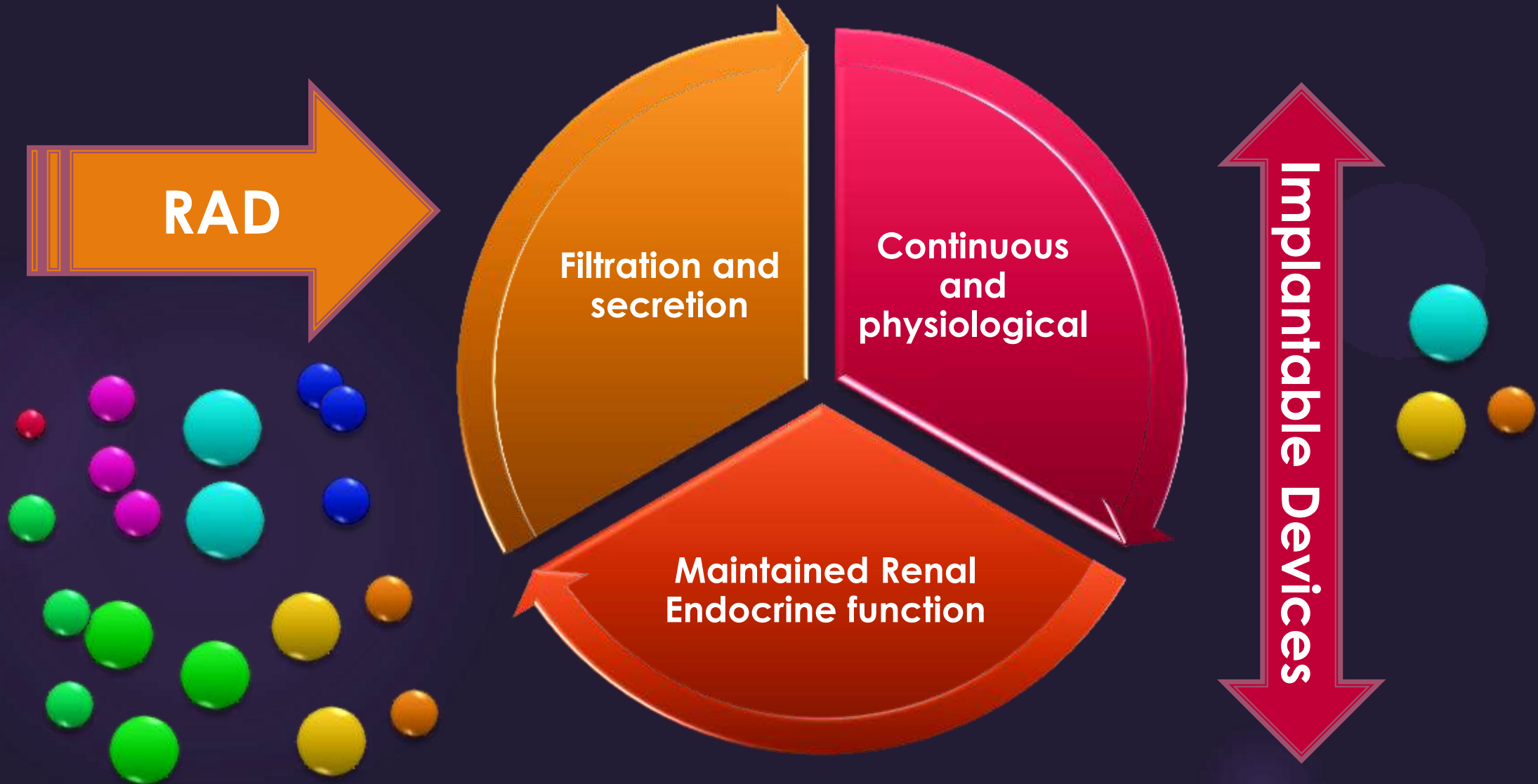
Albumin sieving coefficient of 0.02.



the use of an adsorber in combination with dialysis membranes may be a new therapeutic option to increase the removal rate of these uremic toxins

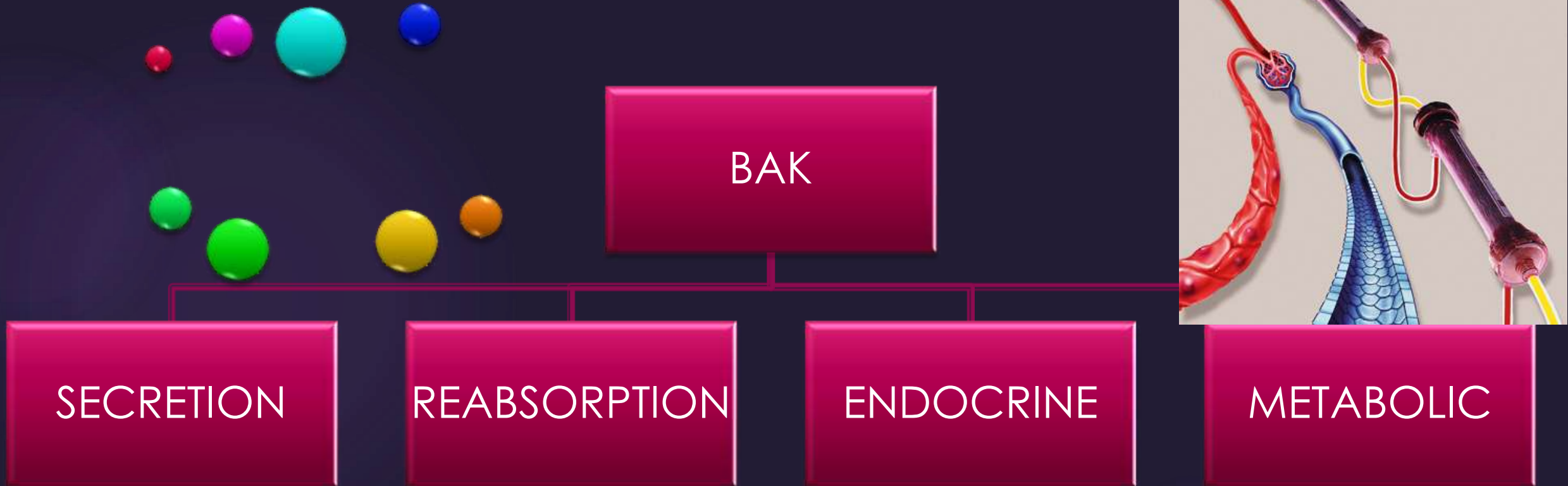
Artificial Organs Volume 37, Issue 4, pages 409–416, April 2013

# The Future Towards

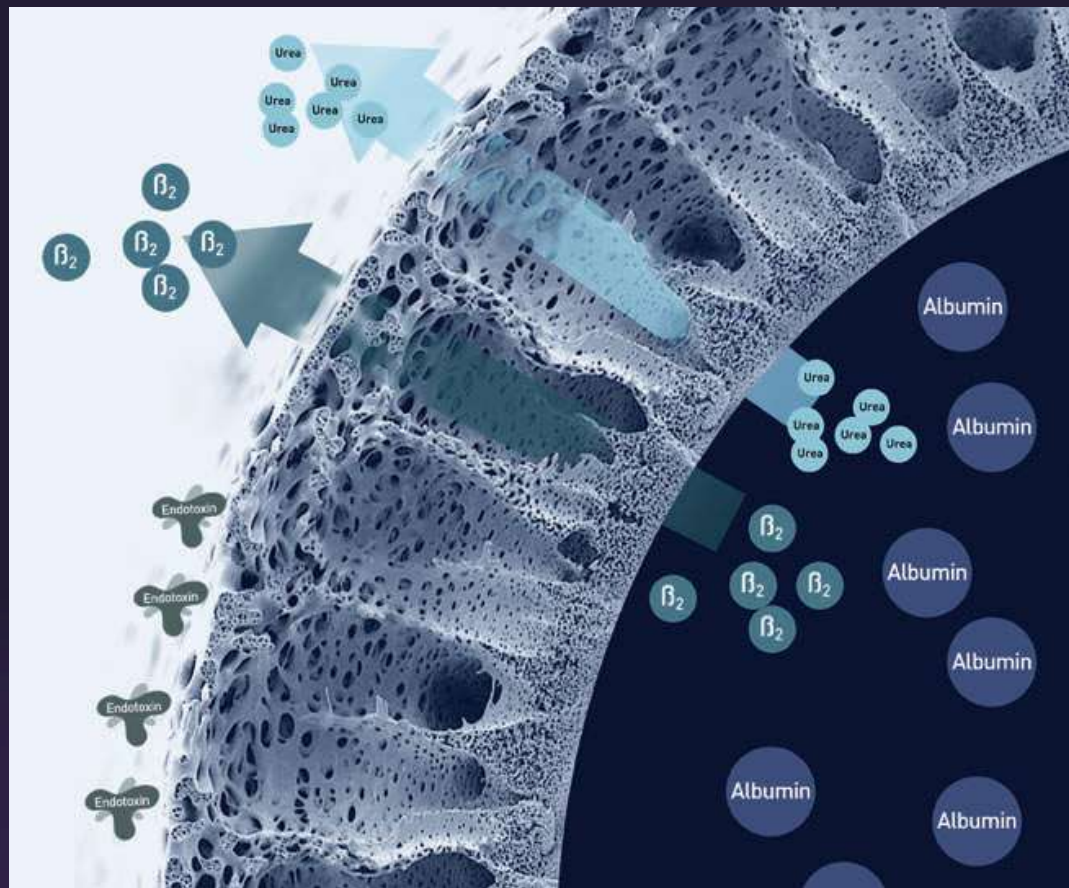


# BAK : The theory and the promise!

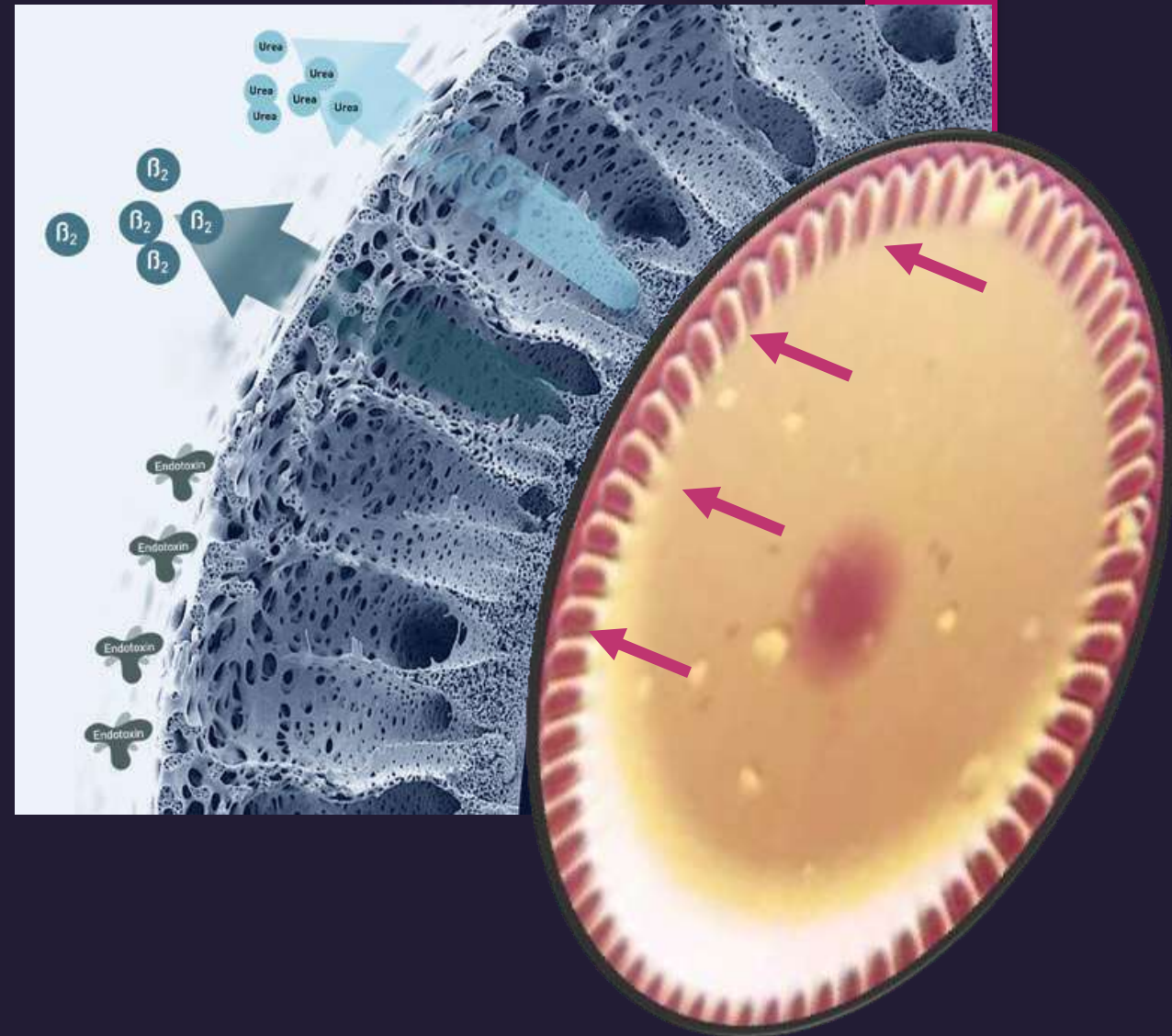
- ▶ placing renal tubule cells, primary cells or cell lines established from various species, on the inner surface of hollow fibers.







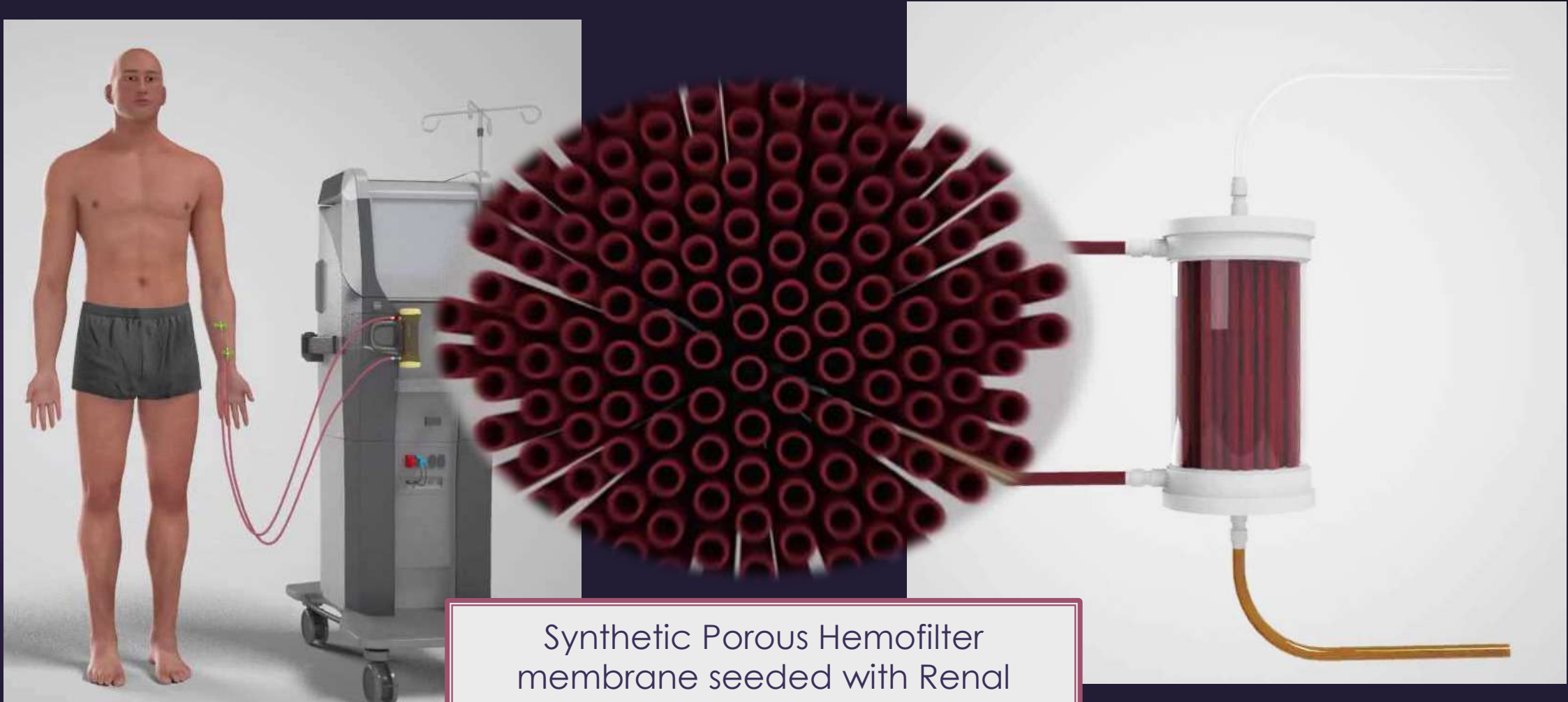
**Filtration**



**RAD : Filtration  
Secretion**



# BAK : The theory and the promise!



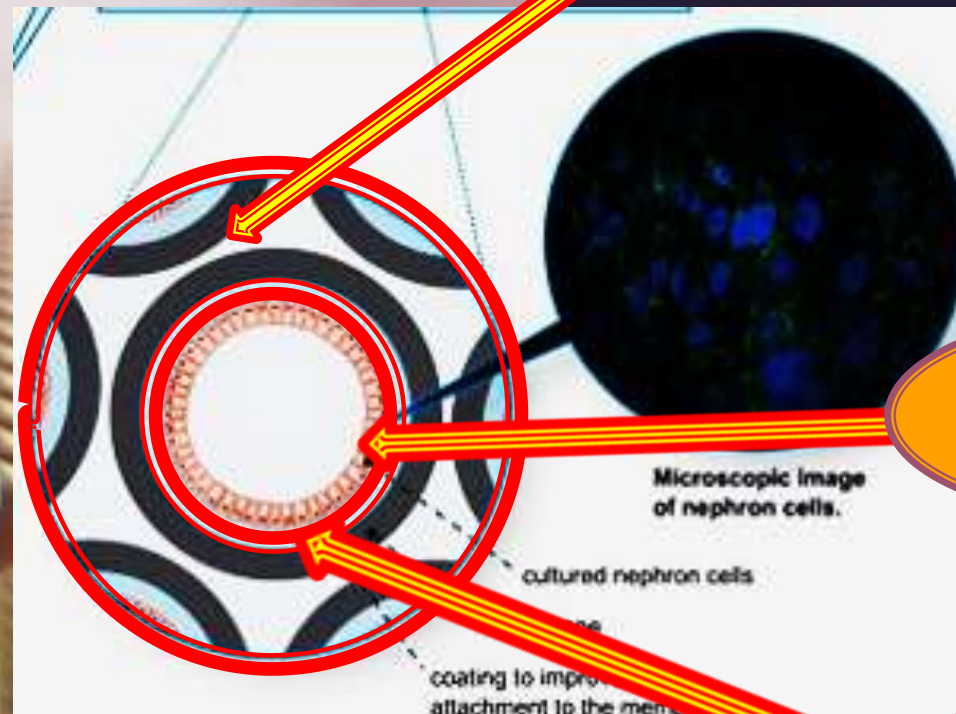
Synthetic Porous Hemofilter  
membrane seeded with Renal  
Tubule cells

# PB Toxins

Hemofilter  
Membrane

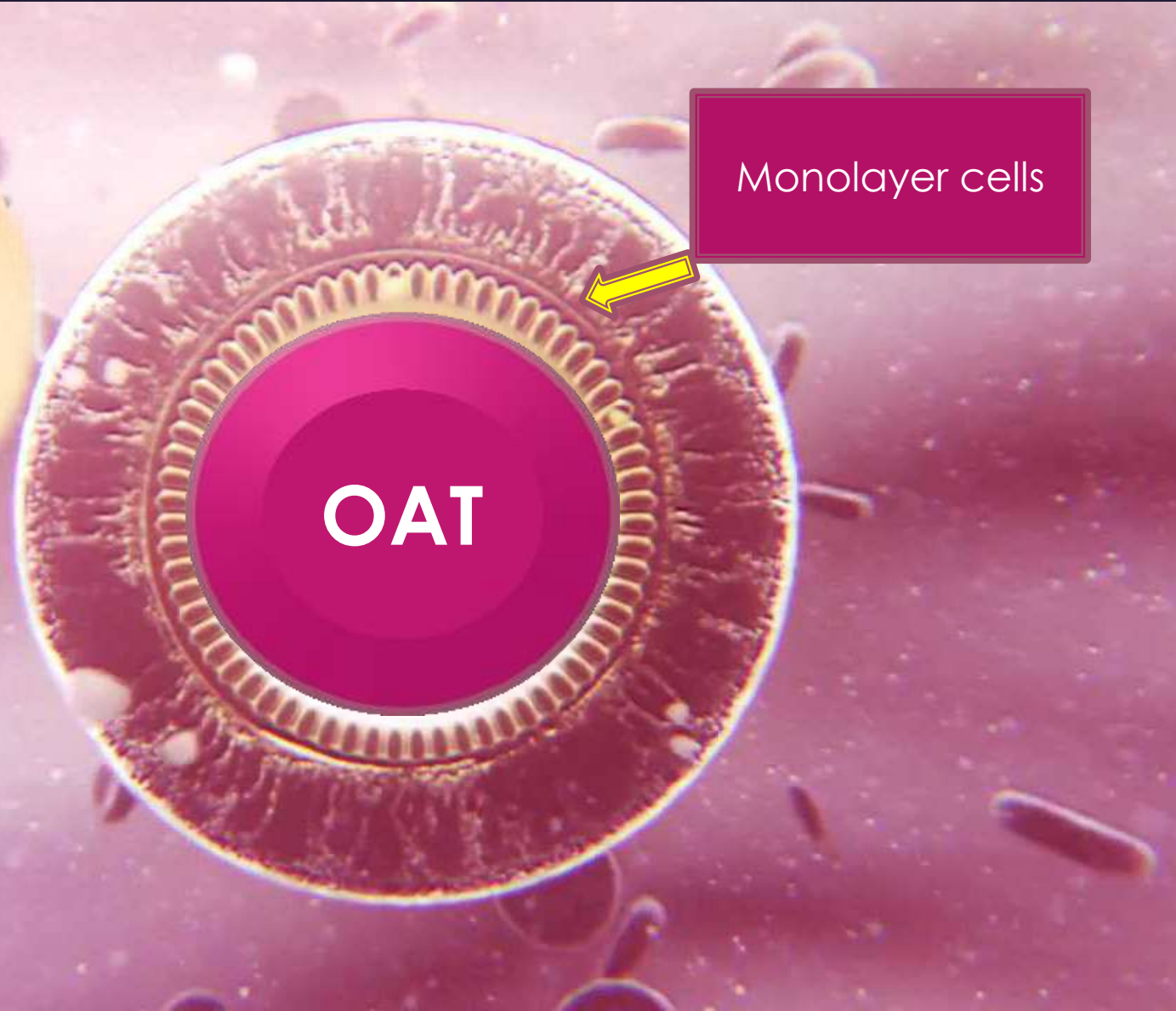
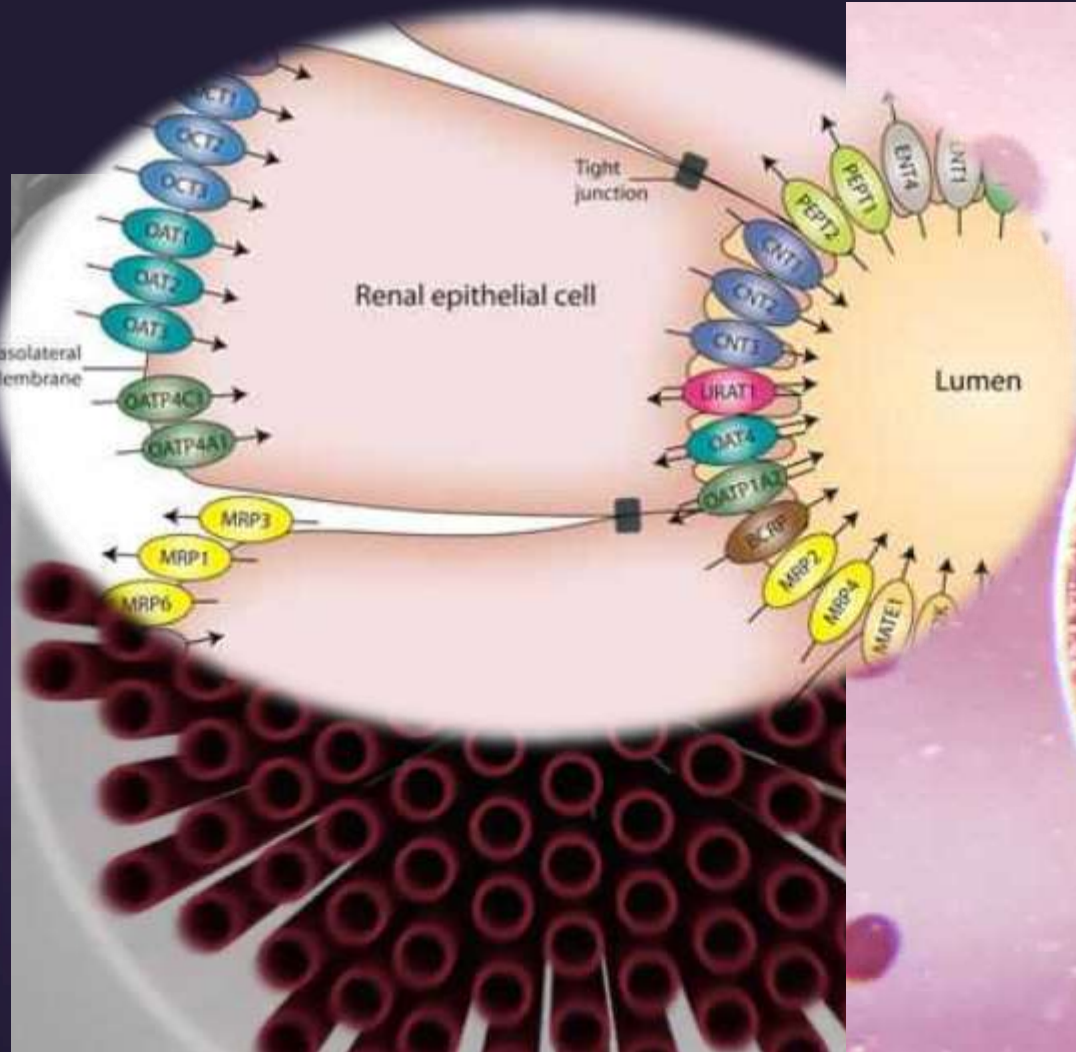
Monolayer  
With Tight  
Junctions

Surface  
coating





# BAK : The theory and the promise

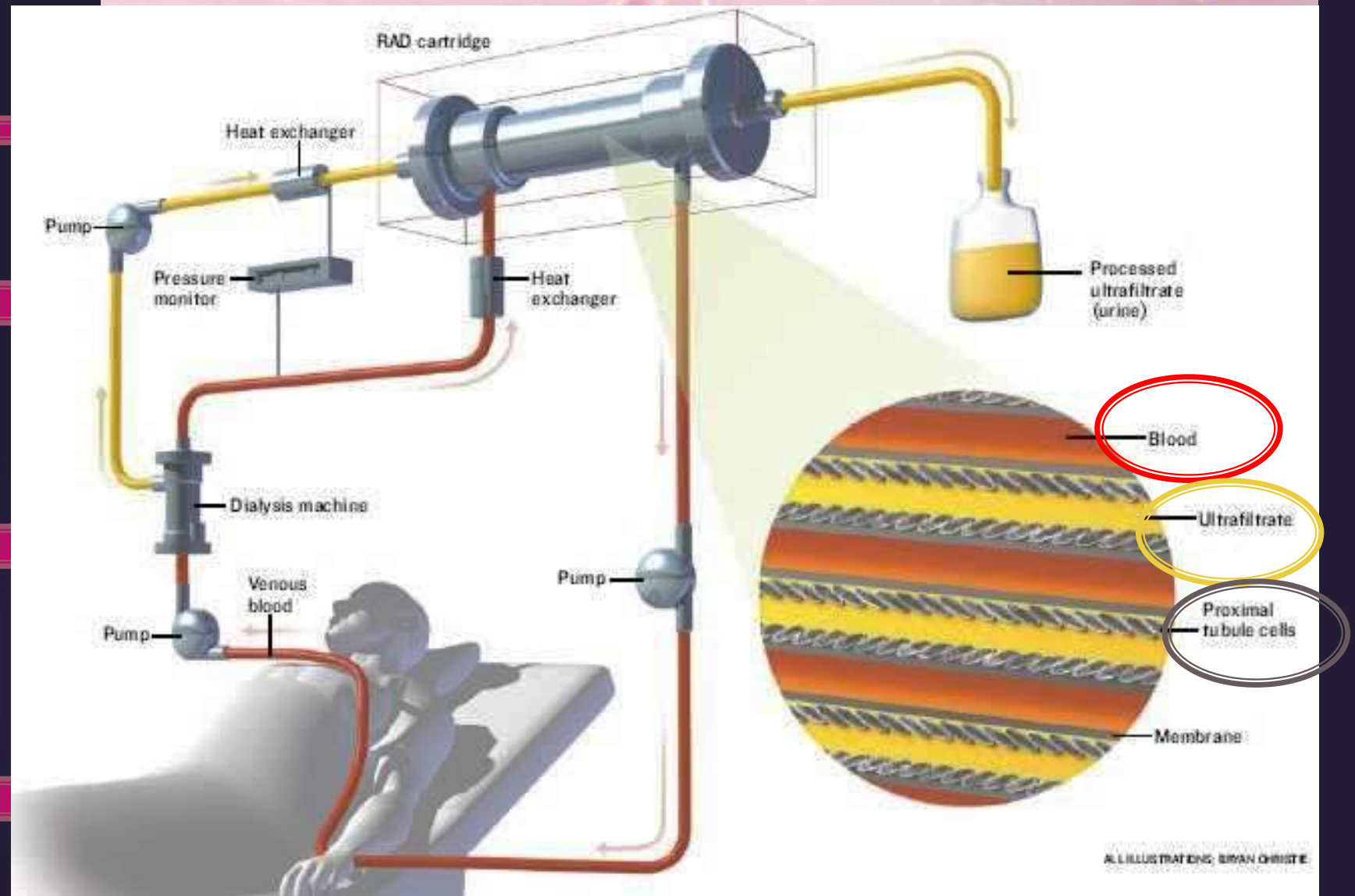


Blood Flow

Outer  
membrane layer  
1  $\mu\text{m}$  pores

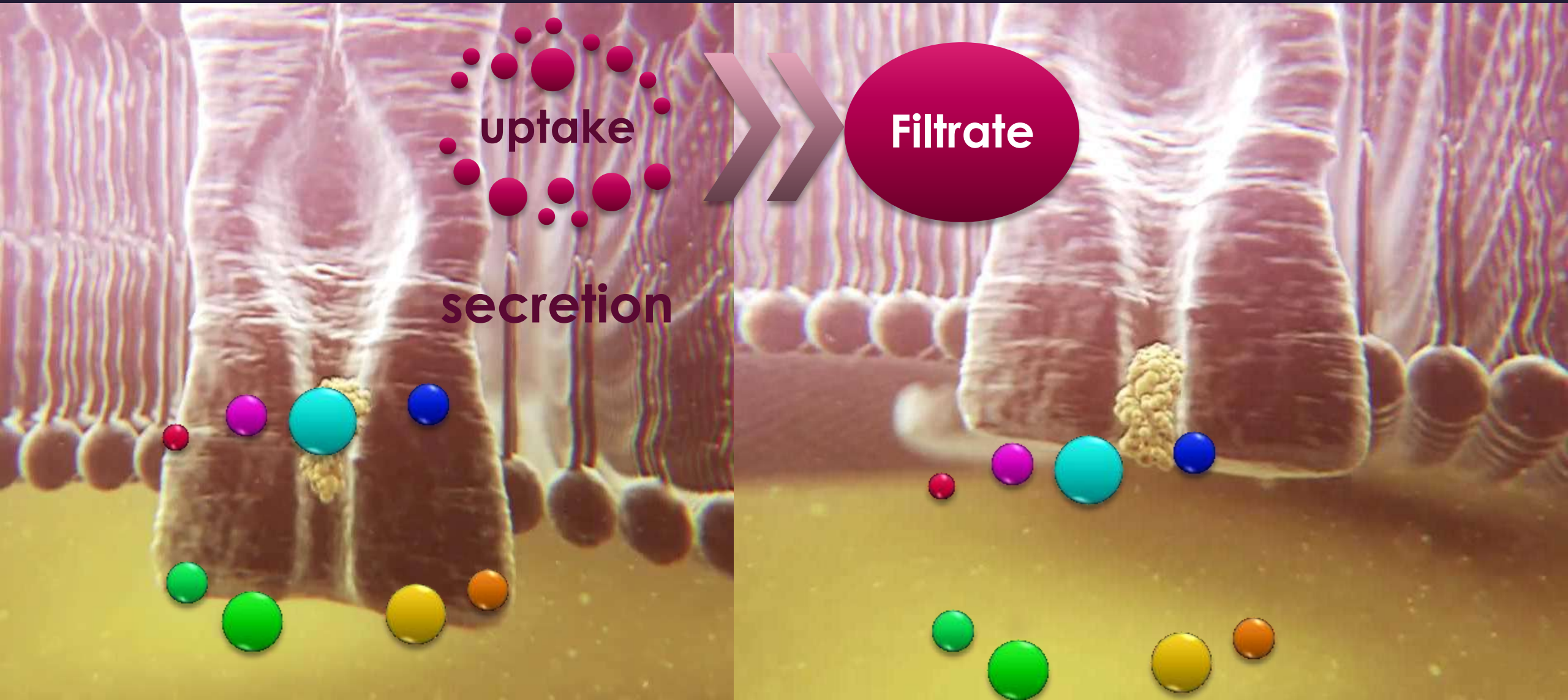
Filtrate flow for  
Reabsorption

Outer layer  
clogging by  
proteins and  
cells

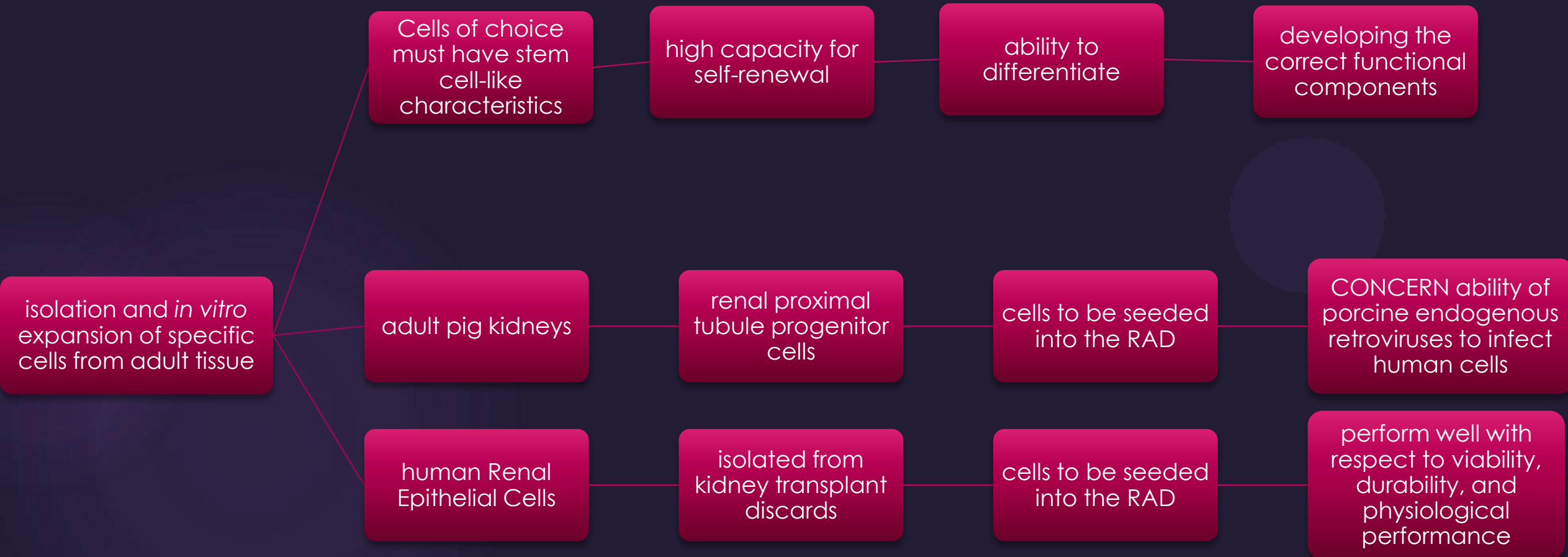




# BAK : The theory and the promise



# Challenge: tissue source and supply



Humes et al Kidney Int. 1999; 55: 2502–2514

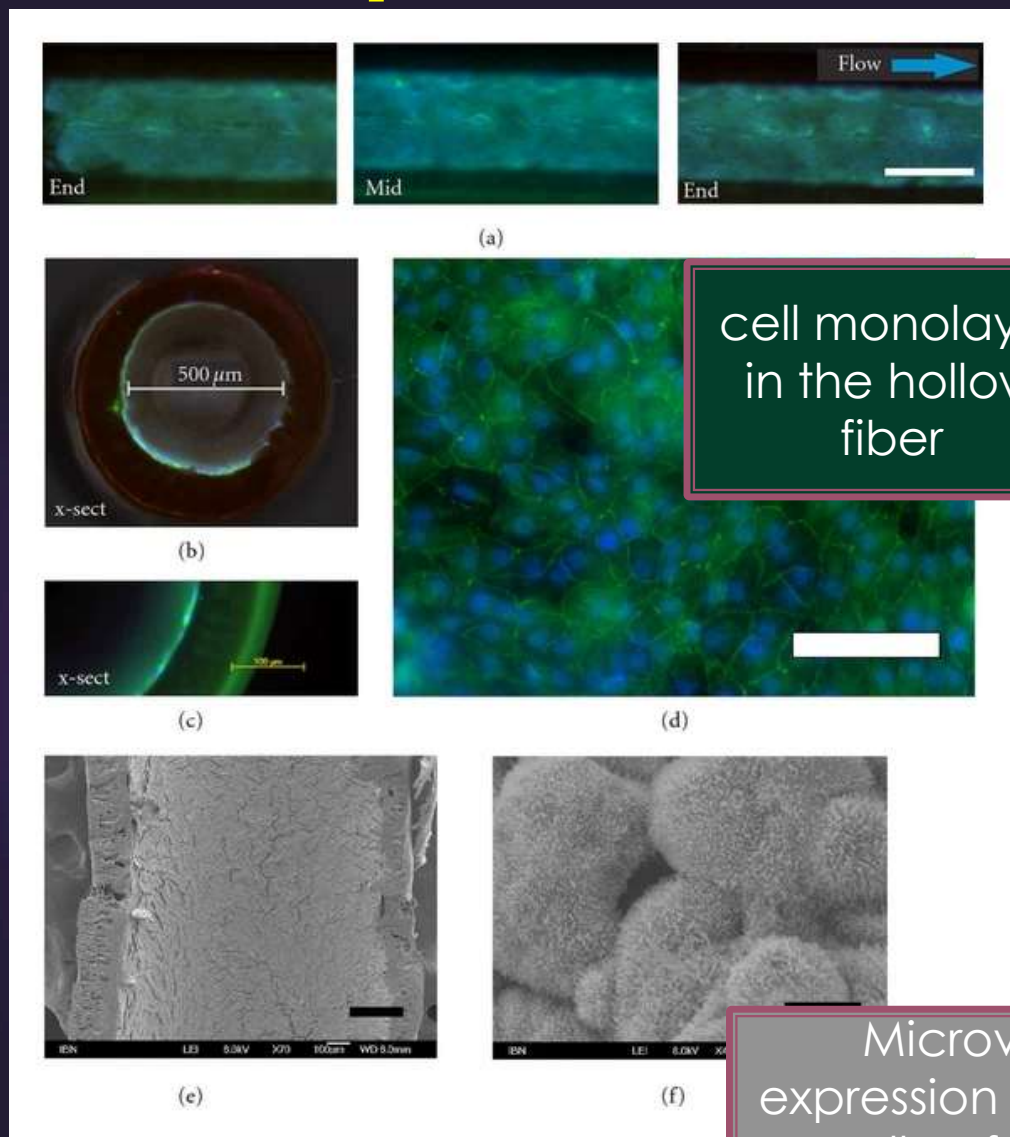
Buffington et al, Cell Med. 2012; 4:

Paradis et al ,Science. 1999; 285: 1236

Westover et al ,J Tissue Eng Regen Med. 2012; 6

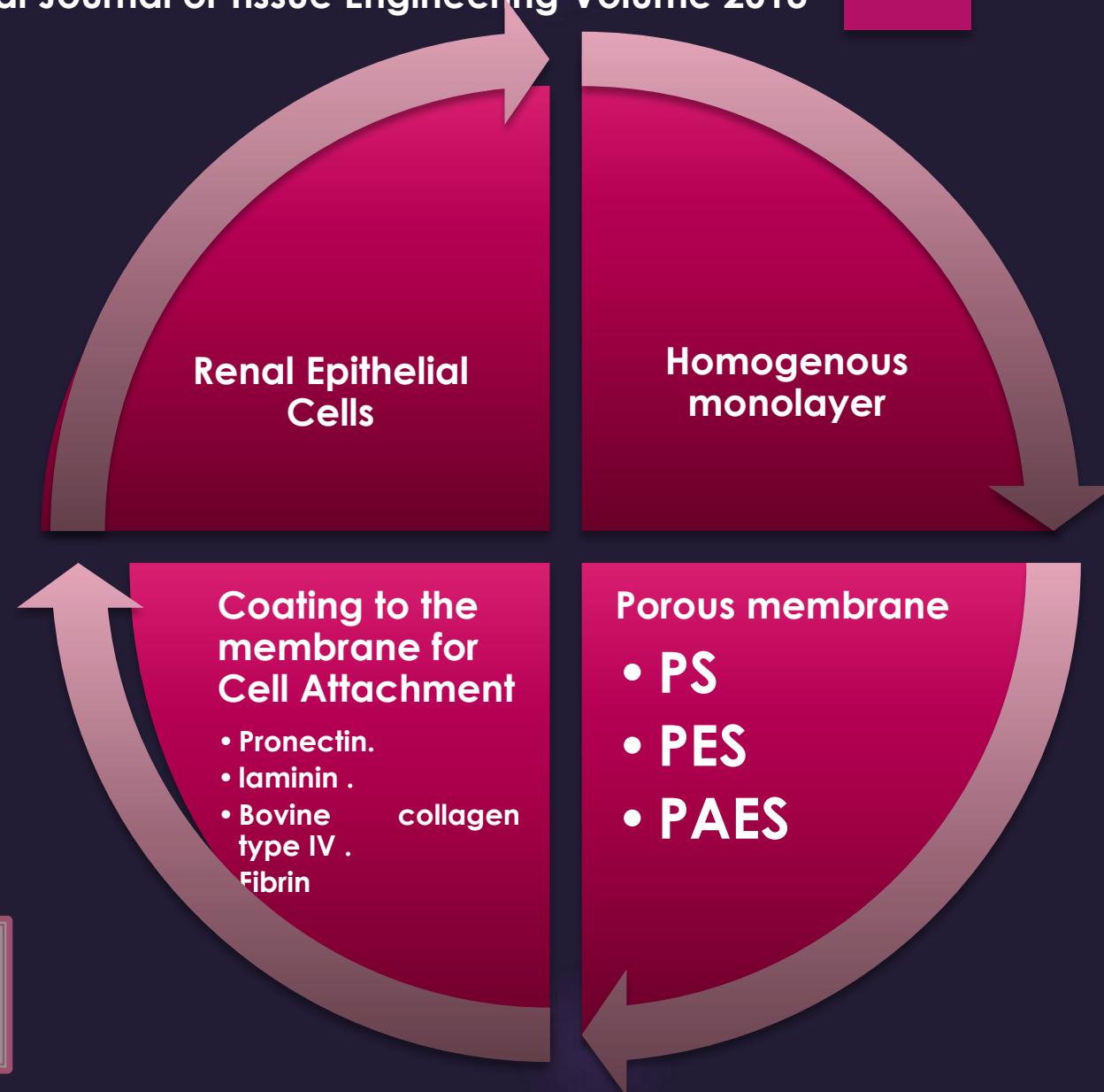
# BAK requirements

International Journal of Tissue Engineering Volume 2013

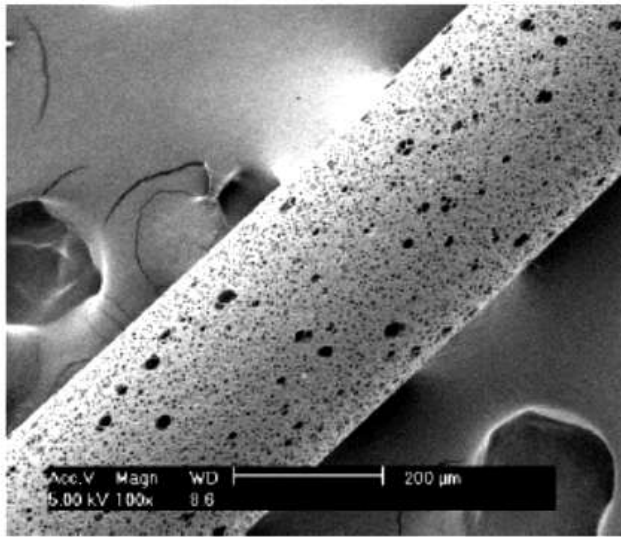


cell monolayer  
in the hollow  
fiber

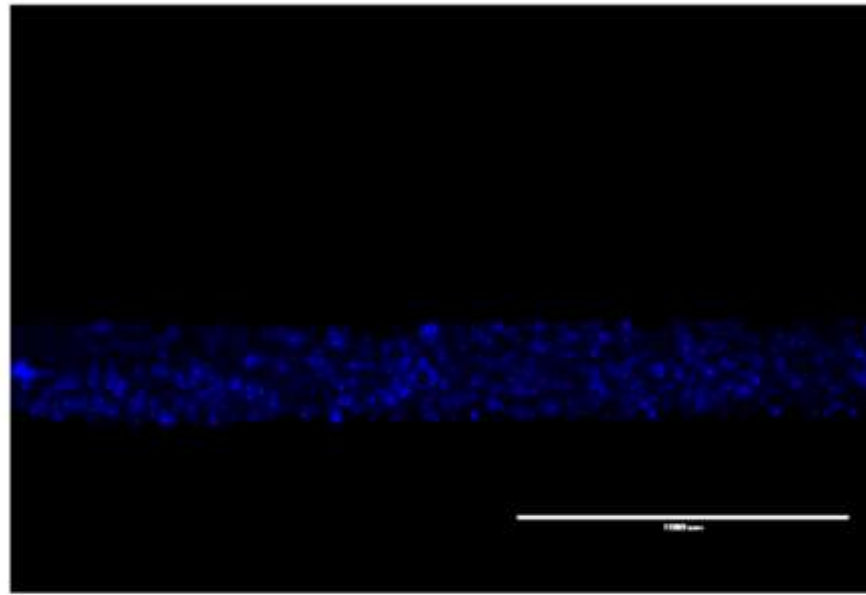
Microvilli  
expression on the  
cell surface



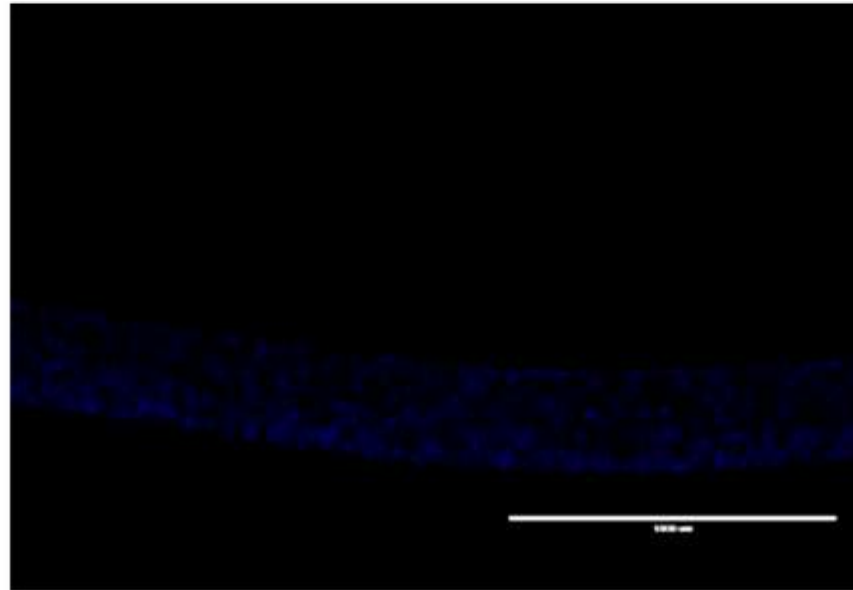
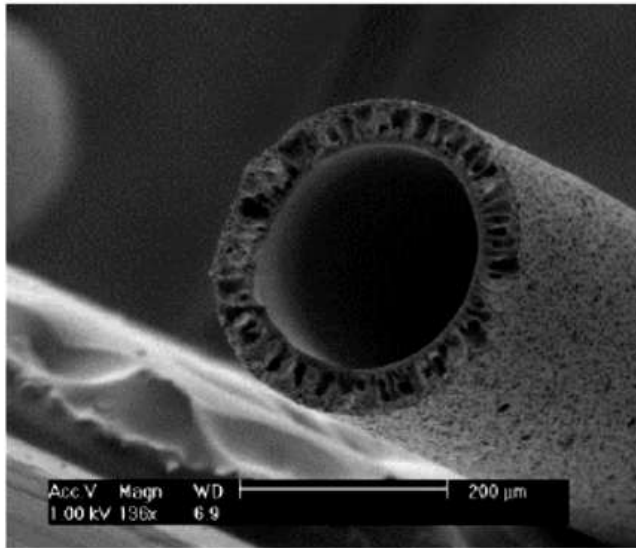
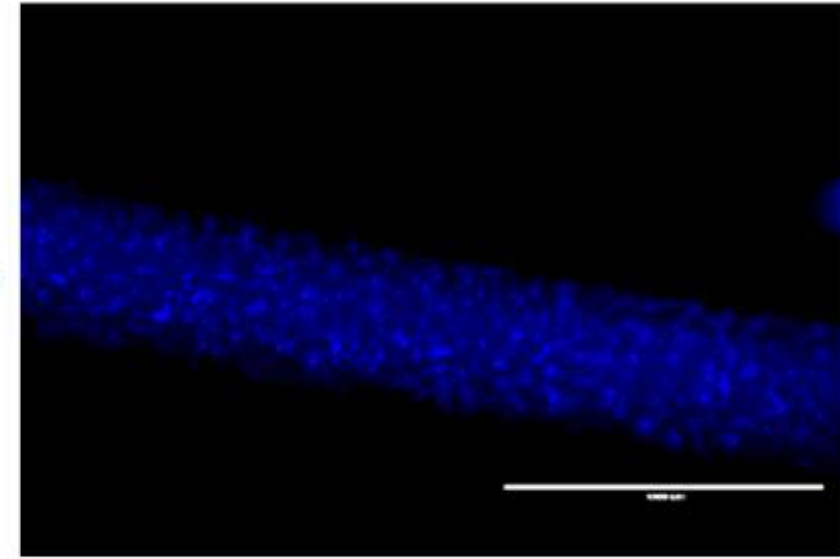




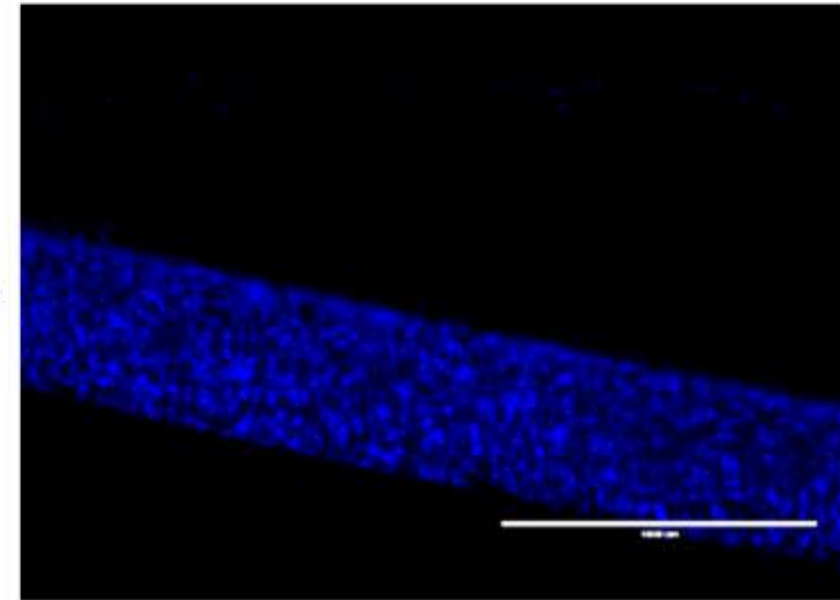
a



a

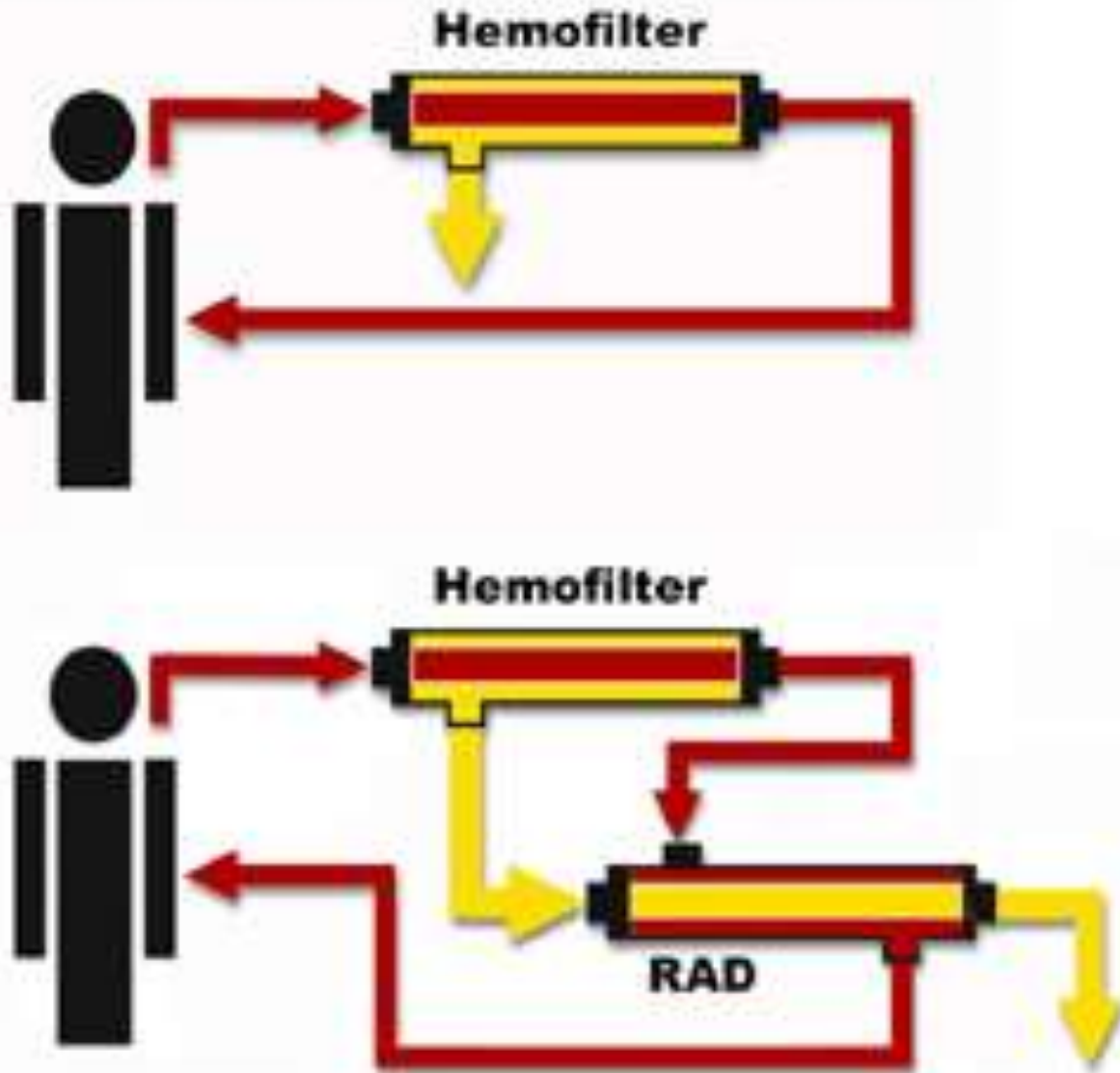


c

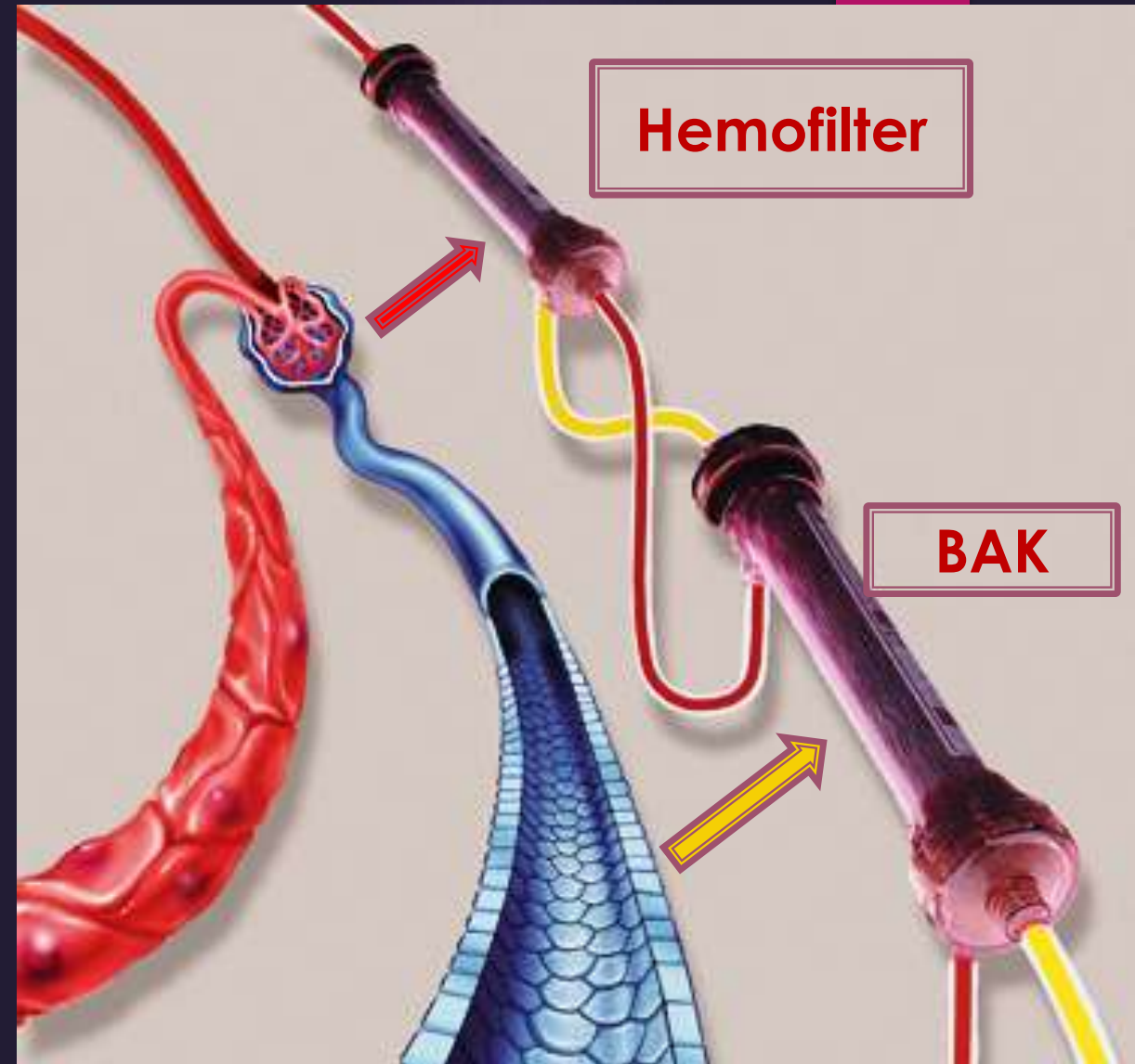


DAPI fluorescent staining for the nuclei of cells attached to the surface of HCO

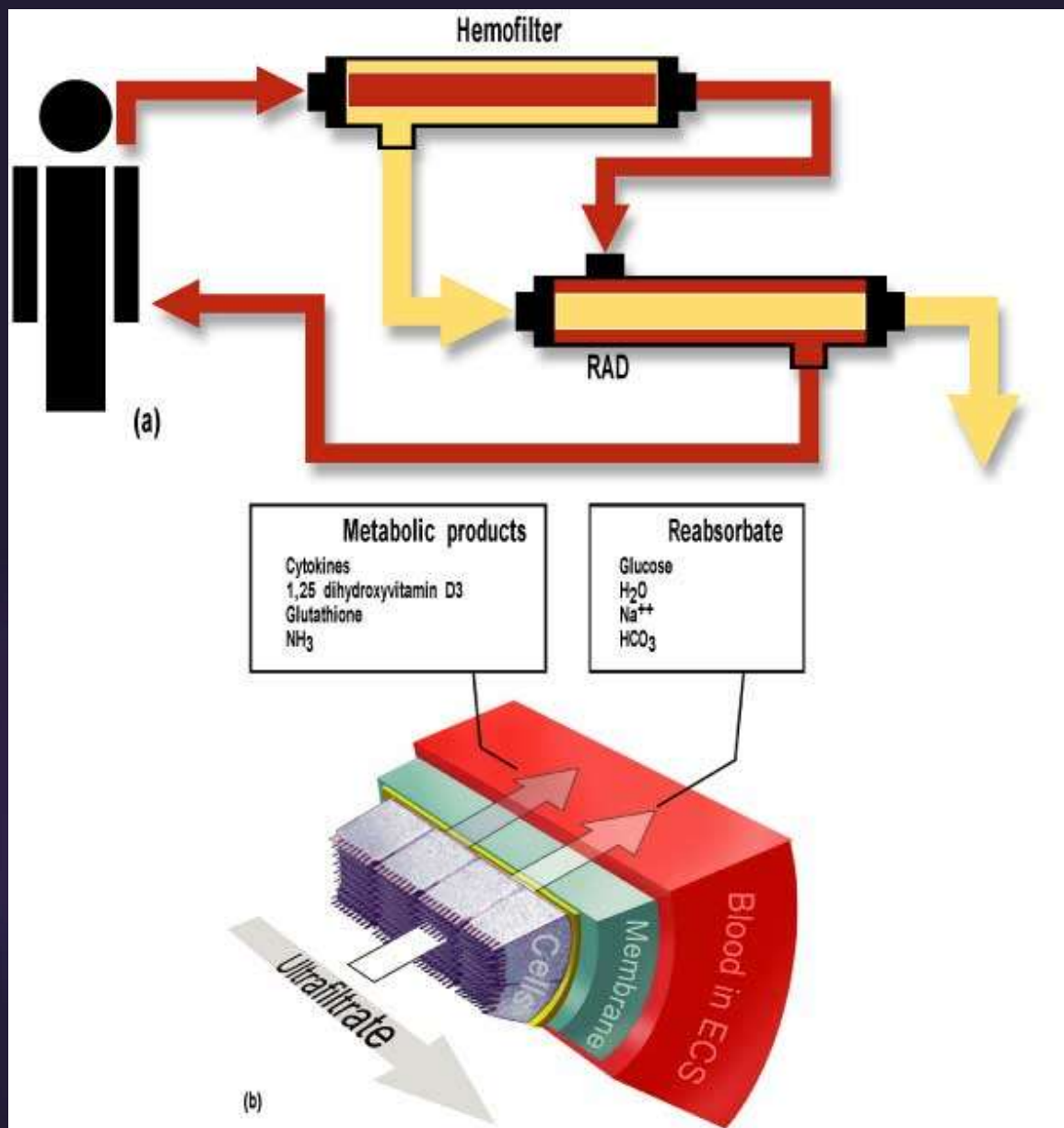




Conventional treatment vs. BAK



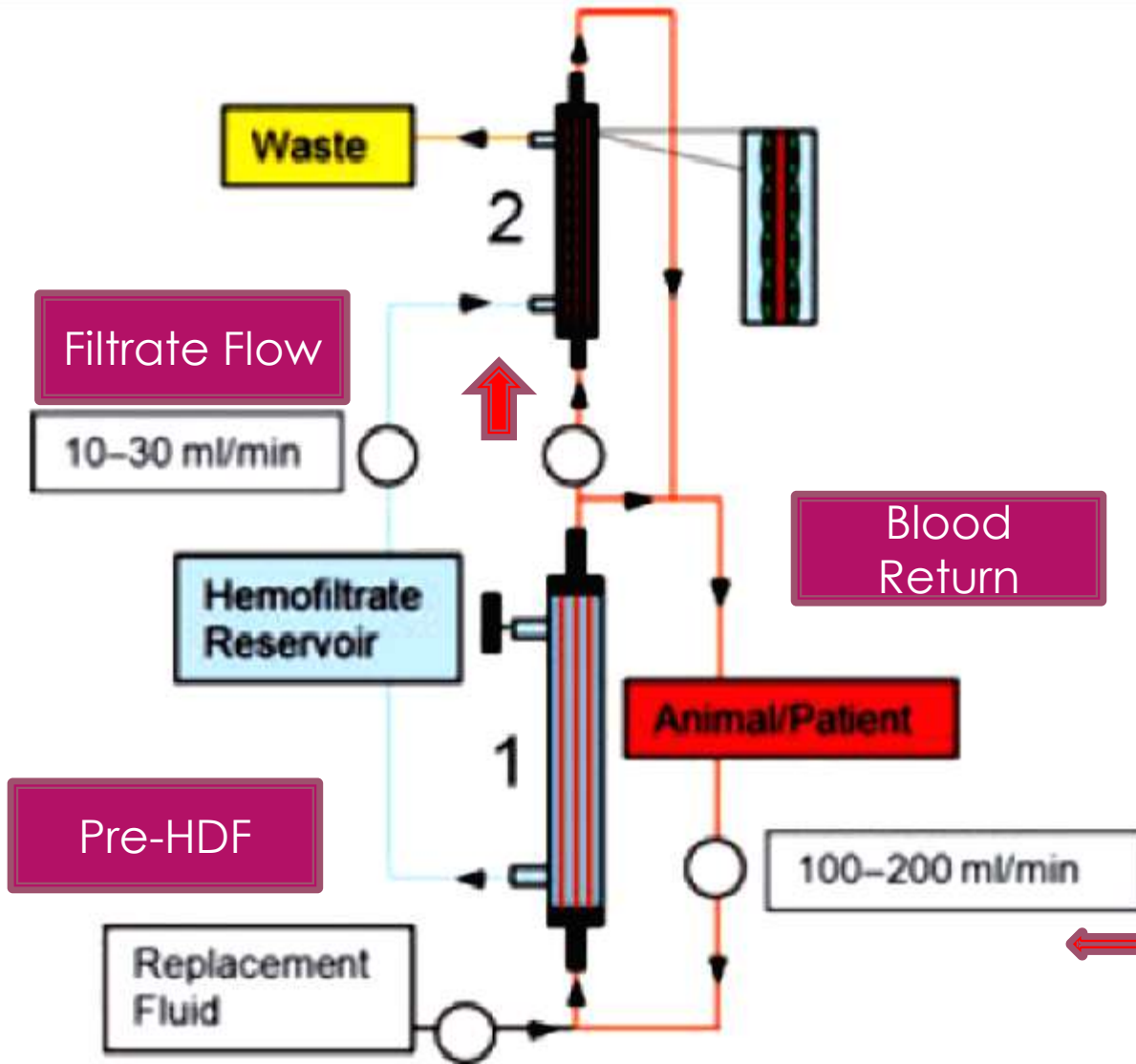
Natural kidney function vs. BAK



The renal tubule cell assist device (RAD) is an extracorporeal device with a standard hemofiltration cartridge covered by nonautologous human renal tubular cells along the inner surface

Journal of the American Society of Nephrology, 2008  
19, 1034

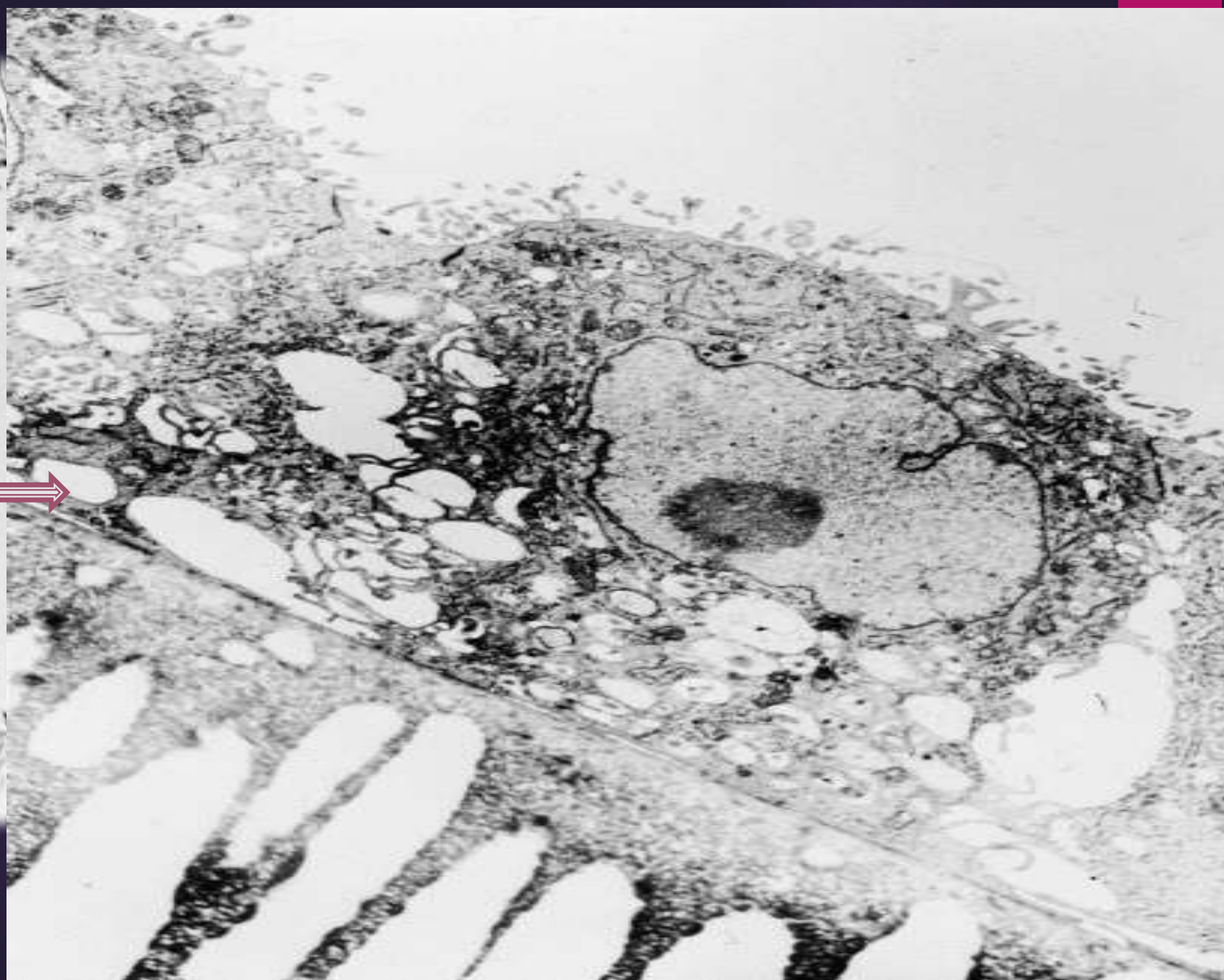
1. This RAD, developed at the University of Michigan and Nephros Therapeutics, improves a conventional kidney dialysis machine's role by returning useful substances, typically removed by the dialysis machine, to the bloodstream (a). For filtering purposes, the RAD makes use of reabsorbate and metabolic material (b).



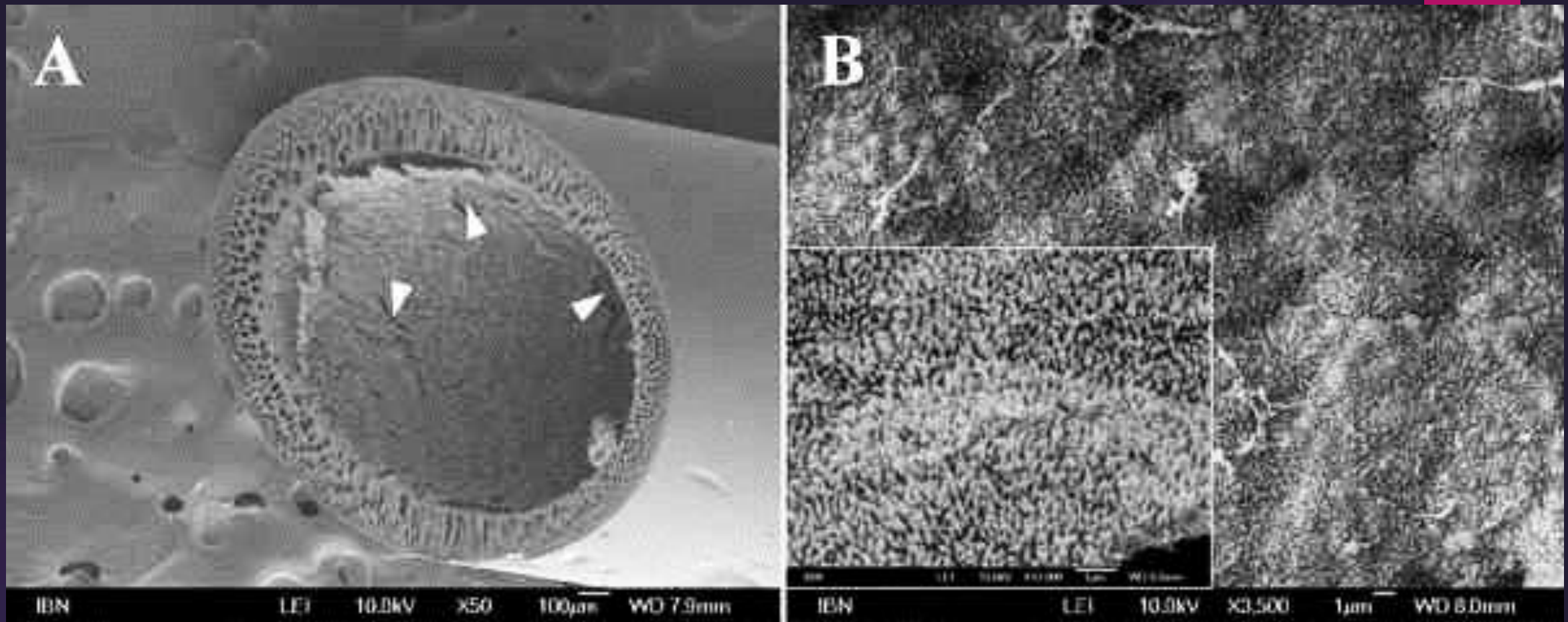
HPTC grow in the bioreactor on the outer surfaces of the HFM, where they are exposed to the haemofiltrate. The blood flows in the lumina of the HFM

A novel design of bioartificial kidneys with improved cell performance and haemocompatibility

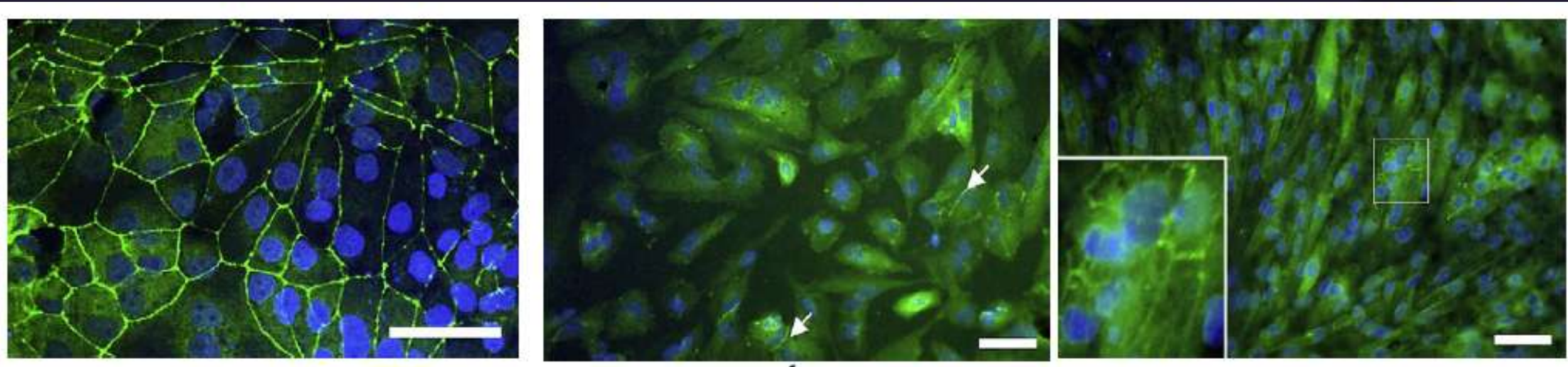








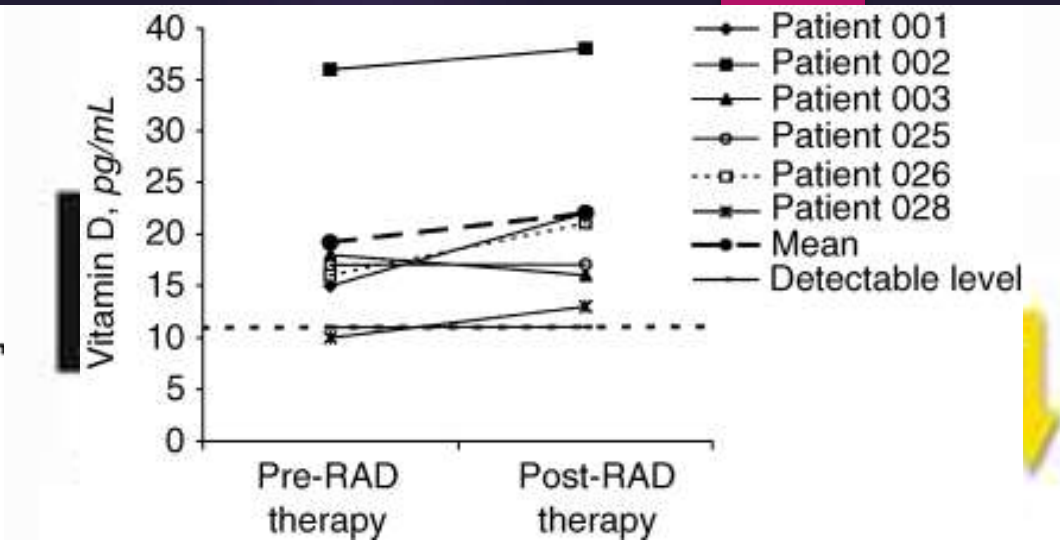
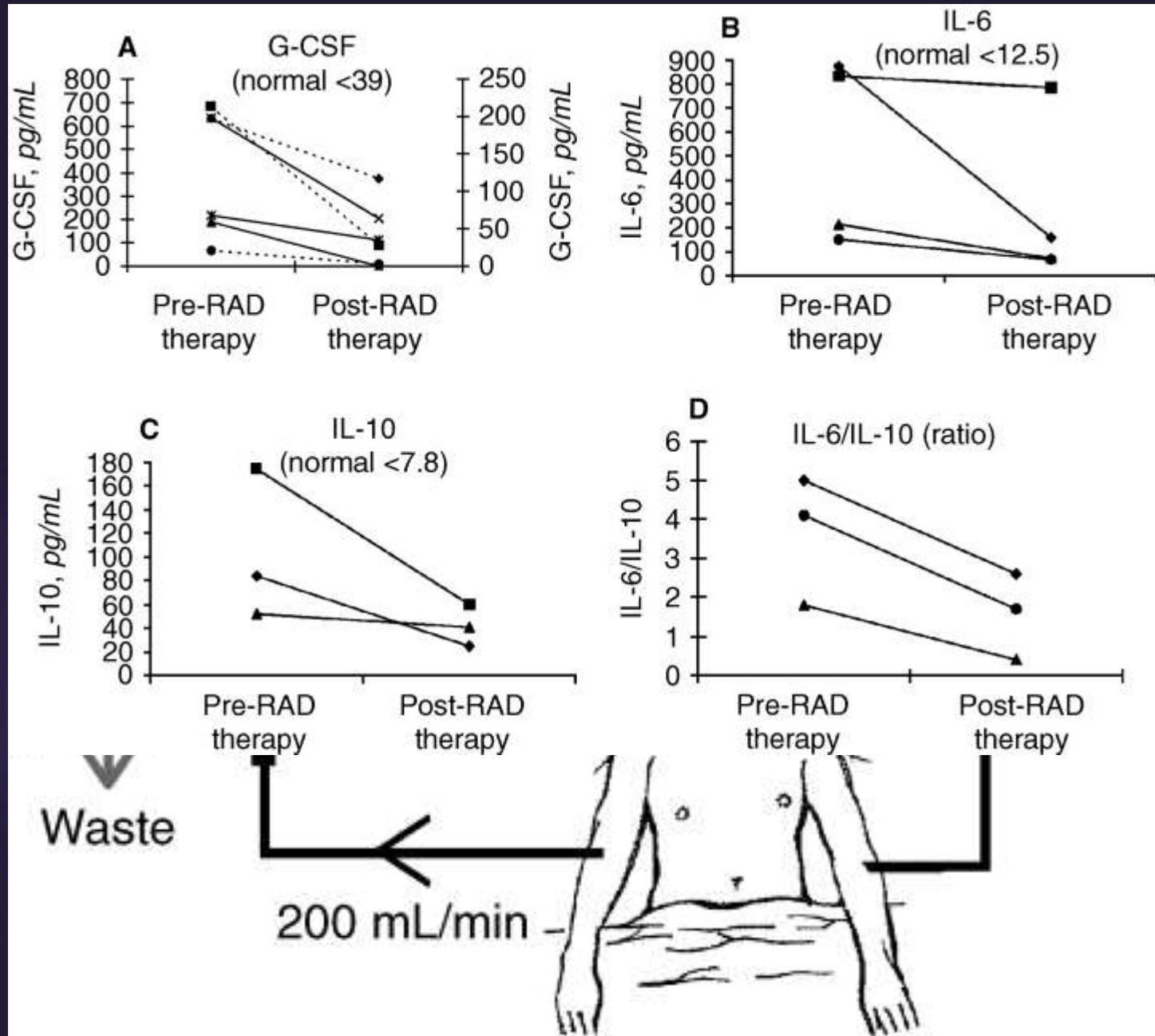
Madin-Darby canine kidney (MDCK) cells form a polarized epithelium on the inner surface of polyethersulfone/polyvinylpyrrolidone (PES/PVP) hollow fiber membranes. (a) Confluent monolayer of MDCK cells on the inner surface of a PES/PVP hollow fiber membrane



Immunostaining for tight junction ZO-1 protein (green) of renal cells after one week incubation on coated flat synthetic membranes

HPTC on coated PES/PVP membrane





Initial clinical results of the bioartificial kidney containing human cells in ICU patients with acute renal failure



# RAD : Clinical Trial All patients were critically ill with AKI and MOF

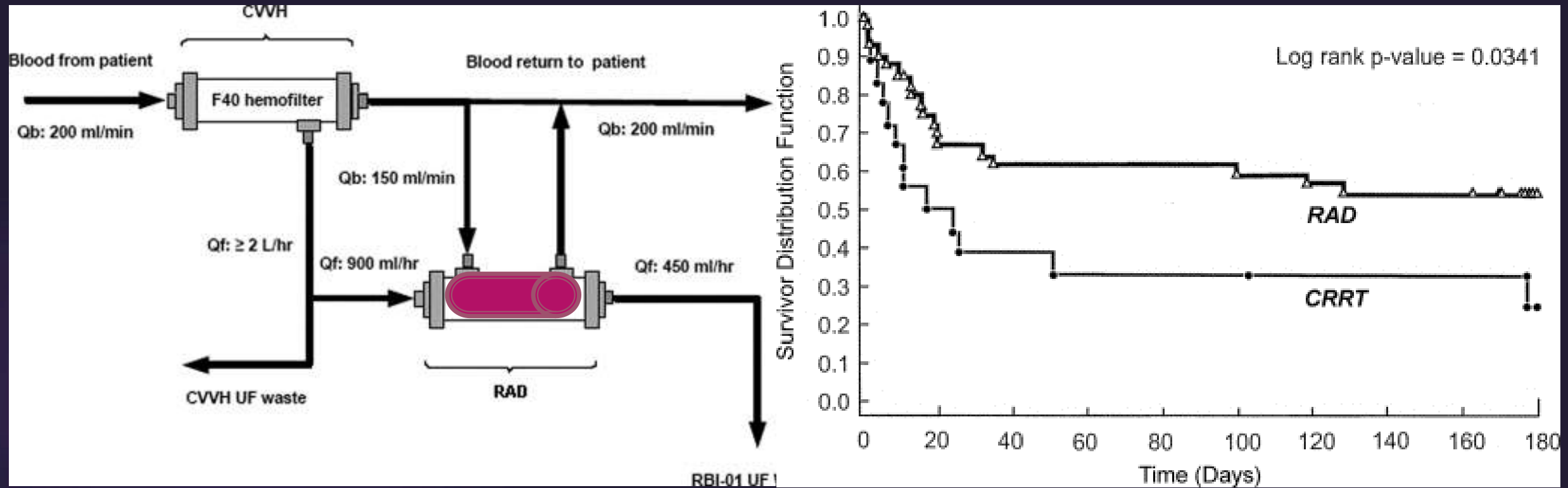
- ▶ initial study, consisting of 10 patients, demonstrated safe use of RAD therapy for up to 24 hours.
- ▶ Under RAD therapy, an actual mortality rate of 40% was demonstrated.
- ▶ RAD treatment resulted in significant declines in granulocyte-colony stimulating factor, interleukin (IL)-6, IL-10, and especially the IL-6/IL-10 ratio.
- ▶ RAD therapy improved the 28-day mortality rate from 61% in the conventional hemofiltration-treated control group to 34% in the RAD-treated group.
- ▶ the clinical trial was halted during the phase IIb interval analysis because of suboptimal clinical protocol design and several fabrication and manufacturing hurdles.

Humes,etal Blood Purif. 2004; 22: 60

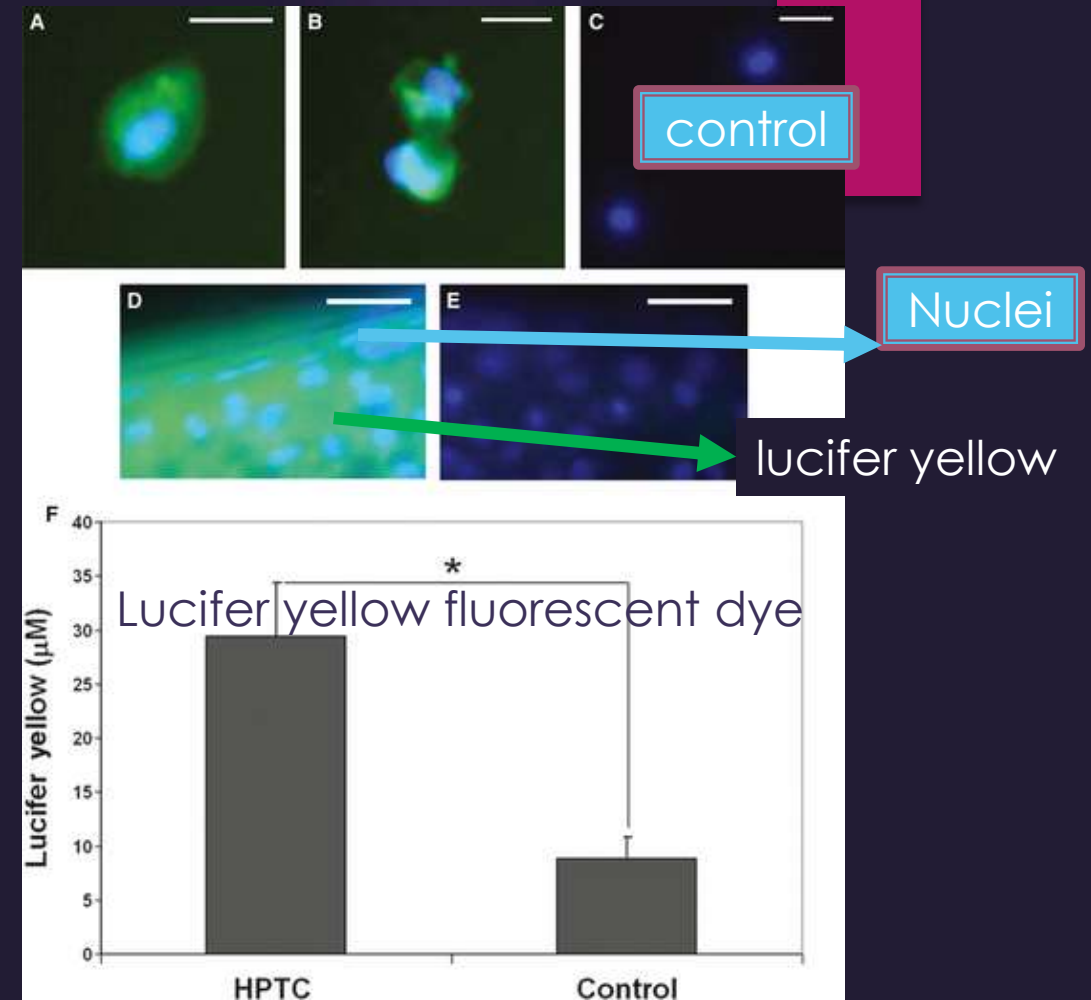
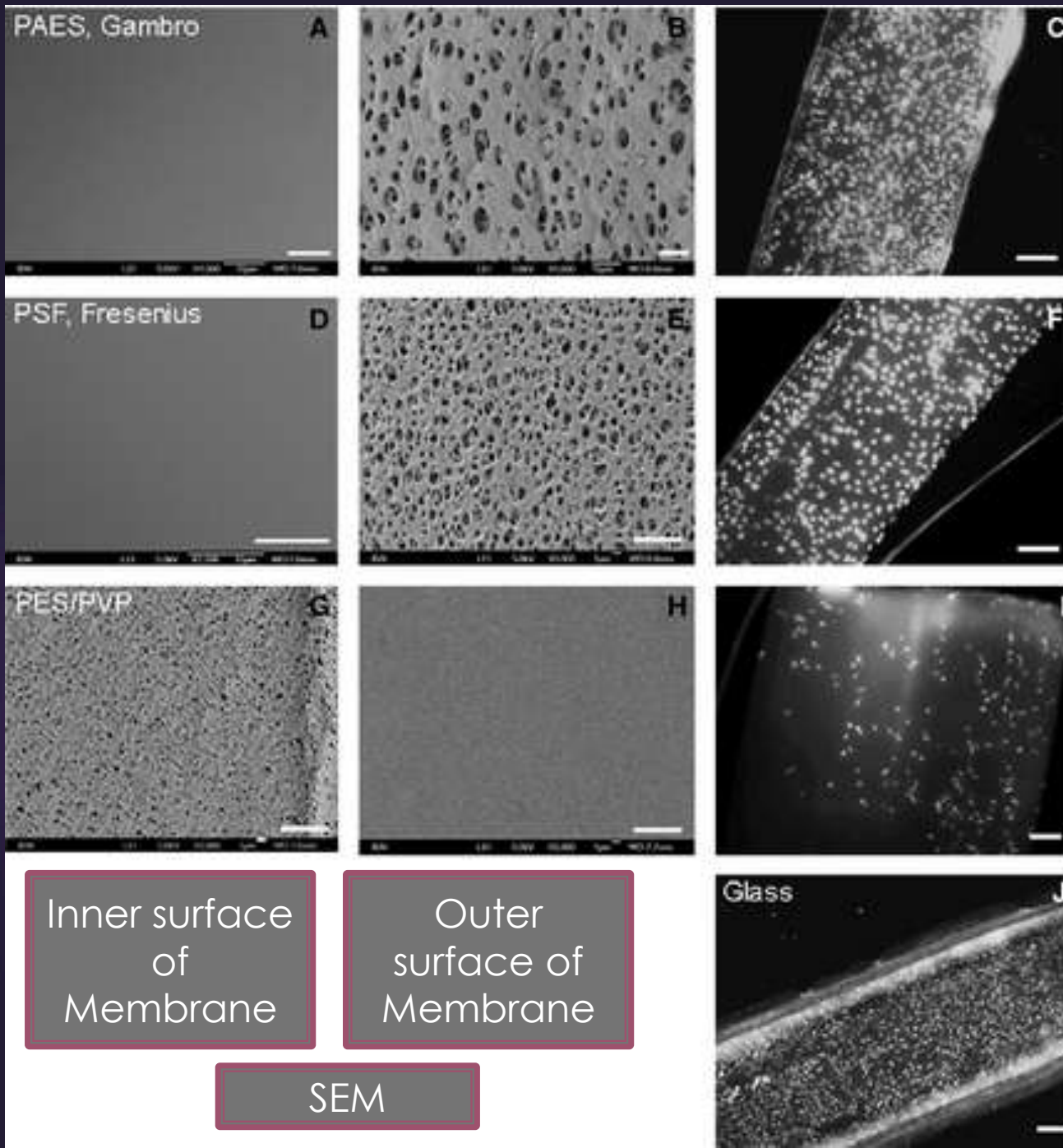
Tumlin etal J Am Soc Nephrol. 2008; 19



# Efficacy and Safety of Renal Tubule Cell Therapy for Acute Renal Failure J Am Soc Nephrol. 2008 May; 19



After the interim analysis, a corporate decision was made to discontinue enrollment in this study and proceed to the design of a confirmatory Phase II study



Baso-lateral cellular uptake and transport of lucifer yellow

J. Cell. Mol. Med. Vol 17, No 4, 2013

## **Bioartificial Renal Epithelial Cell System (BRECS): A Compact, Cryopreservable Extracorporeal Renal Replacement Device**

Deborah A. Buffington,\* Christopher J. Pino,\* Lijun Chen,\* Angela J. Westover,\*  
Gretchen Hageman,\* and H. David Humes\*†‡

\*Innovative BioTherapies, Inc., Ann Arbor, MI, USA

†Department of Internal Medicine, University of Michigan Medical School, Ann Arbor, MI, USA

‡CytoPherx, Inc., Ann Arbor, MI, USA

Bioartificial Renal Epithelial Cell System (BRECS),

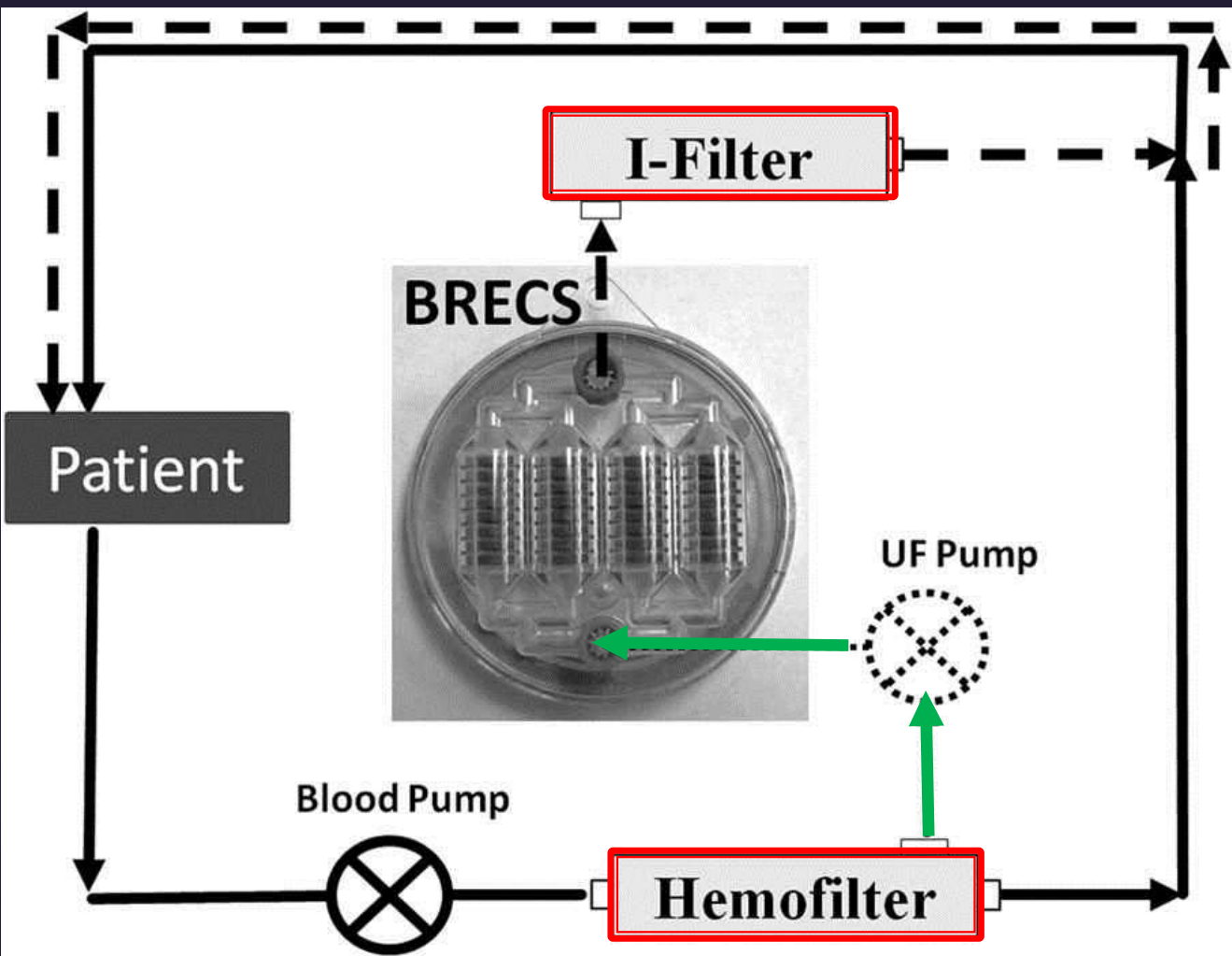


The BRECS was loaded with up to 20 cell-seeded porous disks

Once cells reached over  $5 \times 10^6$  cells/disk for a total therapeutic dose of approximately  $10^8$  cells



BRECS was cryopreserved for storage at  $-80^\circ\text{C}$  or  $-140^\circ\text{C}$ .



65-kDa molecular weight cutoff

an immunoisolation filter (I-Filter), which protects the patient from any large molecular by-products and/or cells released by the BRECS that could cause an adverse reaction





**Blood**



**Filtrate**



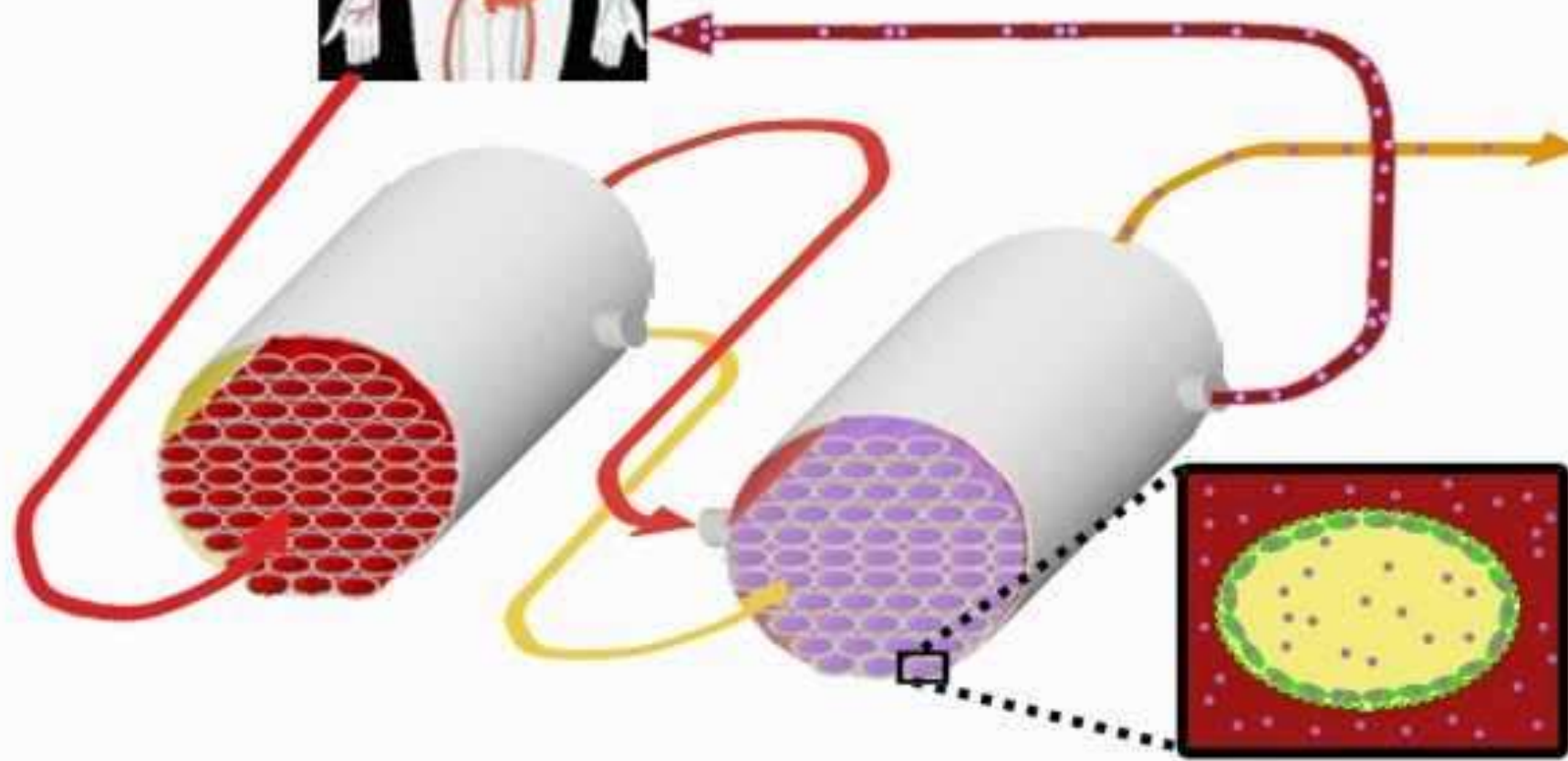
**Processed  
Filtrate**

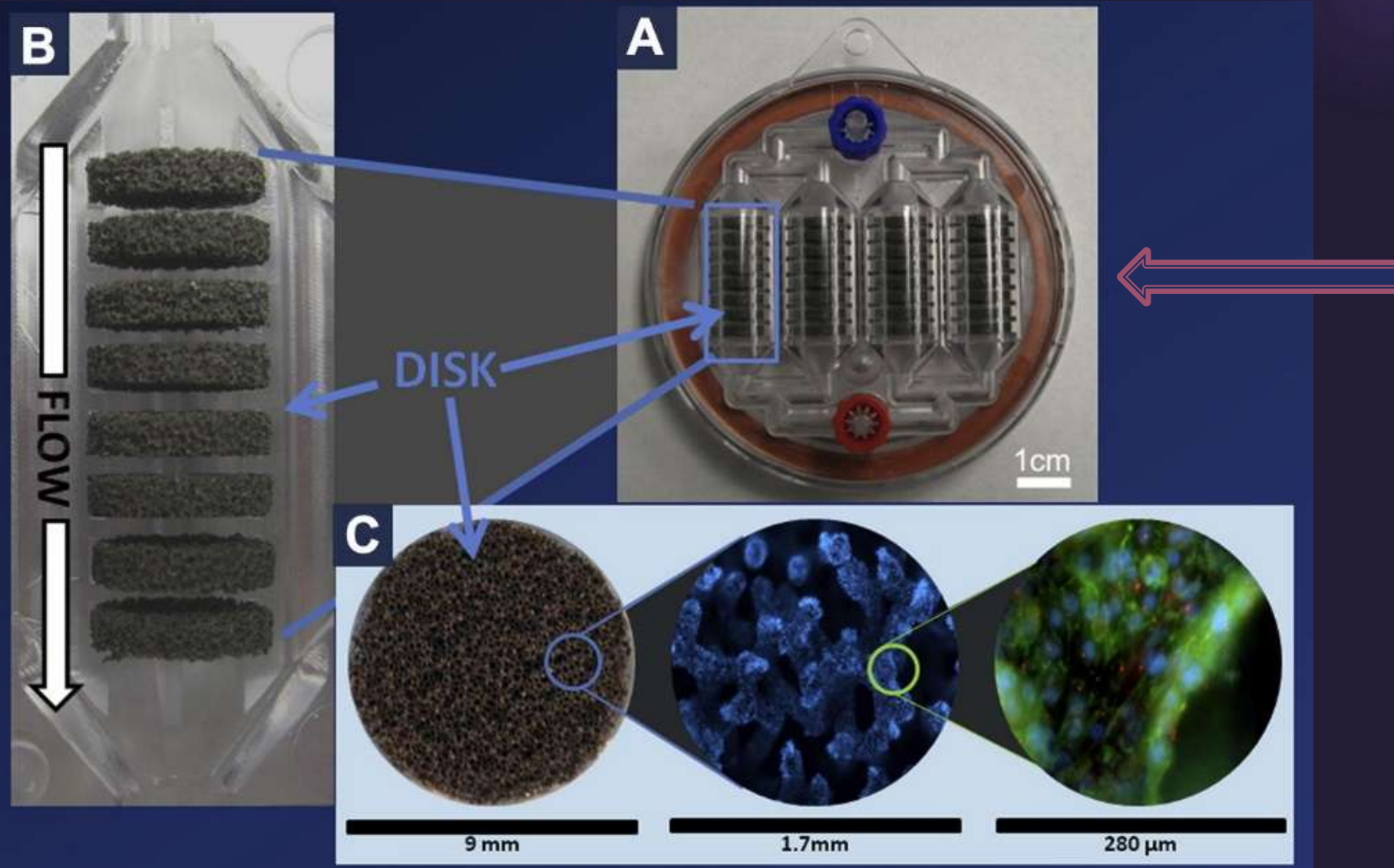


**BMP-7**



**Cells**





carbon disk stack  
channel

human renal epithelial  
cells derived from the  
enhanced propagation  
(EP) method of cell  
expansion

The compact, freezable bioartificial renal epithelial cell system  
(BRECS) design

**more than 5000 BRECS to be fabricated**

# Bioartificial kidney: steps toward clinical application

Hurdle	Solution status
FDA approval for first in human clinical trial testing.	Renal cell therapy has demonstrated safety and efficacy in preclinical (RAD and BRECS) and clinical studies (RAD).
Bioengineered cell system for mass production.	A compact BRECS has been developed for use in renal and inflammatory chronic and acute indications.
Bioengineered cell system capable for onsite, on-demand clinical use.	The BRECS can be cryopreserved for transport, storage, and reconstitution at clinical sites.

BRECS, bioartificial renal epithelial cell system

Translational Research ,April 2014Volume 163,

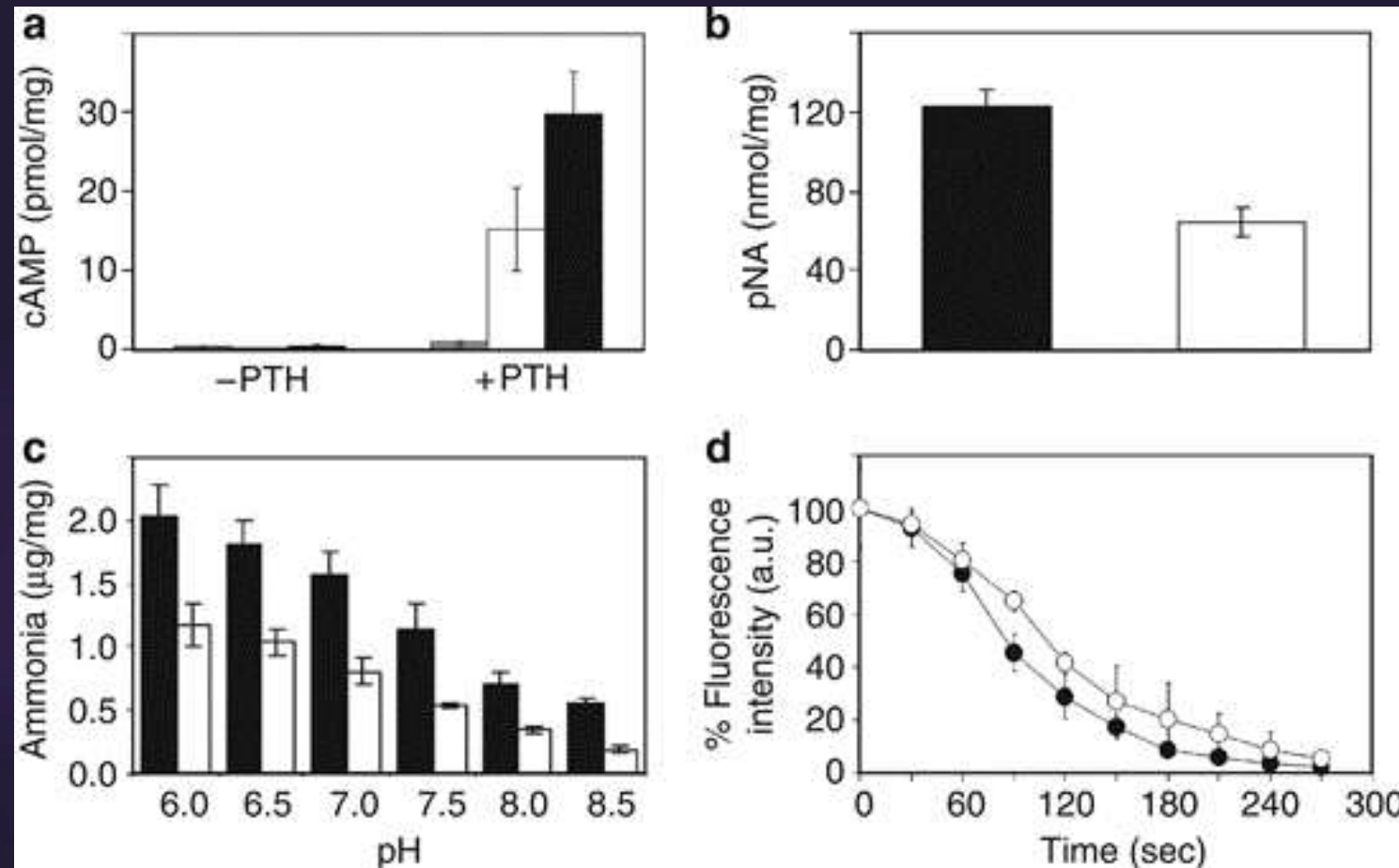


**Toward a bioartificial kidney: will embryonic stem cells be the answer?** Kidney International (2013) 83, 543



# Human embryonic stem cells differentiate into functional renal proximal tubular-like cells

Narayanan et al Kidney International (2013) 83



(HPTCs) (positive control, black bars)

(a) Response to parathyroid hormone (PTH)

(b)  $\gamma$ -glutamyl transferase (GGT) activity  
Measured by The concentration of p-nitroaniline (pNA) produced by the cells

(c) Ammonia production

(d) Water transport assay

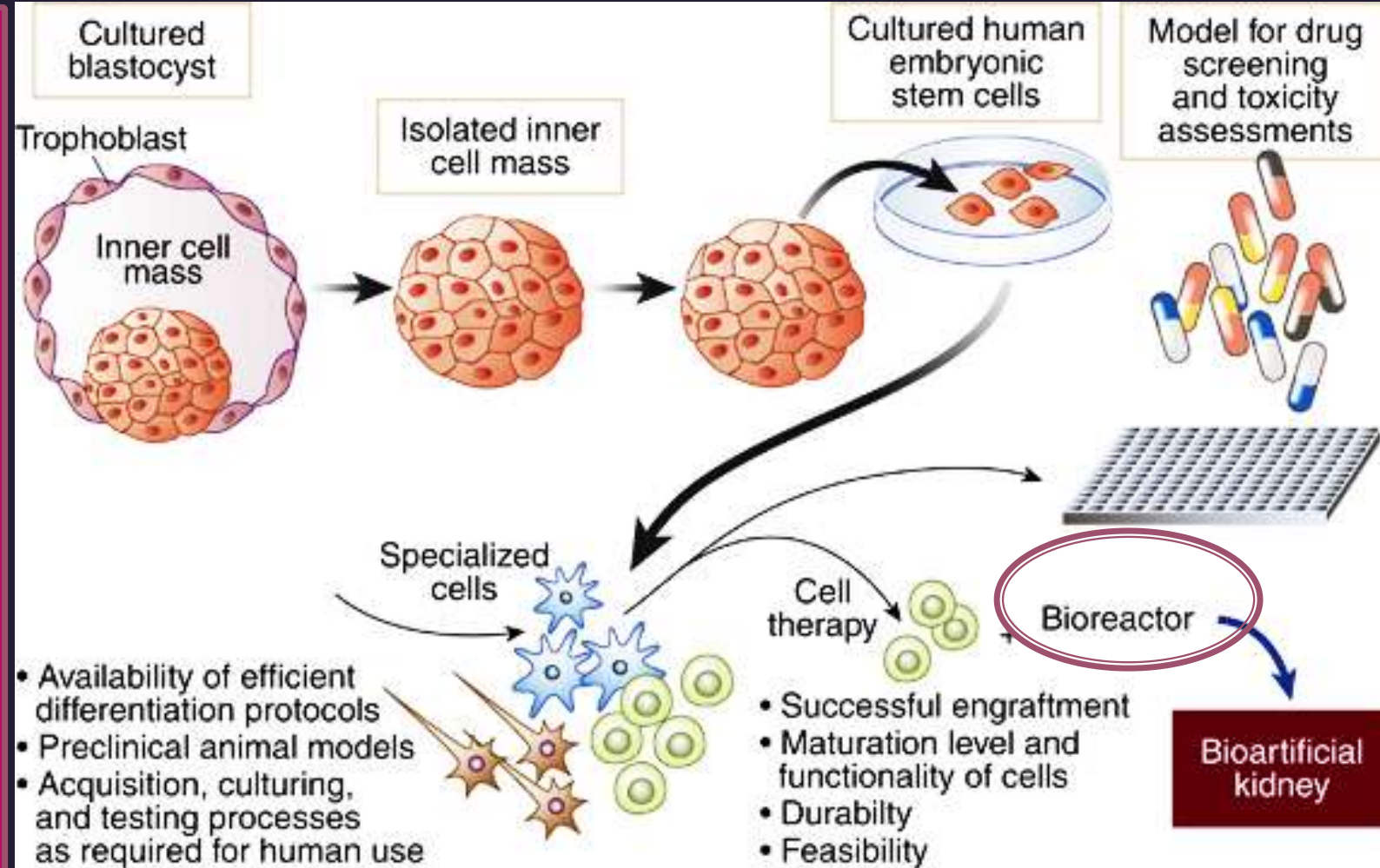
Functional assays with differentiated human embryonic stem cells (hESCs) in static cultures

# Toward a bioartificial kidney: will embryonic stem cells be the answer? Kidney International (2013) 83, 543

## Problems

downregulation of several transporters, including apical and basolateral glucose transporters and organic acid, cationic, and peptide transporters.

Additionally, a proportion of these cells dedifferentiated in *in vivo* experiments, and hence future tumorigenesis studies and epigenetic characterization are important if clinical use is contemplated



## **Understanding the bioactivity of stem cells seeded on extracellular matrix scaffolds produced from discarded human kidneys: a critical step towards a new generation bio-artificial kidney**

*A. Petrosyan<sup>1</sup>, G. Orlando<sup>2,3</sup>, A. Peloso<sup>2,4</sup>, Z. Wang<sup>2</sup>, A.C. Farney<sup>2</sup>, J. Rogers<sup>2</sup>, R. Katari<sup>2,3</sup>, S. Da Sacco<sup>1</sup>, S. Sedrakyan<sup>1</sup>, R.E. De Filippo<sup>1</sup>, R.J. Stratta<sup>2</sup>, S. Soker<sup>3</sup>, L. Perin<sup>1</sup>*

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<sup>1</sup>GOFARR Laboratory, Saban Research Institute, Children's Hospital Los Angeles; Department of Urology, University of Southern California, Los Angeles, CA, USA.

<sup>2</sup>Department of General Surgery, Section of Transplantation, Wake Forest School of Medicine, Winston Salem, NC, USA

<sup>3</sup>Wake Forest Institute for Regenerative Medicine, Wake Forest School of Medicine, Winston Salem, NC, USA

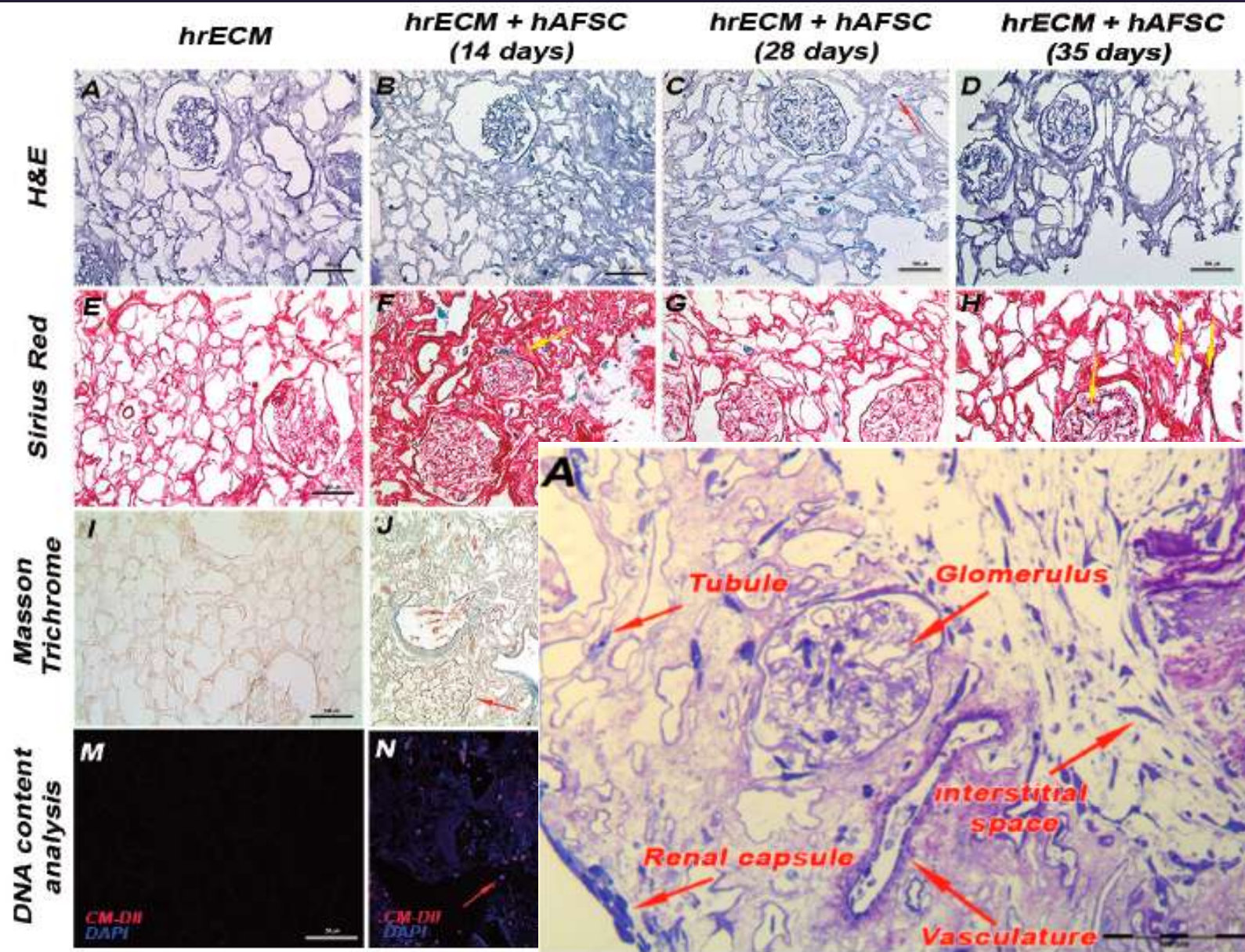
<sup>4</sup>General Surgery, Fondazione IRCCS Policlinico San Matteo Pavia and University of Pavia, Pavia, Italy

<sup>5</sup>Carolina Donor Services, Winston Salem, USA

Giuseppe Orlando and Astgik Petrosyan share the first Authorship

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Histological analysis of Human Amniotic Stem cells (hAFSC) distribution over 14, 28, and 35 days after seeding on human renal extracellular matrix (hrECM)

**CELLR<sup>4</sup>**

CellR4 2015; 3 (1): e1401

This model provides critical information which may be of importance in both kidney bioengineering and regeneration



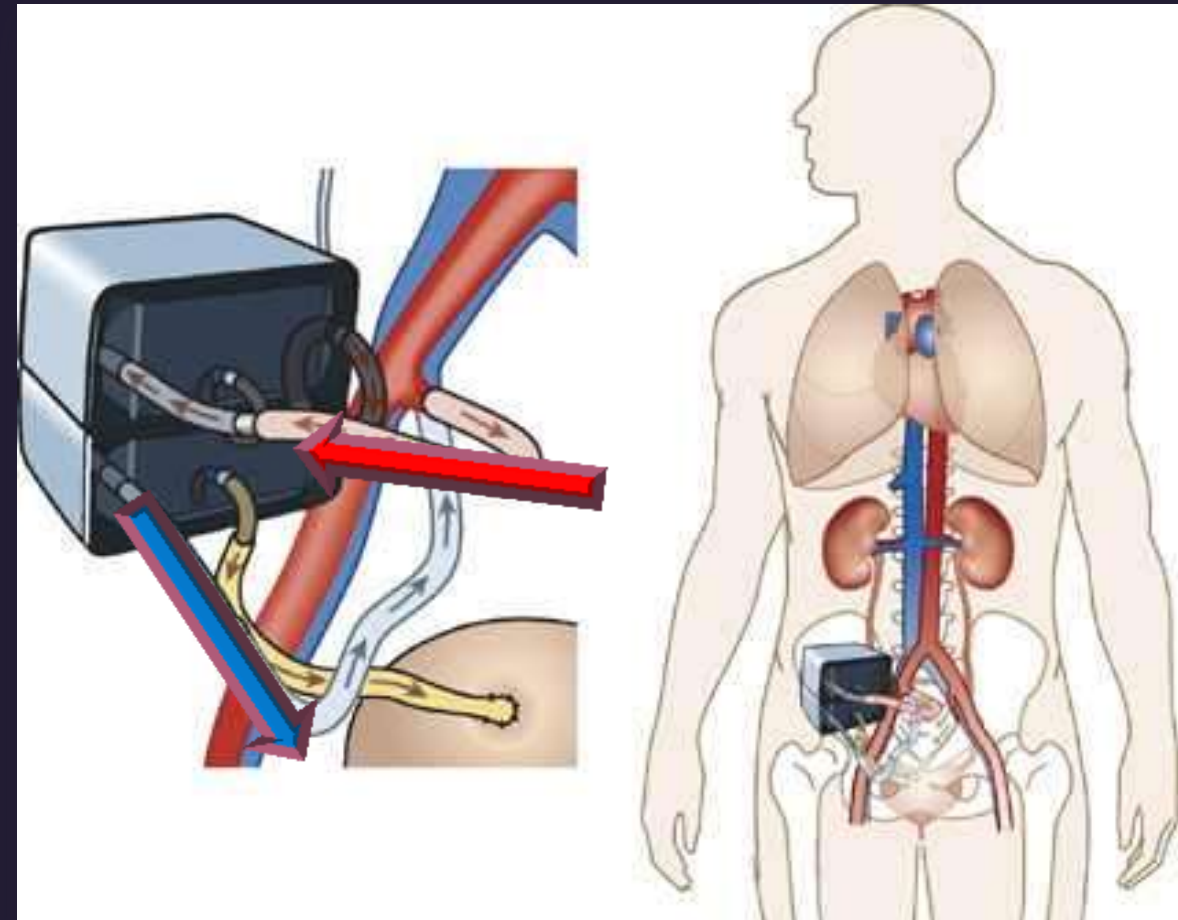
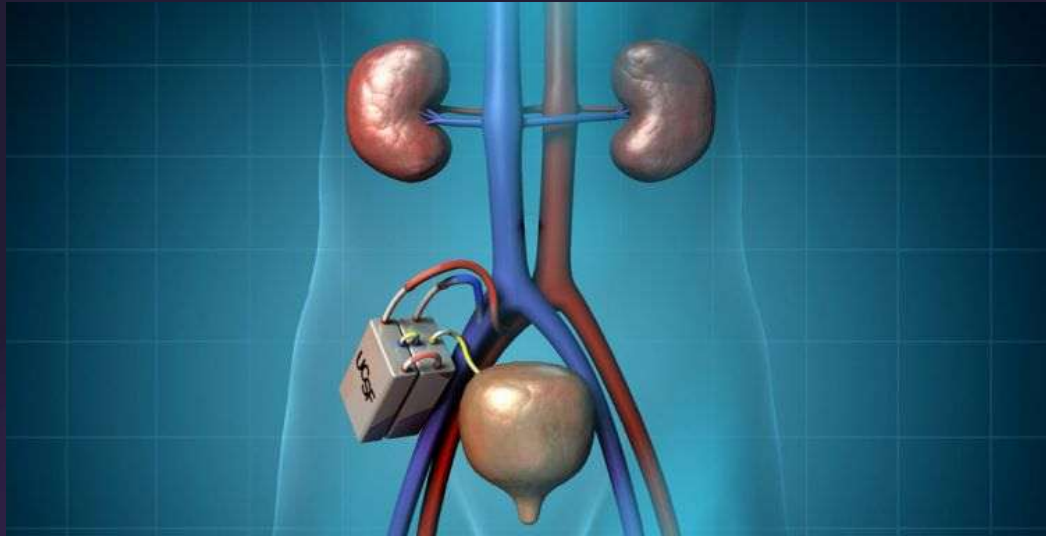
# Implantable Device

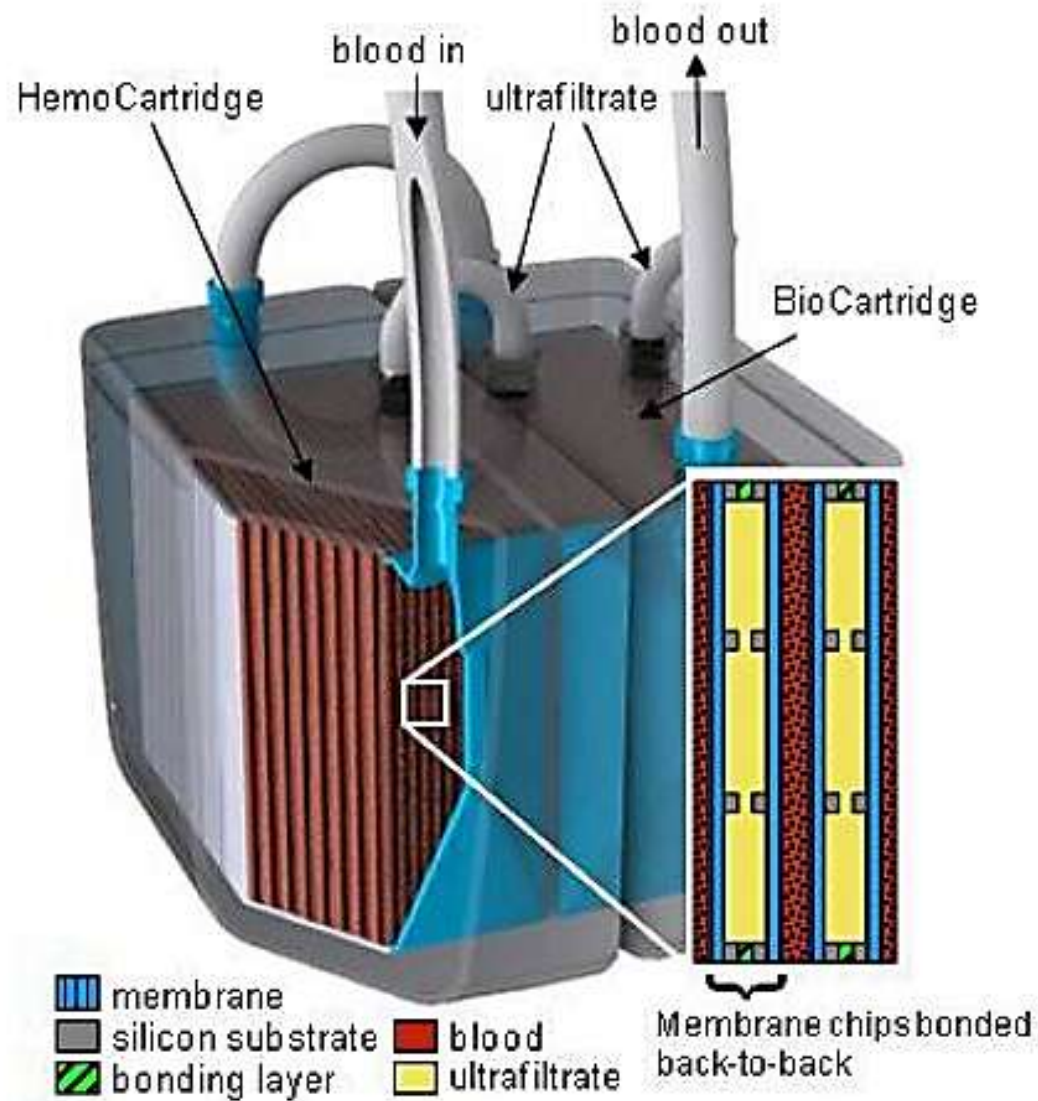


- ▶ University of California-San Francisco researchers unveiled a prototype model of the first implantable artificial kidney on September 2, 2010
- ▶ Received \$3 million in funding as of October 1, 2012.
- ▶ Plan to go through human clinical trials by 2017.

# Implantable Device

University of California San Francisco





First compartment holds thousands of nano-scale filters remove toxins from the blood (Super efficient membranes)

A second compartment would hold live kidney cells that perform the other biological actions of a real kidney

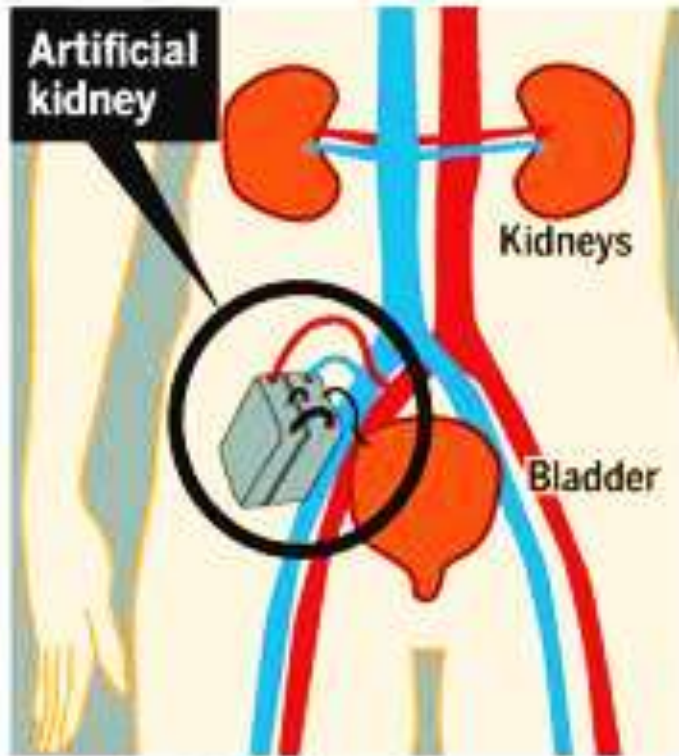


# Implantable Device



## Implantable artificial kidney

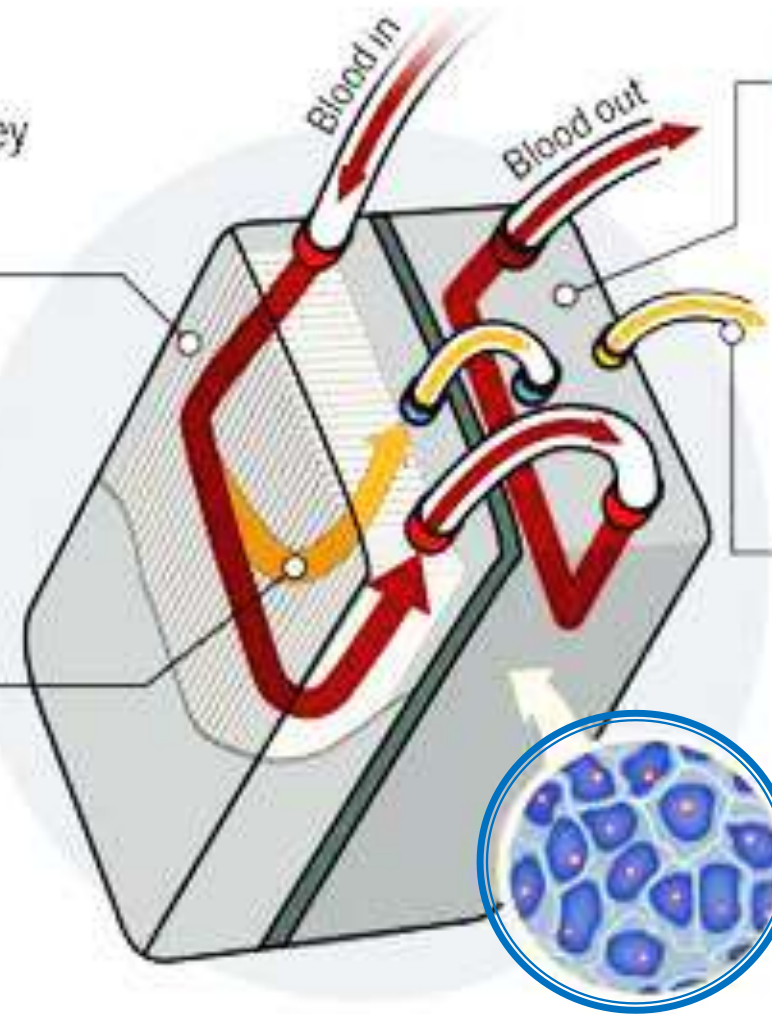
UC San Francisco is heading a team of researchers around the country who are working to create an implantable, artificial kidney the size of a coffee cup. The device consists of two chambers:



### 1 Hemofilter

The left chamber filters incoming blood with super-efficient membranes made with silicon nanotechnology.

Ultrafiltrate, separated from the blood, contains dissolved toxins, as well as water, sugars and salts.



### 2 Cell bioreactor

The right chamber contains live kidney cells that reabsorb much of the water, sugars and salts into the bloodstream.

The toxins and excess water are passed into the waste outlet connected to the bladder.

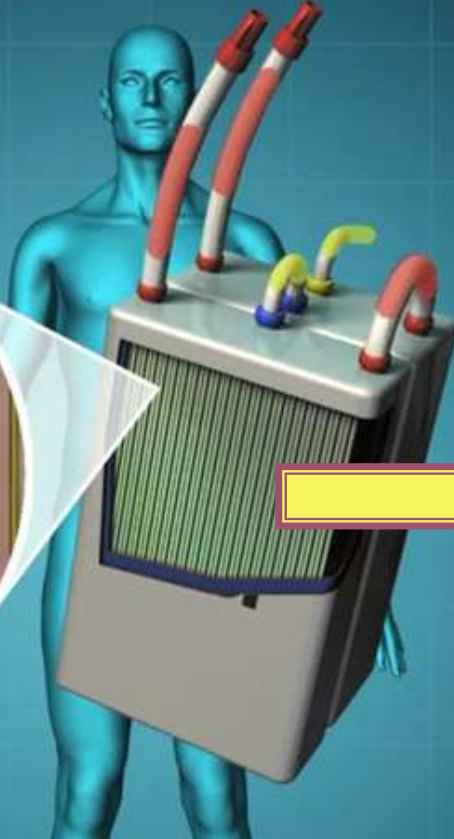
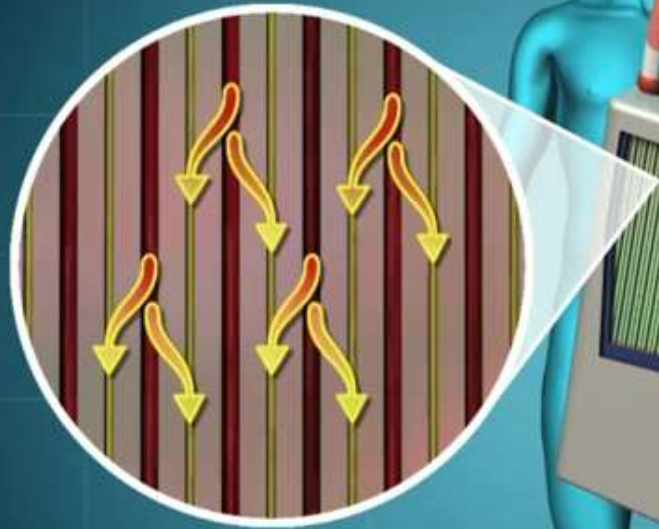
Kidney cells

# Implantable Device

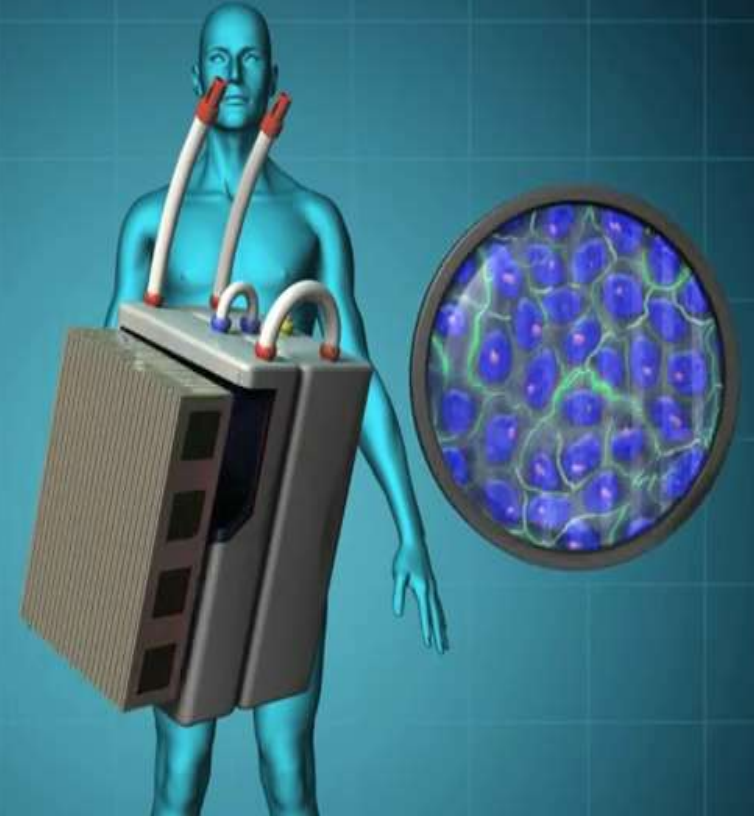
## Fast Tract FDA registration



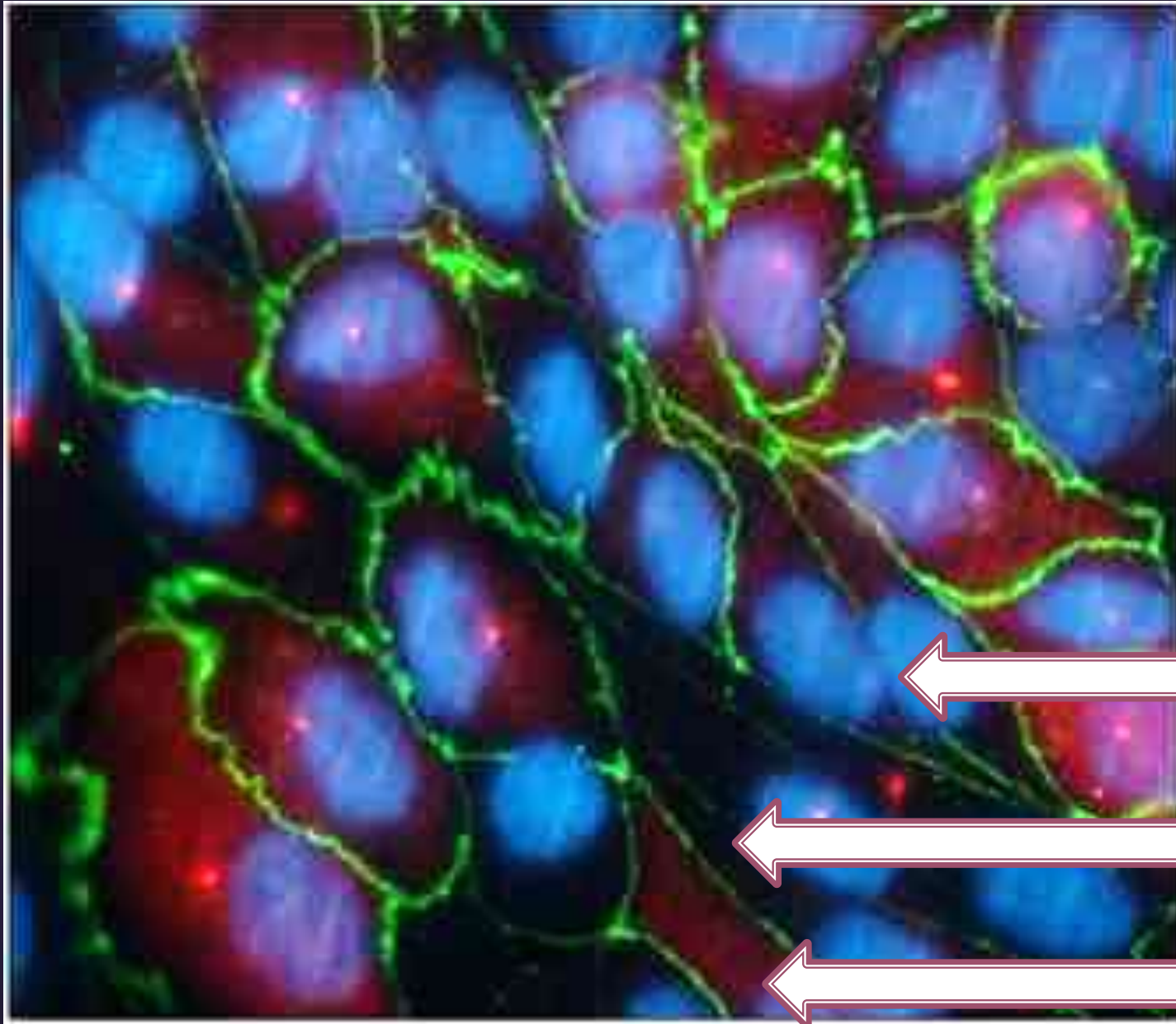
1



2







**Fluorescent  
microscopy image of  
human renal proximal  
tubule cells cultured  
from discarded renal  
transplant kidneys on  
silicon nanopore  
membranes.**

Blue stain refers to cell  
nuclei,  
green refers to tight  
junctions, and  
red refers to cilia



# Conclusion

## Current status of bioartificial kidney

Journal of Biomedical Science and Engineering Vol.7 No.3(2014),

Although studies about cell therapy and wearable devices have not been conducted for quite a long-term period, it is promising that these new therapies will be available as options in the near future.

it is not a daydream that new therapeutic options such as Bioartificial kidney and wearable dialysis devices for ESRD patients will be applied in the routine clinical practice in nephrology area.

Thank  
you

